

Preprocessing & denoising of fMRI data

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Plan

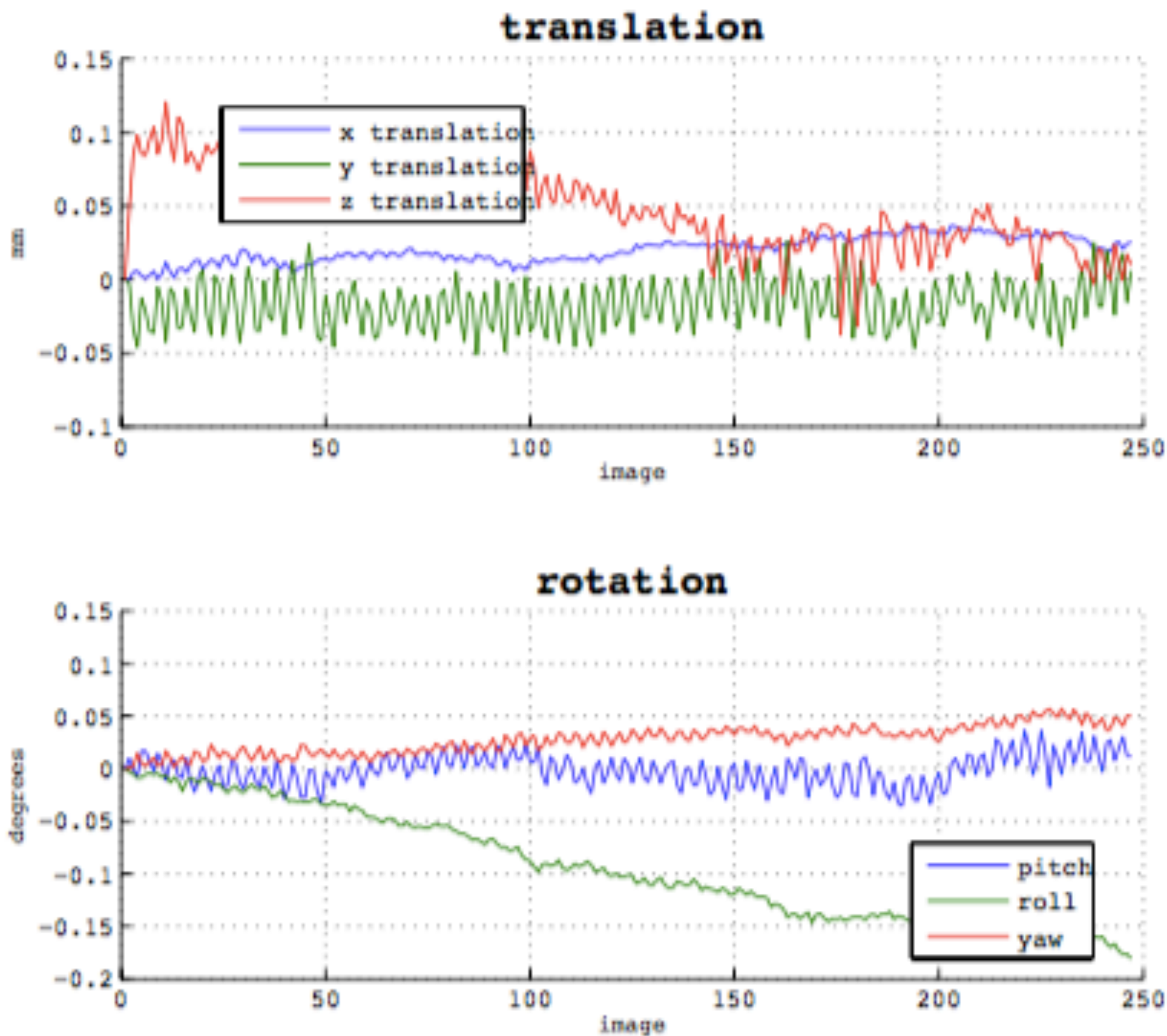
- Simple fMRI pre-processing pipeline in 2018
- Signal fluctuations or noise
- Motion related noise & denoising in GLM
- Denoising based on external physiological signals
- TAPAS Physio Toolbox
- Denoising based on PCA of noise regions signals
- Example of results
- Questions to be addressed
- Next step : Multi-Echo acquisitions
- Conclusion & references

Simple fMRI pre-processing pipeline (2018)

- * Check of the data : quality, coregistration, ...
- * Fielmap computation → Voxel Displacements Map
- * Realign & unwarp
- * Coregistration of anatomical data to functional data
- * Spatial Normalisation to the MNI space (DARTEL)
- * Spatial smoothing

Nota : the slice timing step is often skipped because of the interpolation problems and is no more really useful thanks to short TRs (≈ 1 sec)

Motion parameters estimates



→ Signal fluctuations or noise ...

EPI Multi-bande sequences

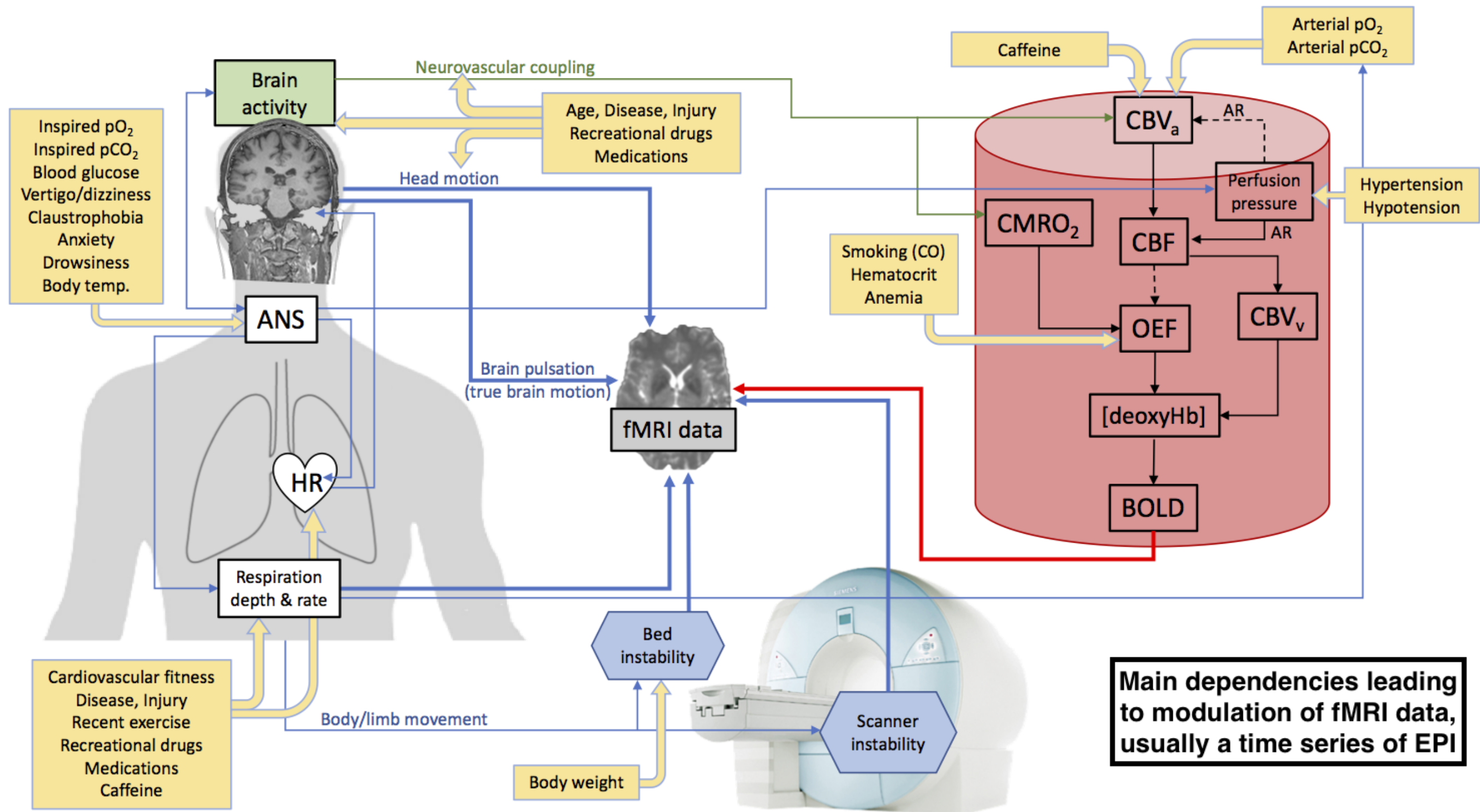
- Very short TR (≈ 1 sec)
 - Small voxels (≈ 2.5 mm iso)
 - High SNR (multi-channel receiving coils)
- Artefacts seem to be more visibles than with older MRI systems

→ Signal fluctuations or noise ...

Different sources of noise :

- Head motion
- Cardiac pulsatility → motion (global) & inflow (local)
- Respiratory induced changes → change of B0 in the head
- Draining veins
- Slow drifts
- Hardware related instabilities

→ Signal fluctuations or noise ...

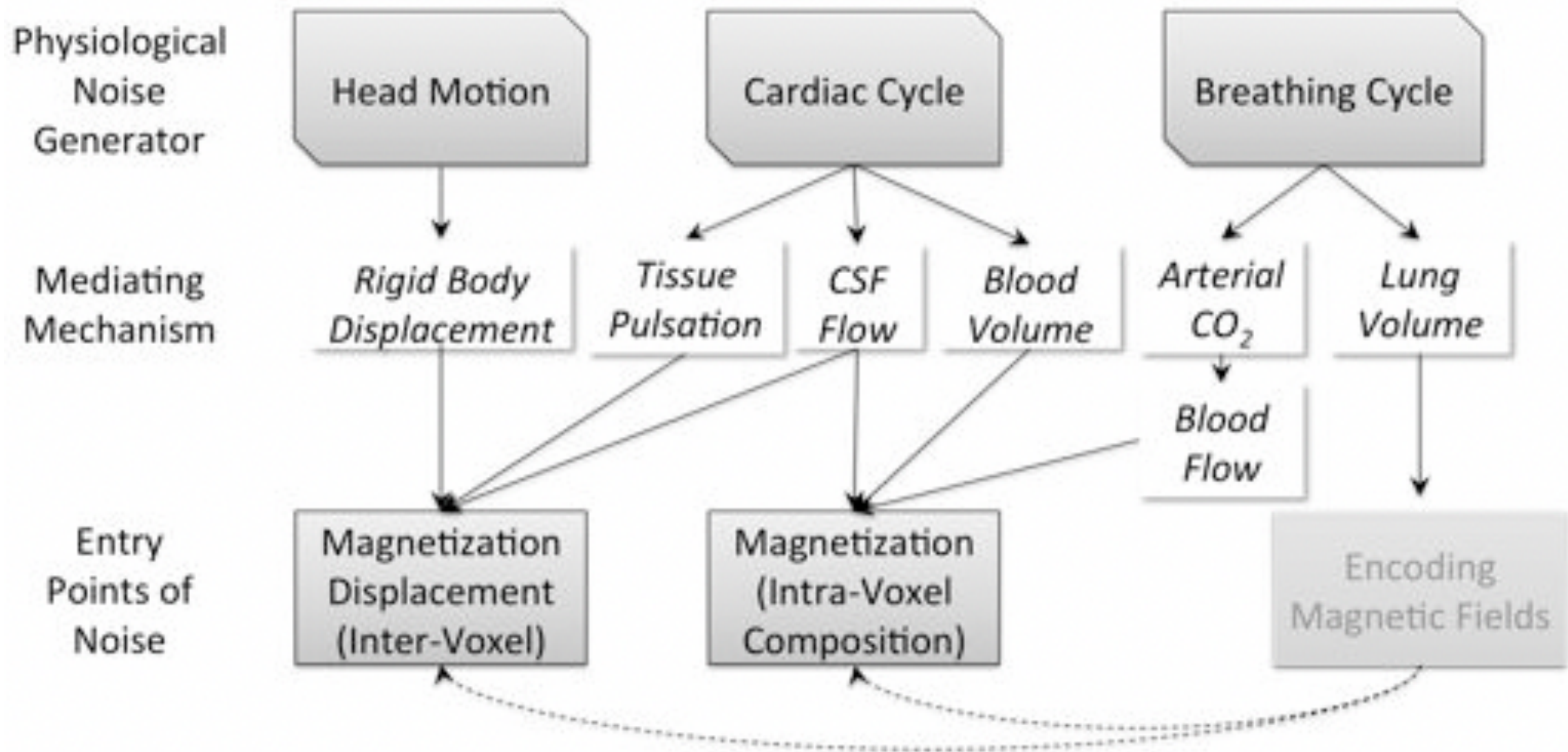


Krainik & al, 2013

→ Signal fluctuations or noise ...

Different sources of noise :

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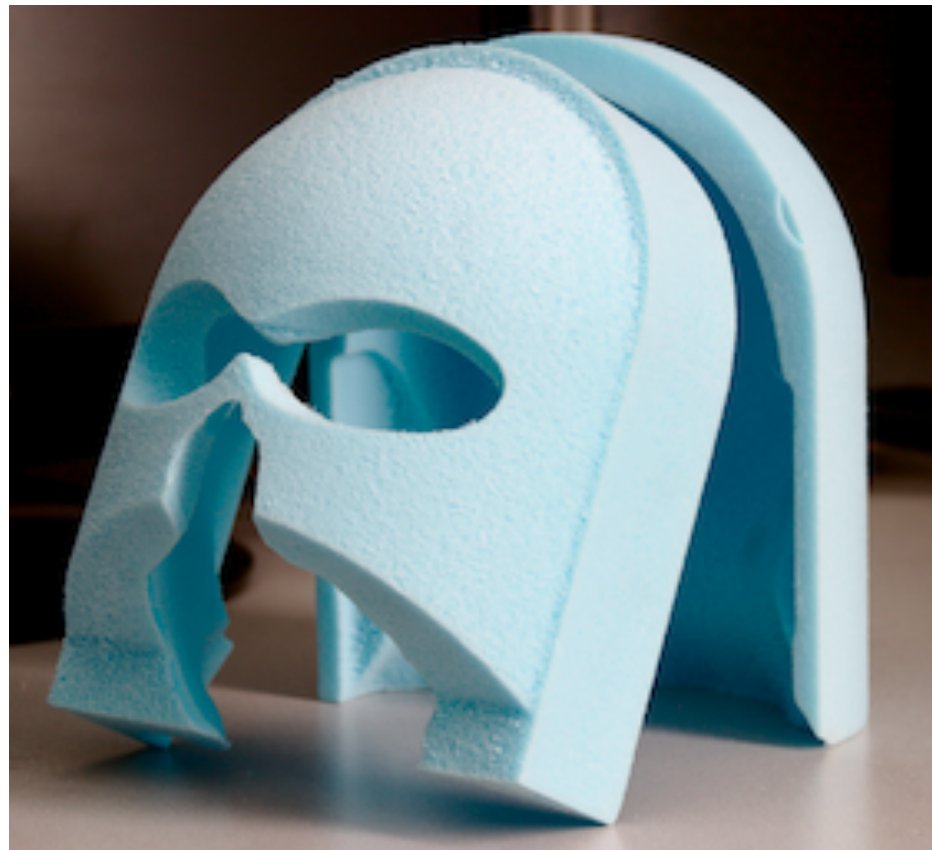
Motion-related noise

- The best solution is to limit the head motion of the subject **during** the data acquisition :
 - compliant & trained subjects : mock-scanner is useful !



Motion-related noise

- The best solution is to limit the head motion of the subject **during** the data acquisition :
 - compliant & trained subjects
 - good head restraint : inflating pads (already available)
- or the ultimate solution : <https://caseforge.co/>



Motion-related noise

- The best solution is to limit the head motion of the subject **during** the data acquisition :
 - compliant & trained subjects
 - good head restraint
- on-line head motion monitoring :
 - feedback to the subject in case of problematic motion
 - and/or run longer acquisitions

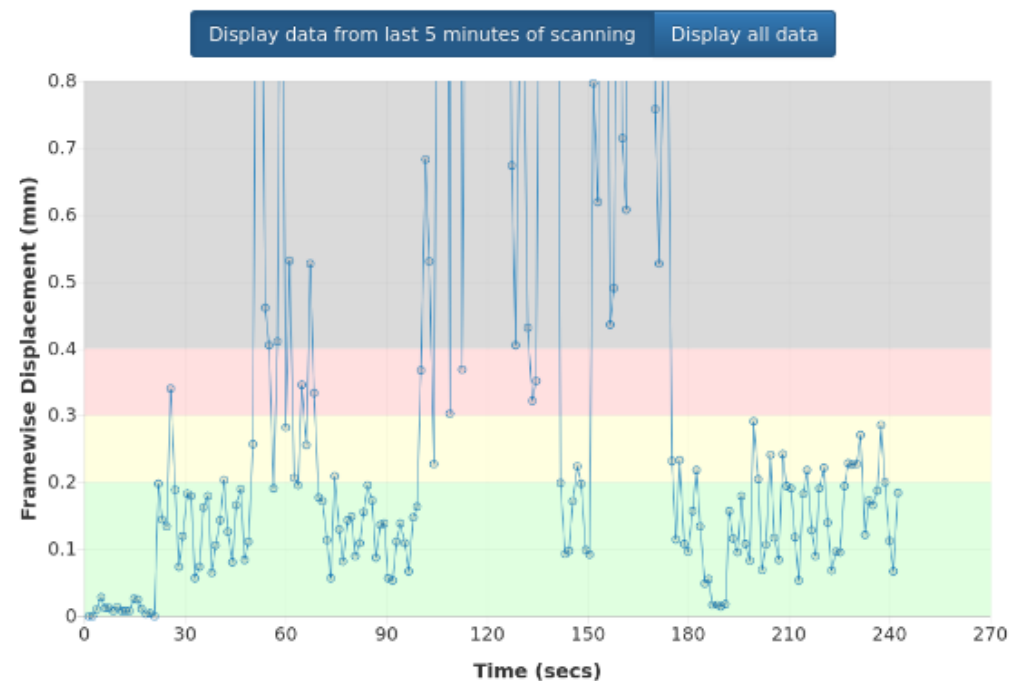
FIRMM : Real-time head motion analysis

FIRMM version 2.1.3

Waiting for next DICOM...

DICOM folder being monitored	/home/firmmproc/FIRMM/incoming/20180214_JS_TOF3.18.02.14_16_45_26_STD_1.3.12.2.1107.5.2.43.66072
Patient Name	JS_TOF3
Patient ID	18.02.14-16:45:26-STD-1.3.12.2.1107.5.2.43.66072

Toggle patient info table



Summary

Series	Description	Frames	TR (sec)	Time (min)	< 0.2 mm (min) (%)	< 0.3 mm (min) (%)	< 0.4 mm (min) (%)
15	AUDIO_RUN1_PERC	182	1.224	3:42	1:57 (52.7%)	2:25 (65.4%)	2:35 (69.8%)
10	task-rest_bold	15	1.224	0:18	0:18 (100.0%)	0:18 (100.0%)	0:18 (100.0%)
9	task-rest_bold_SBRef	1	1.224	0:01	0:01 (100.0%)	0:01 (100.0%)	0:01 (100.0%)

FIRMM version 2.1.3

Start

Reset

Load Previous Scan



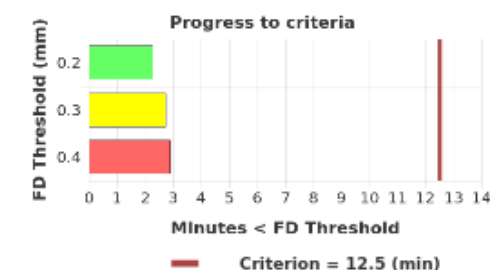
< 0.2 mm



< 0.3 mm



< 0.4 mm



Collected Low Movement Frames

	< 0.2 mm	< 0.3 mm	< 0.4 mm
Good Time (min) (%)	2:17 (56.6%)	2:45 (68.2%)	2:55 (72.2%)
Good Frames	112	135	143
Bad Frames	86	63	55

Predicted Duration to Scan Criteria

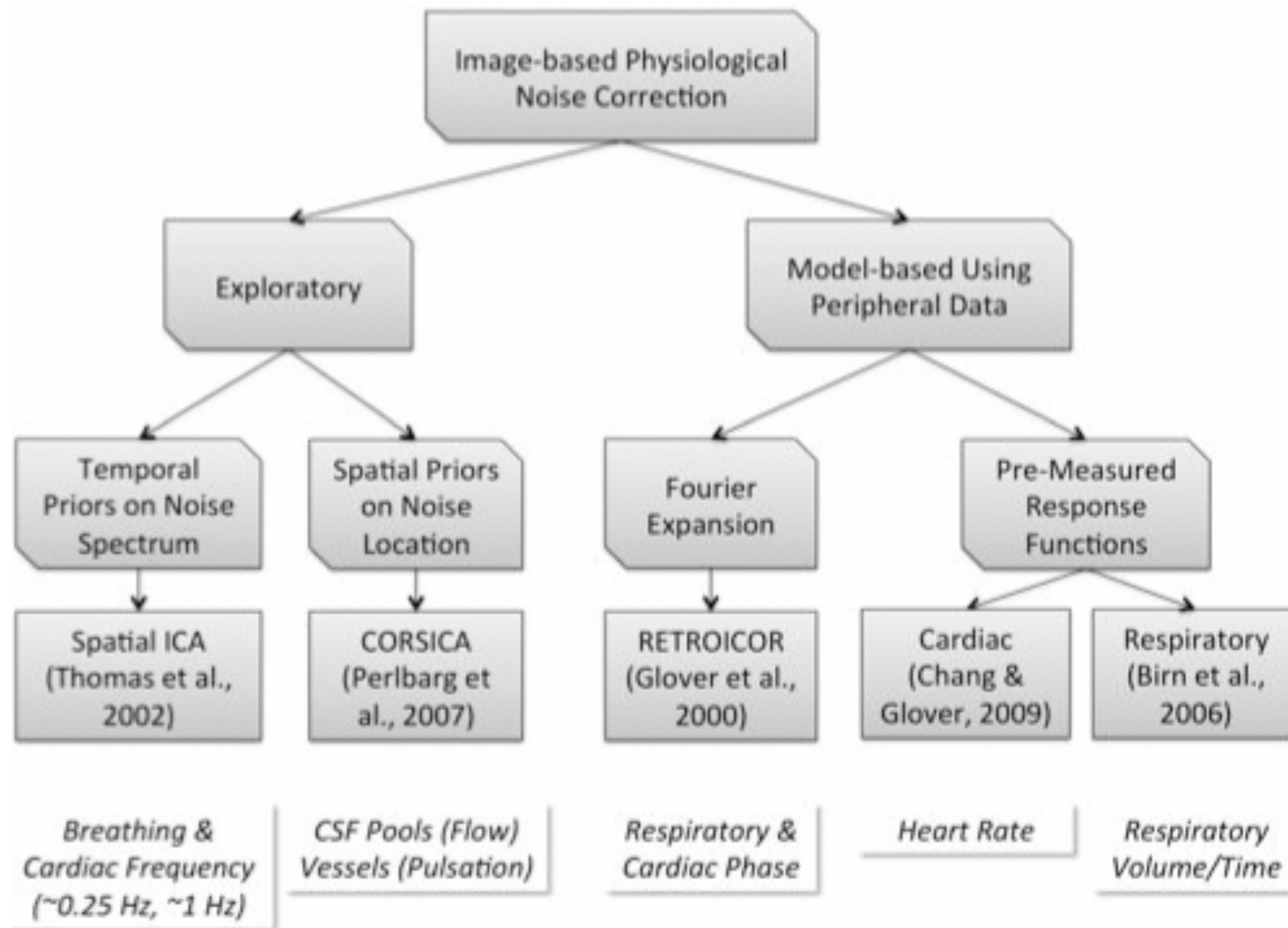
	< 0.2 mm	< 0.3 mm	< 0.4 mm
Minutes to	20:53	16:47	15:14

Denoising motion-related noise

- 1/ Motion correction : Realignment pre-processing
 - classical rigid-body volume correction
 - or slice by slice : SLOMOCO (Ball & Lowe 2014), to be tested
- 2/ Modelisation of motion-related artifacts : in GLM, 6, 12, 24 or 36 nuisance regressors : realignment parameters time series ($rp(t)$), their squared time series ($rp^2(t)$), plus one or two temporal derivatives ($rp(t-1)$) (Friston & al, 1996)
- 2bis/ Modelisation of artifacted scans (head jerks, transitory problem) : censoring (1 regressor per outlier scan). See Artifact Detection Tools (ART) for example.

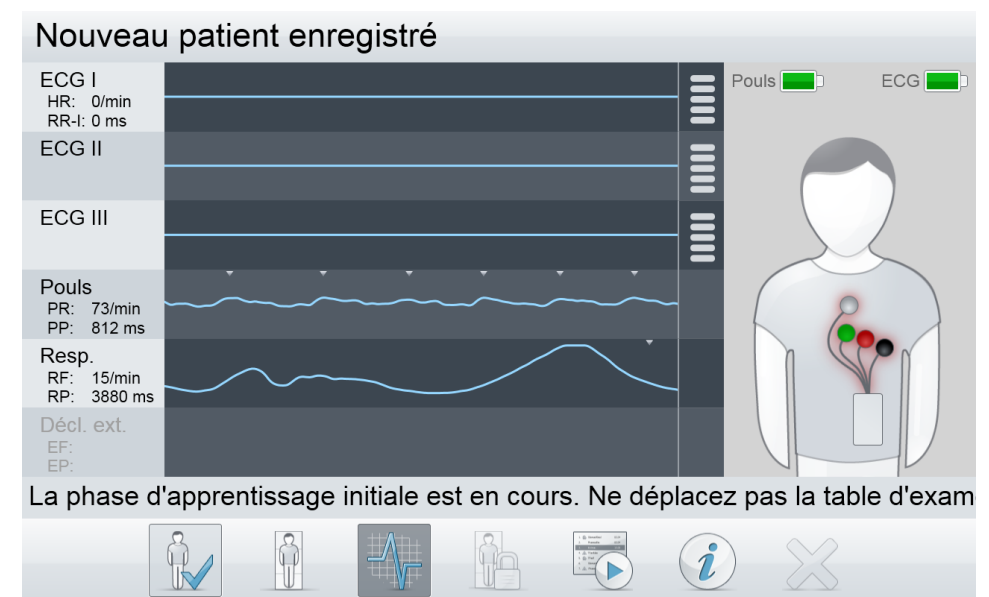
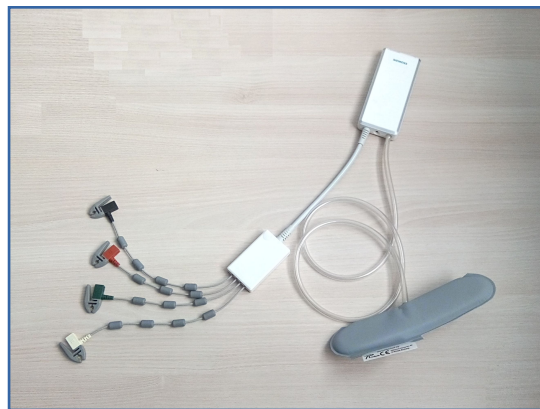
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
- Data-driven denoising methods of physiological noise



Denoising physiological-related noise

- Denoising physiological noise based on external recordings
 - Respiration cycle : pneumatic belt
 - Cardiac pulse : Photo-Plethysmo-Graph (PPG)



Denoising physiological-related noise

- Denoising physiological noise based on external recordings

In RETROspective Image CORrection (RETROICOR, Glover et al., 2000), the quasi-periodic physiological noise time series is modelled by means of a low-order Fourier series with time-varying cardiac and respiratory phases, which are fit to the data as nuisance regressors and removed.

Denoising physiological-related noise

- Denoising physiological noise based on external recordings

The same physiological recordings can also be employed to reduce low-frequency BOLD fluctuations related to varying cardiac and respiratory rates

- Heart Rate Variability (HRV)
 - Respiration Volume Time series (RVT)
- Assuming that the relationship between the HRV and RVT fluctuations and the BOLD signal follows a linear model
→ nuisance regressors obtained by convolving the HRV and RVT time series with a respiratory response function (Birn et al., 2008) and cardiac response function (Chang et al., 2009)

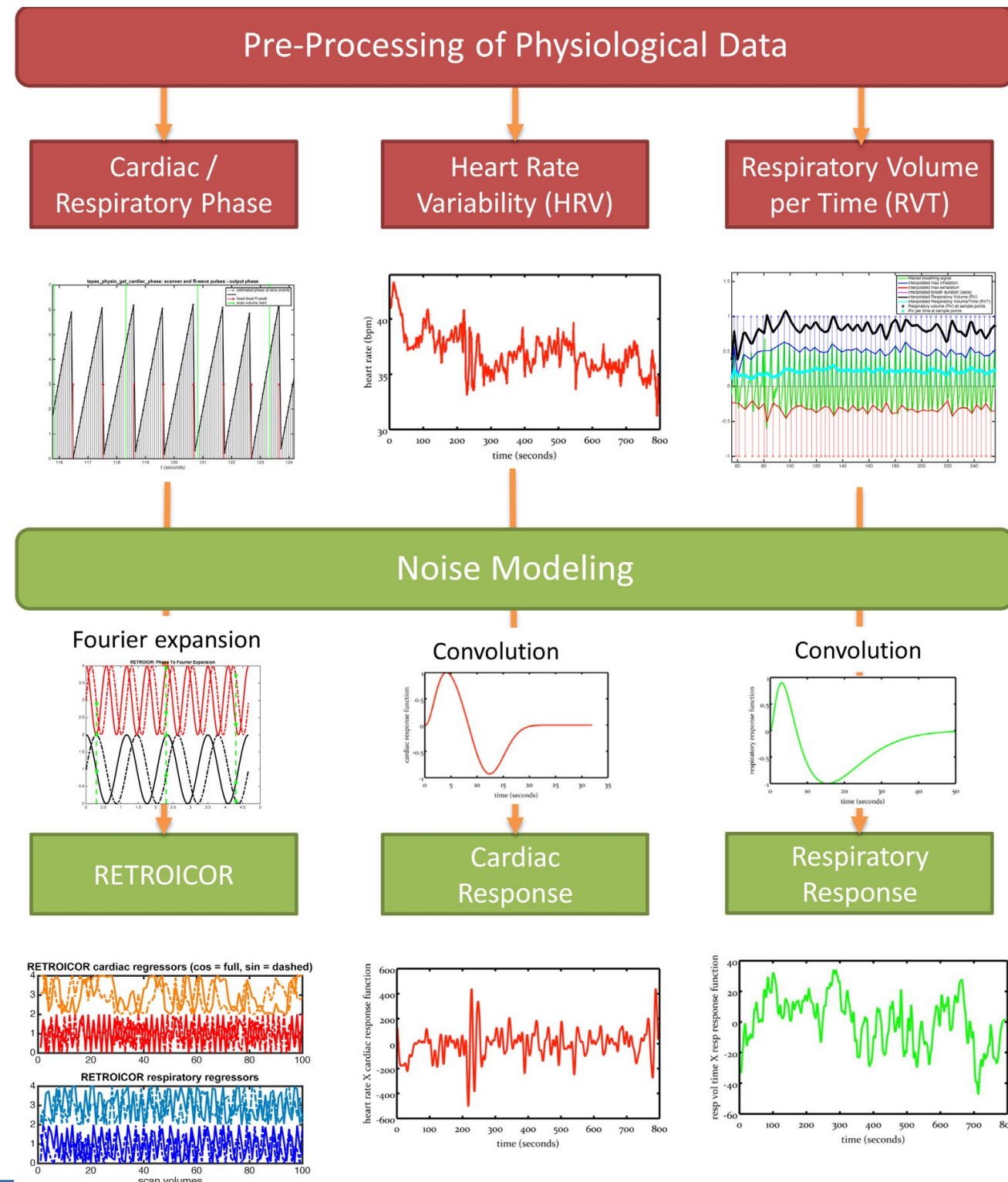
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
- ## 2/ Nuisance regressors (RETROICOR, HRV, RVT)

TAPAS Physio Toolbox

The PhysIO Toolbox for Modeling Physiological Noise in fMRI Data
Kasper & al.

J of Neuroscience Methods 276 (2017) 56–72



Denoising physiological-related noise

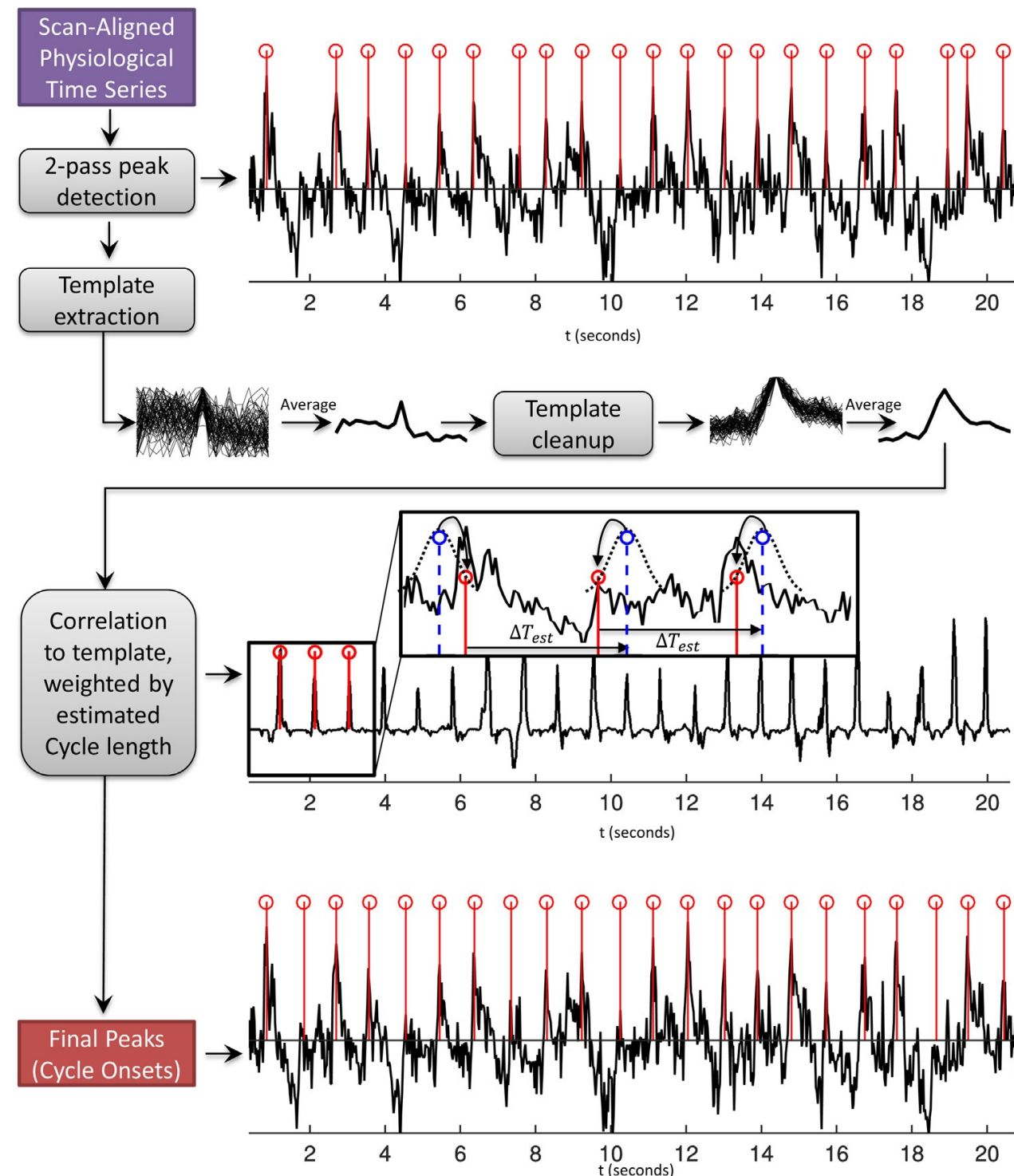
- Denoising physiological noise based on external recordings

1/ Physiological Peak Detection Algorithm

TAPAS Physio Toolbox

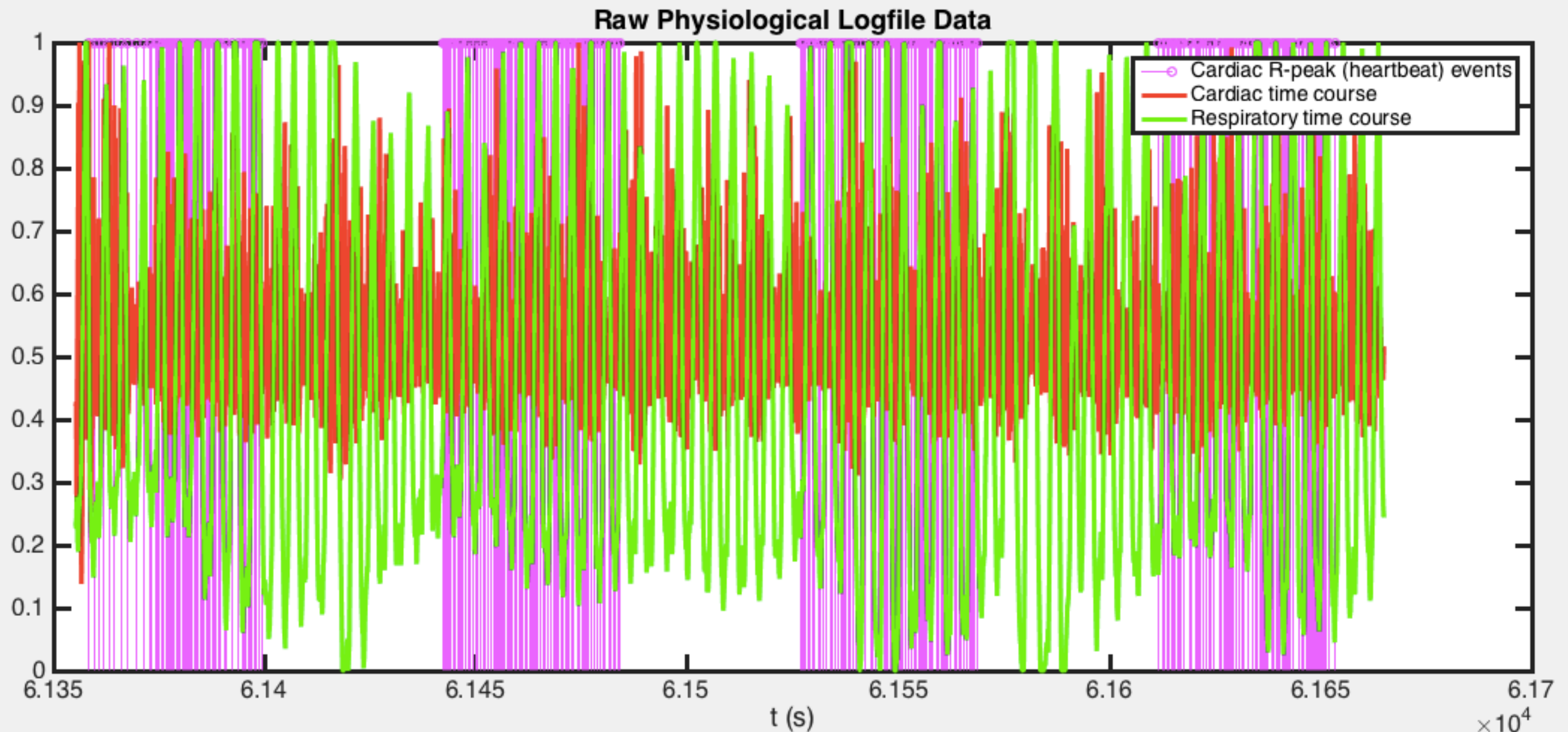
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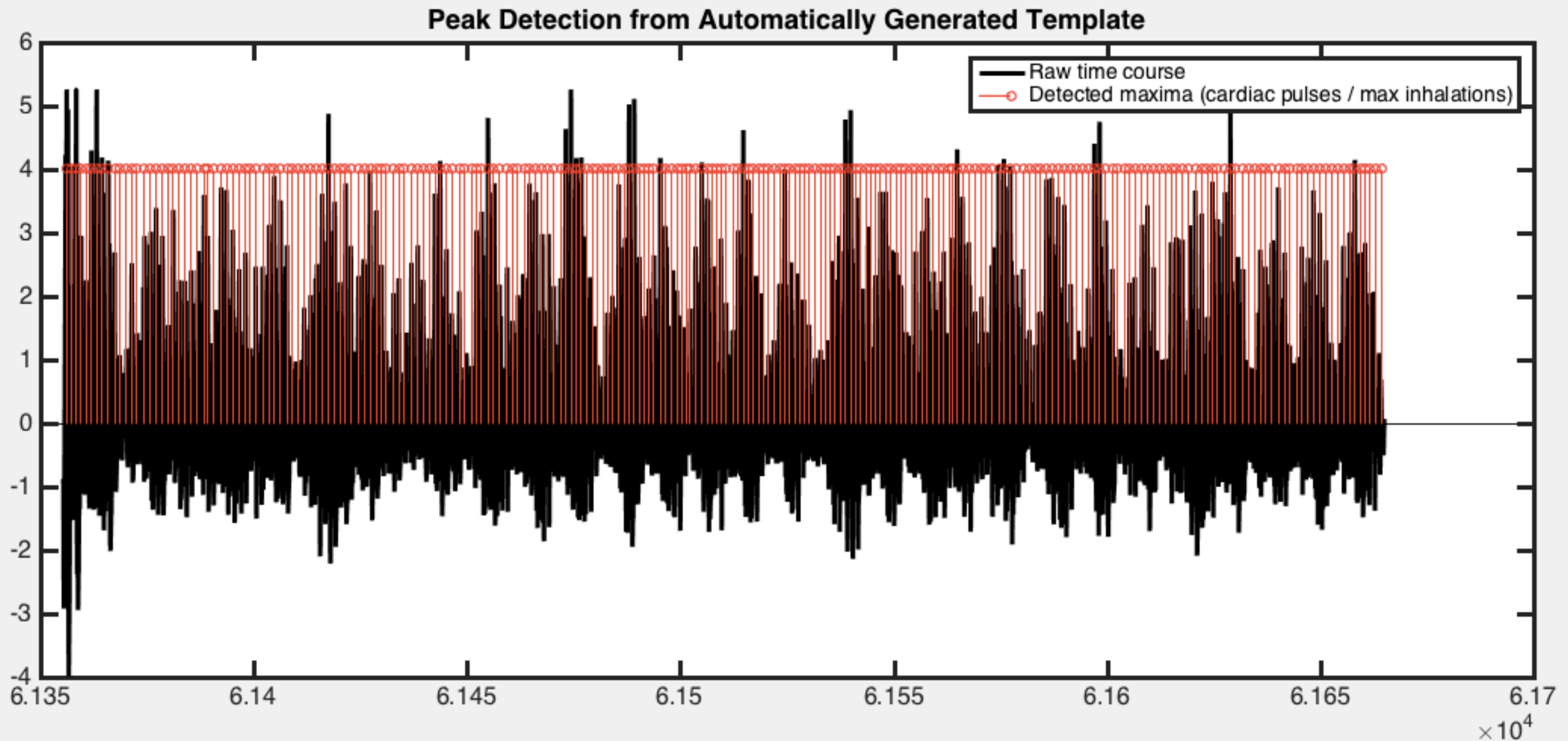
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
 - 1/ Preprocessing of physiological data



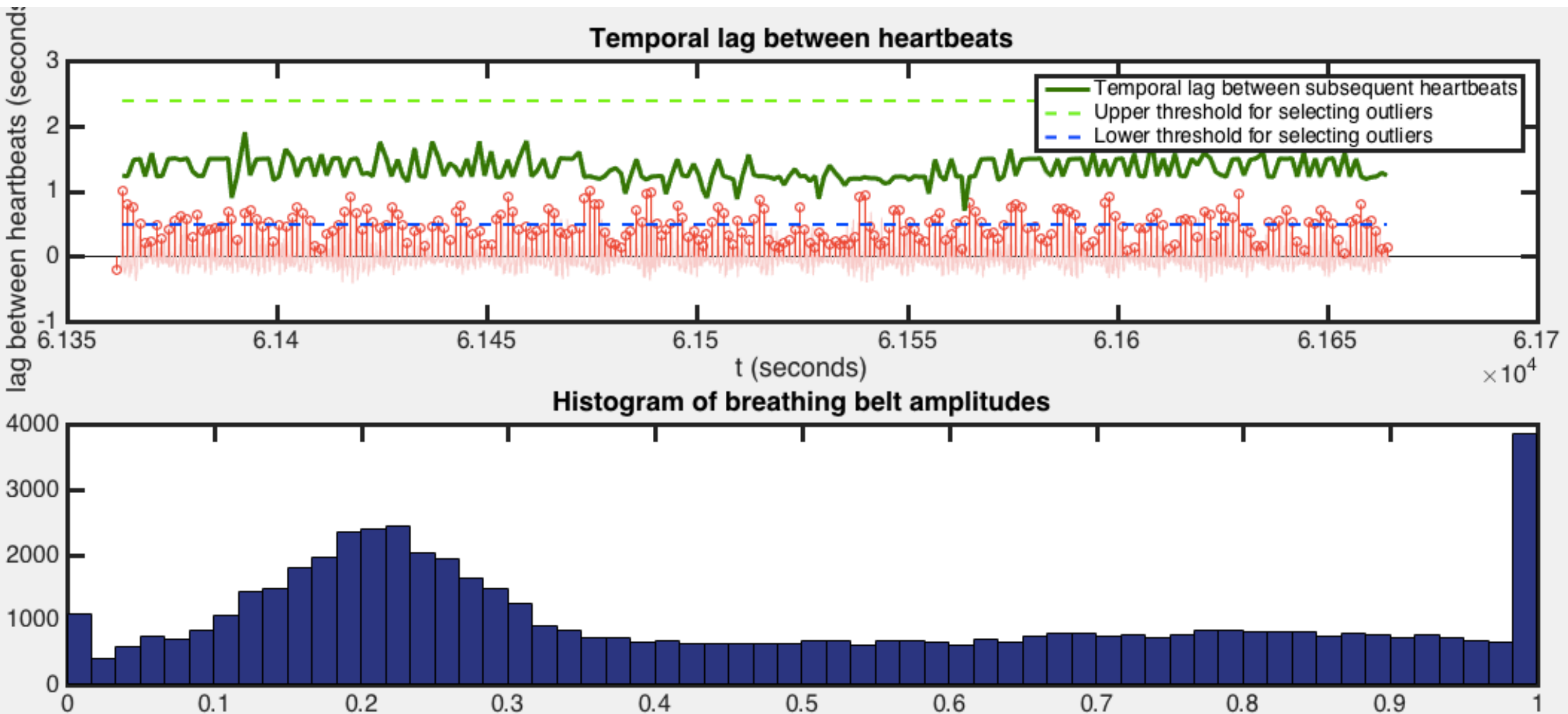
Denoising physiological-related noise

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Denoising physiological-related noise

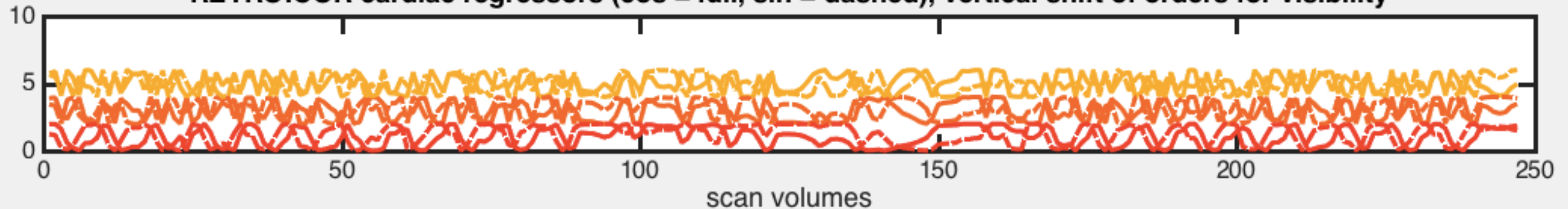
- Denoising physiological noise based on external recordings
 - 1/ Preprocessing of physiological data



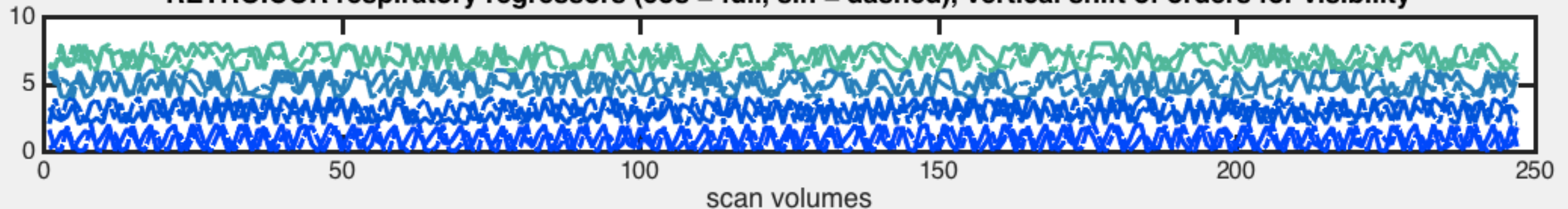
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
2/ Nuisance regressors : RETROICOR

RETROICOR cardiac regressors (cos = full, sin = dashed), vertical shift of orders for visibility



RETROICOR respiratory regressors (cos = full, sin = dashed), vertical shift of orders for visibility

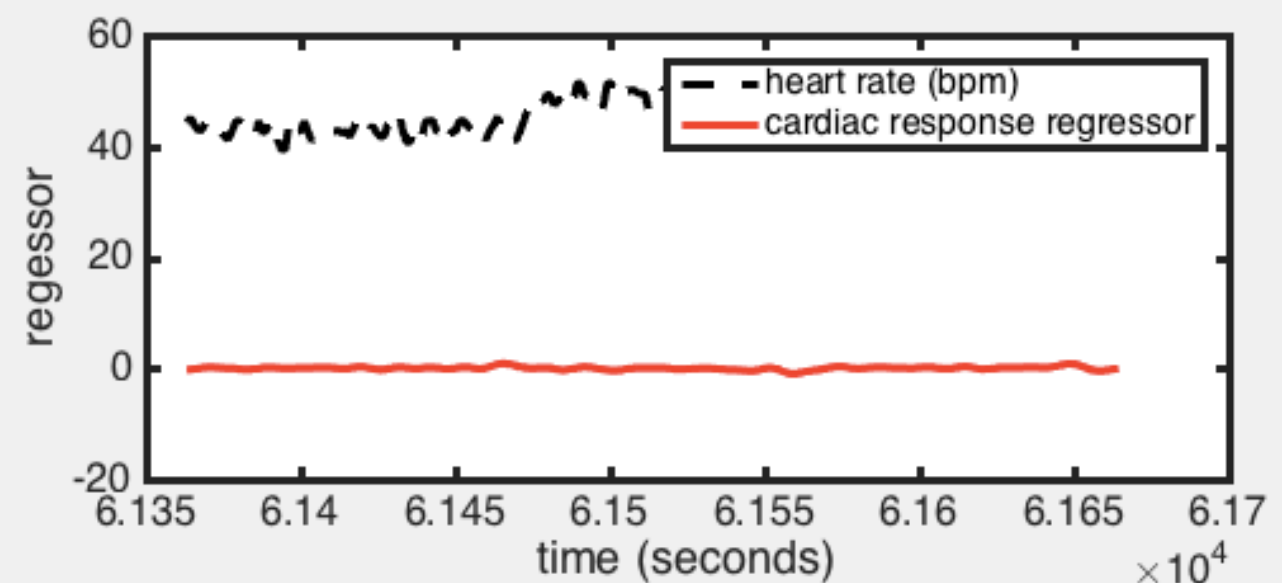
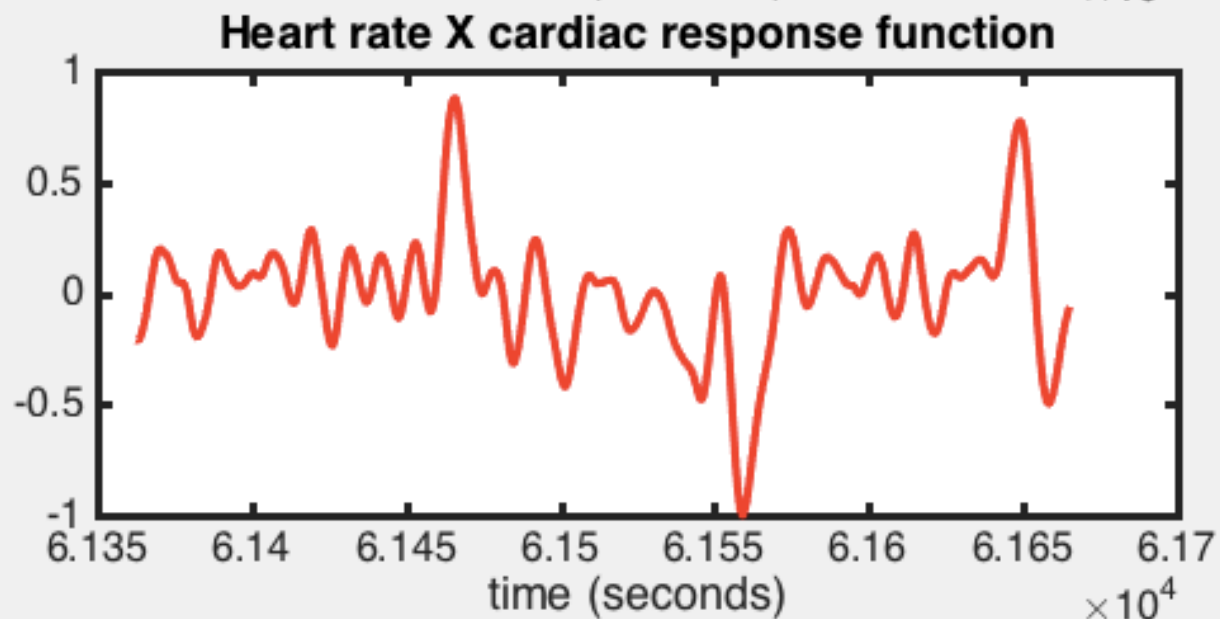
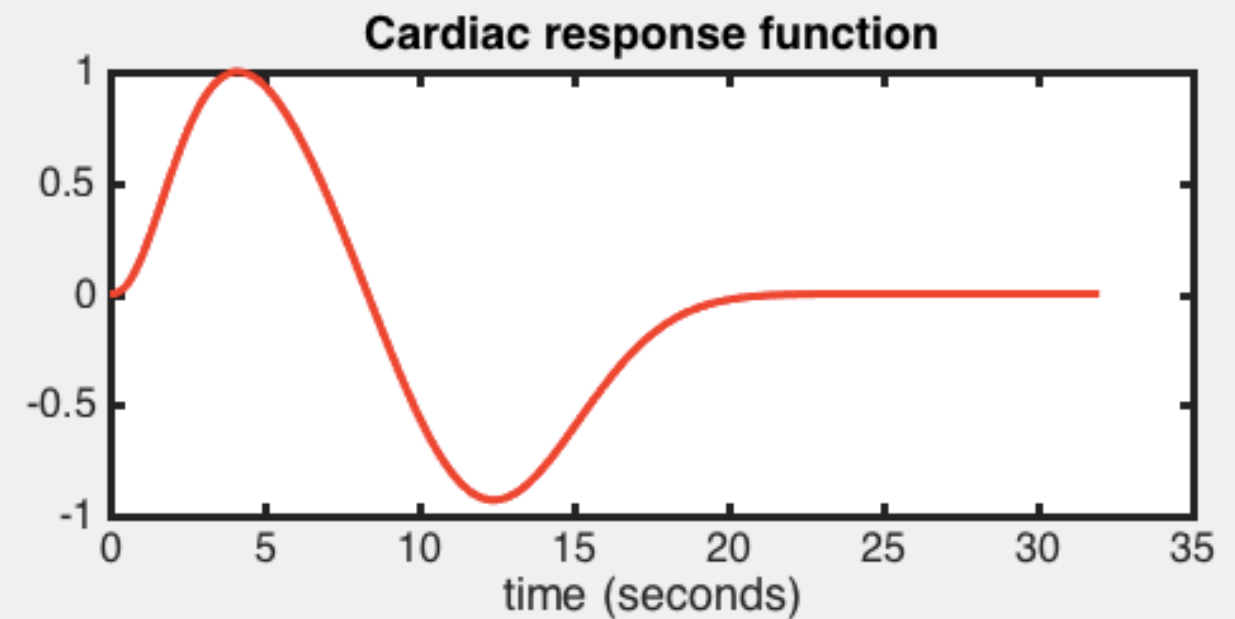
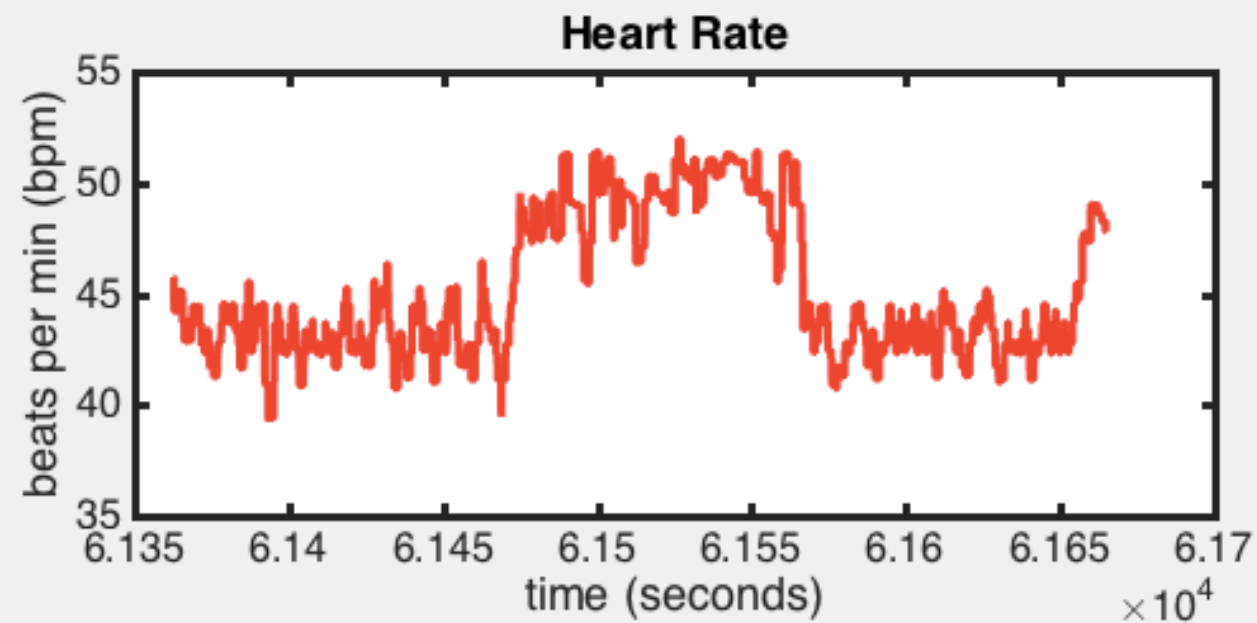


RETROICOR multiplicative cardiac x respiratory regressors, vertical shift for visibility



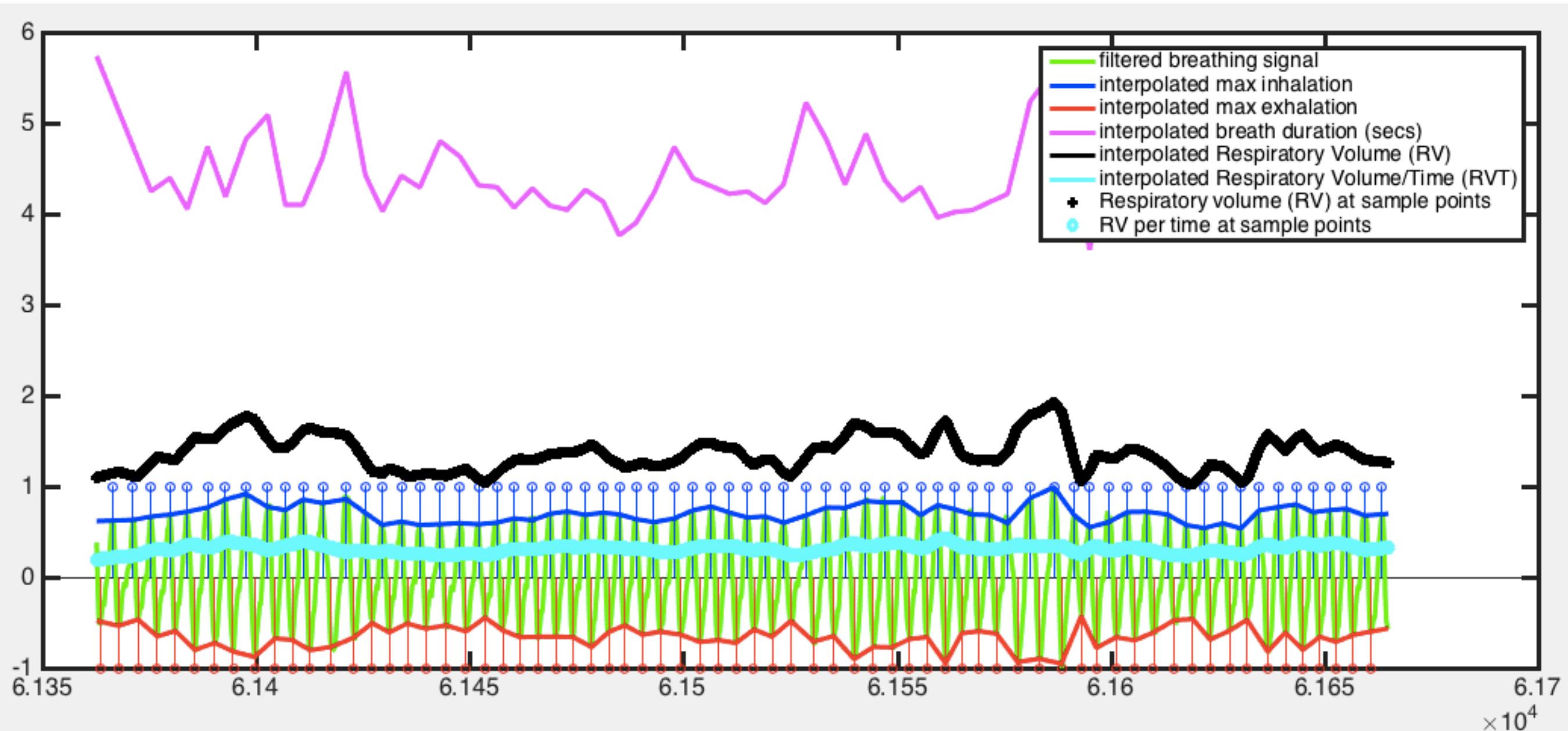
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
2/ Nuisance regressors : HRV x CRF



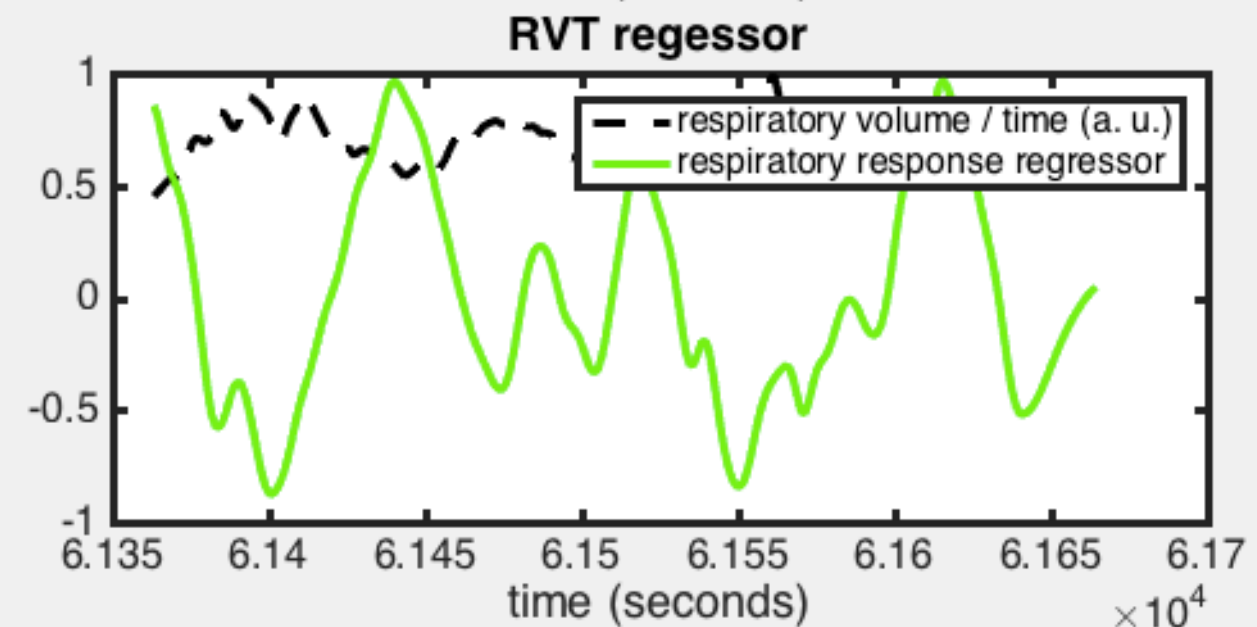
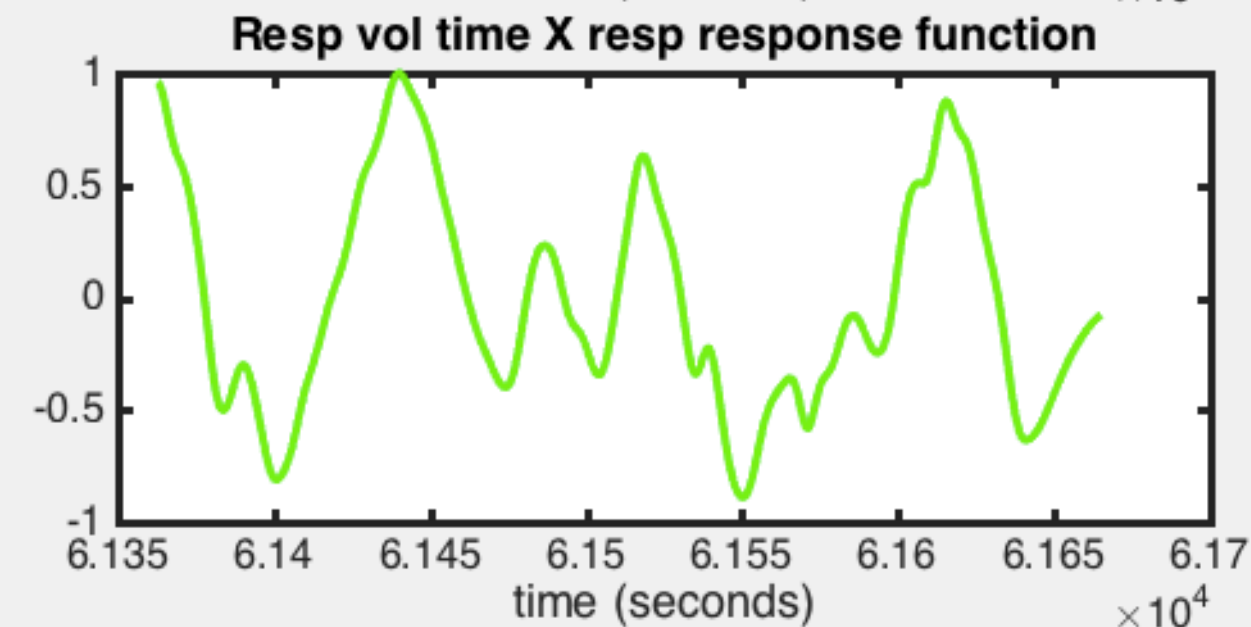
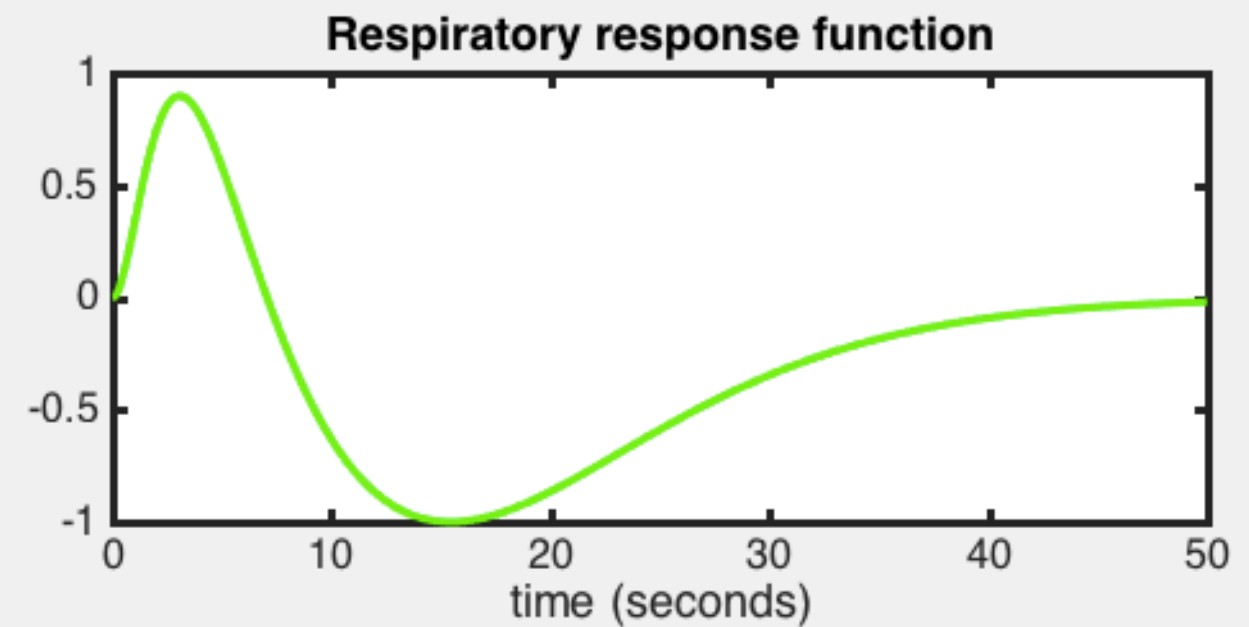
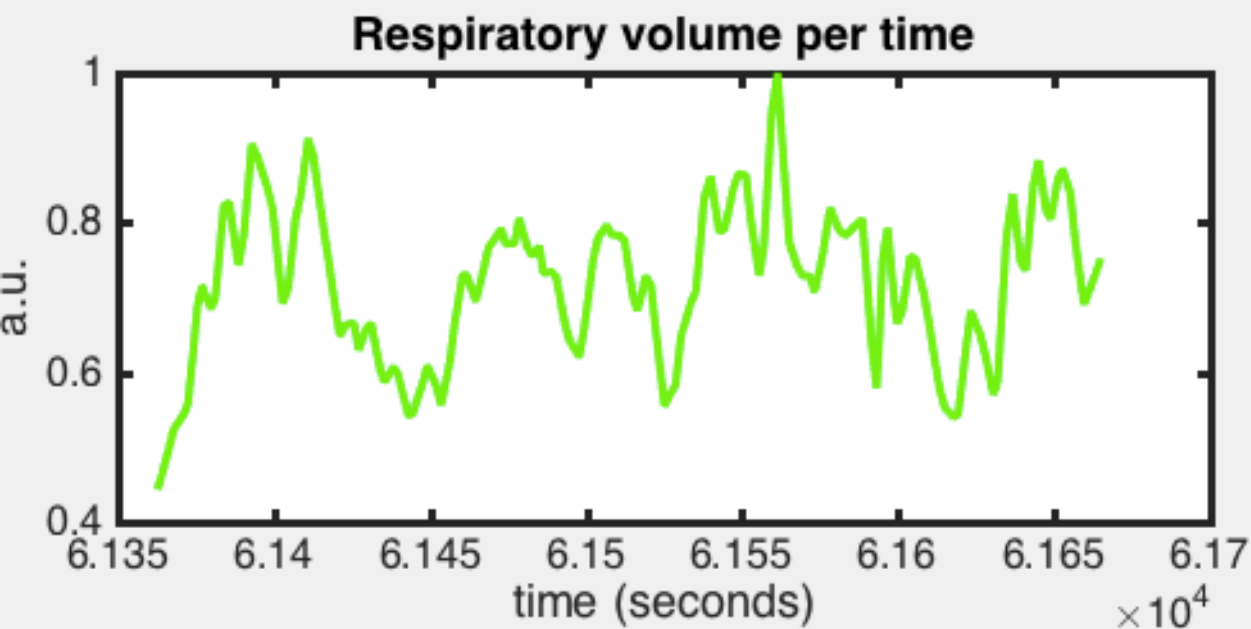
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
2/ Respiratory Volume per Time (RVT)



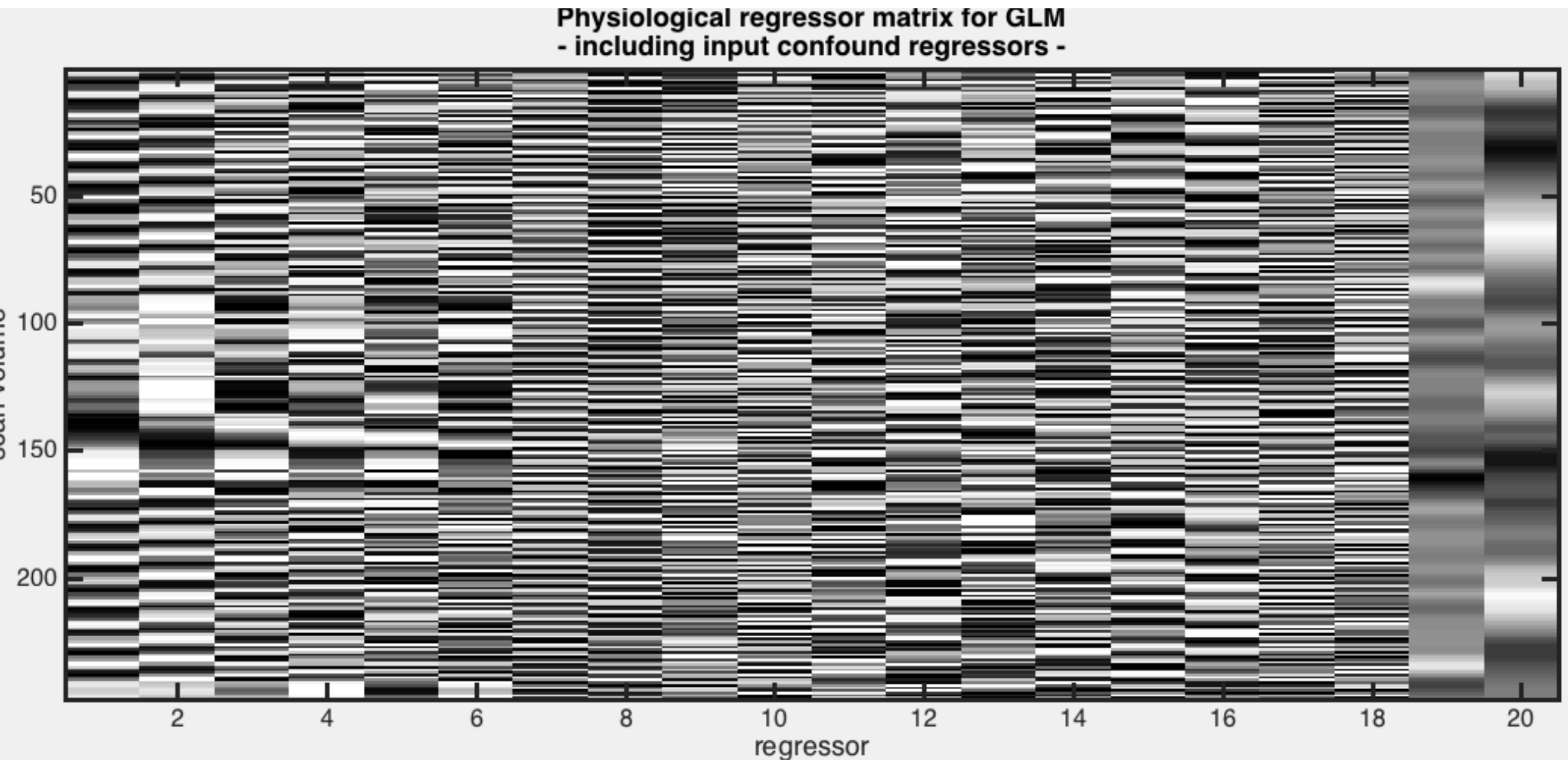
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
2/ Nuisance regressors : RVT x RRF



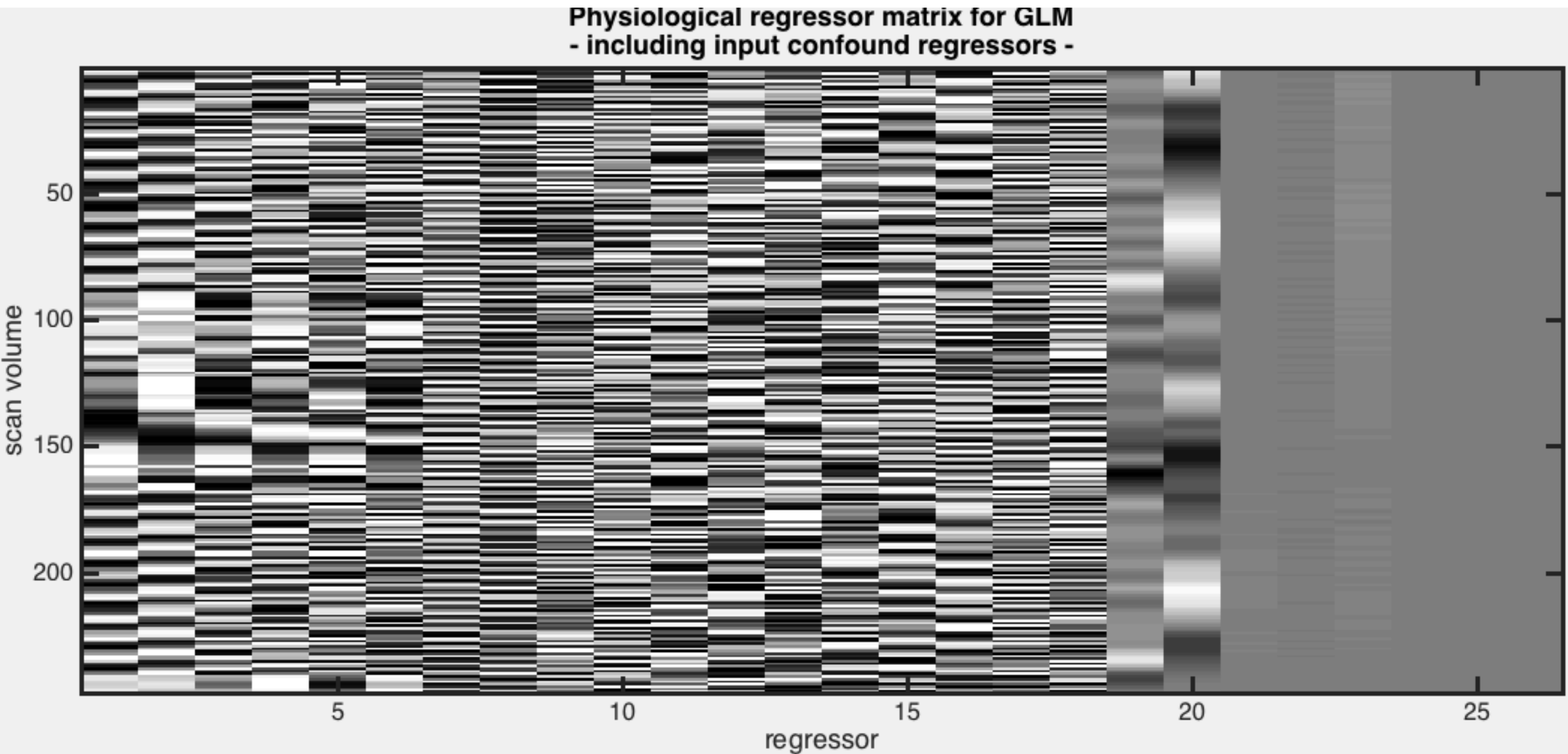
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
2/ Nuisance regressors (RETROICOR, HRV, RVT)



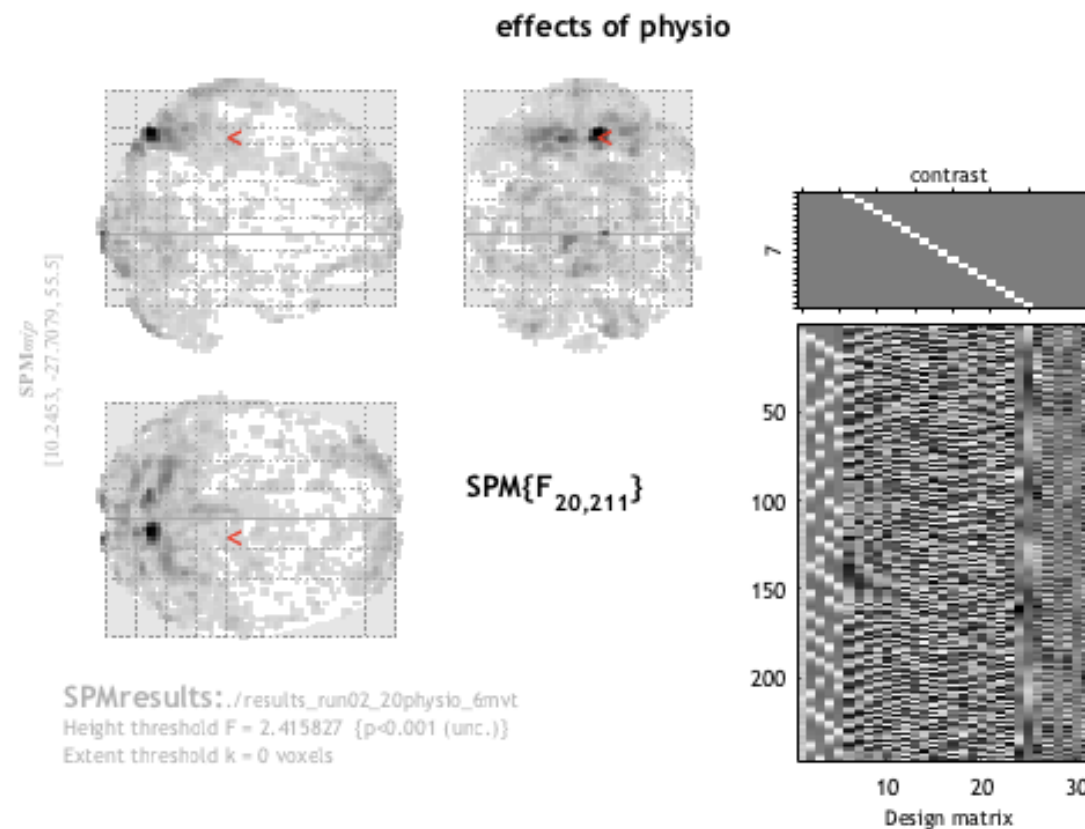
Denoising physiological-related noise

- Denoising physiological noise based on external recordings
2/ Nuisance regressors (RETROICOR, HRV, RVT) + 6 mvts

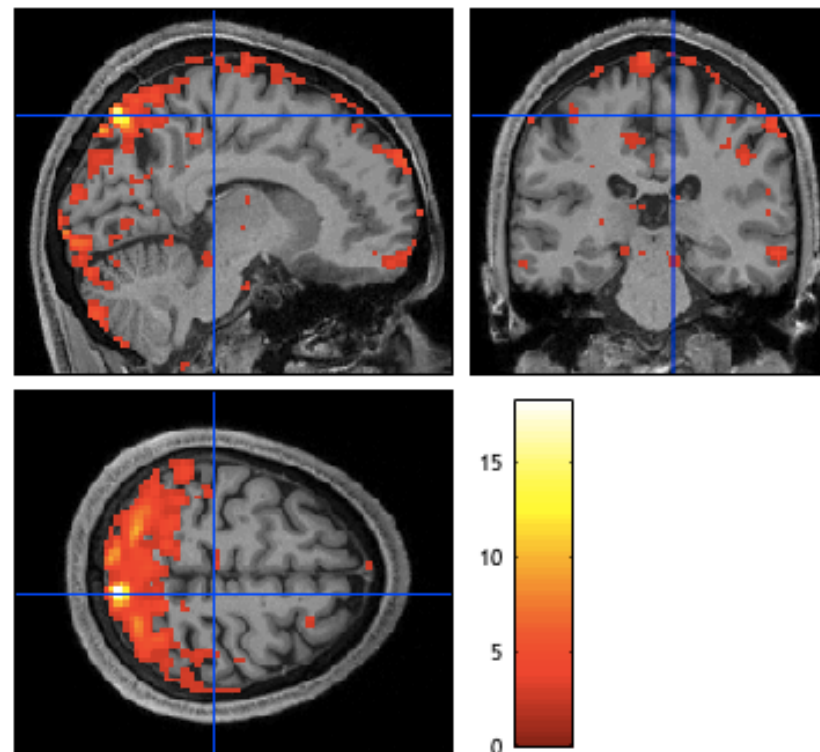


Denoising physiological-related noise

- Denoising physiological noise based on external recordings

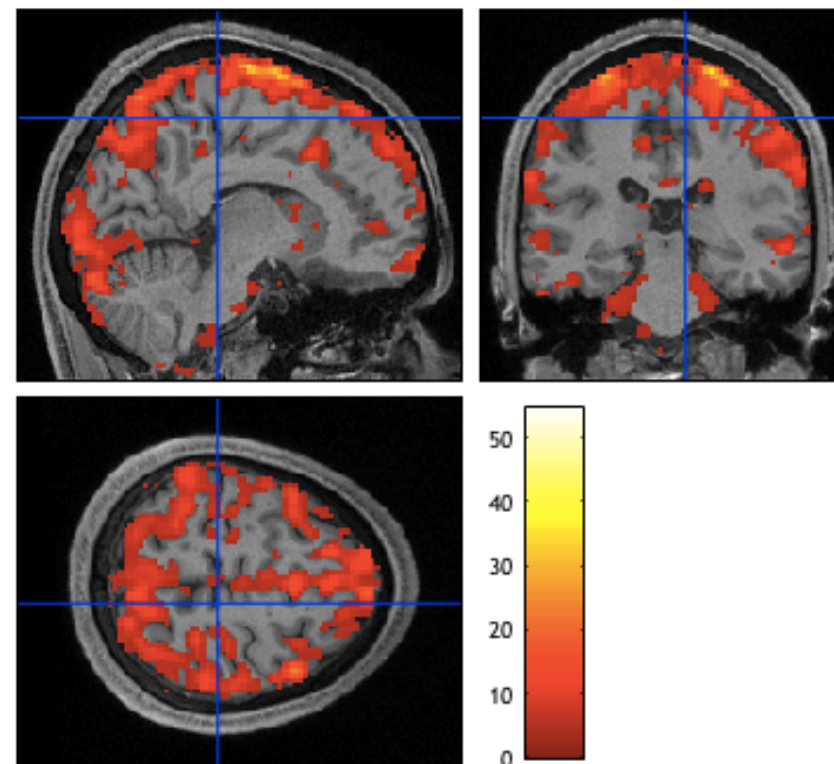
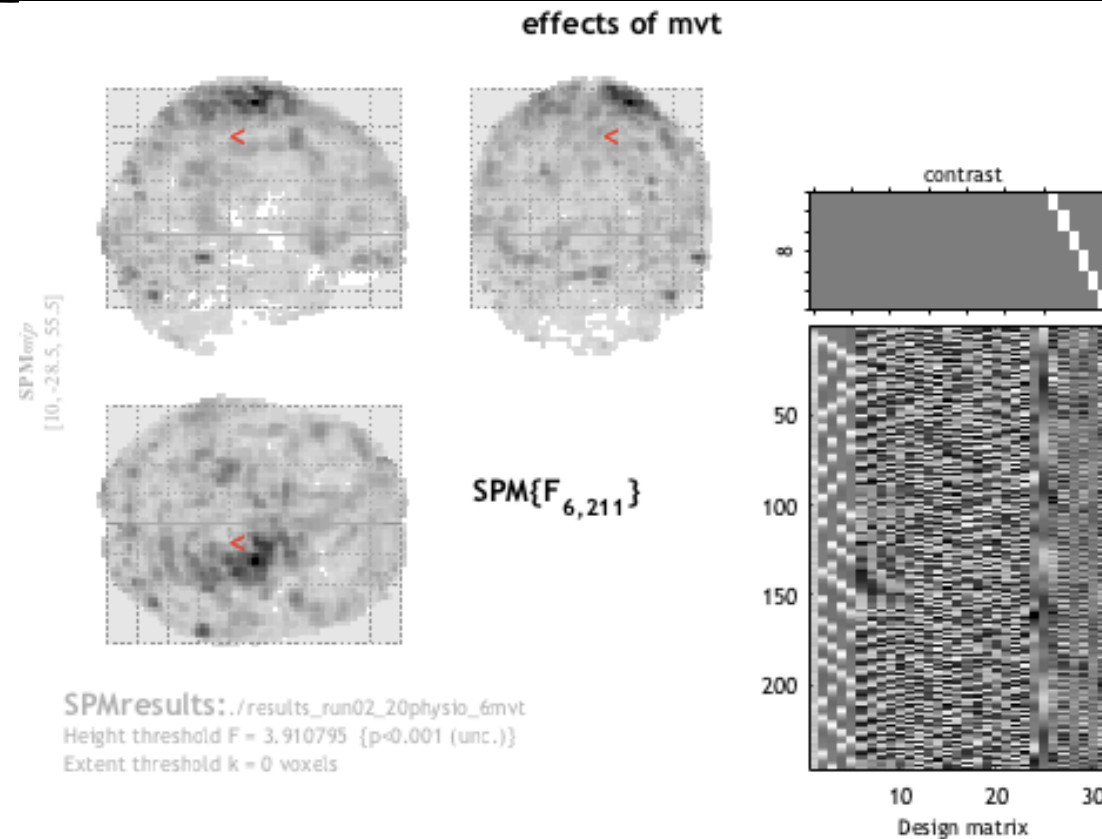


Effects of physio
nuisance regressors



Denoising physiological-related noise

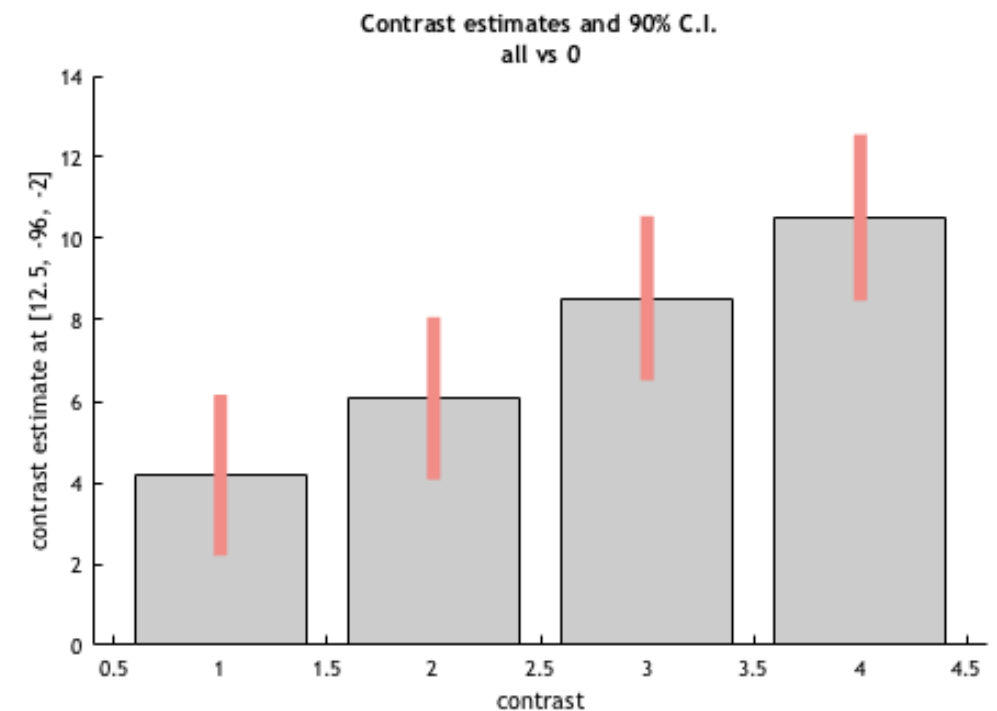
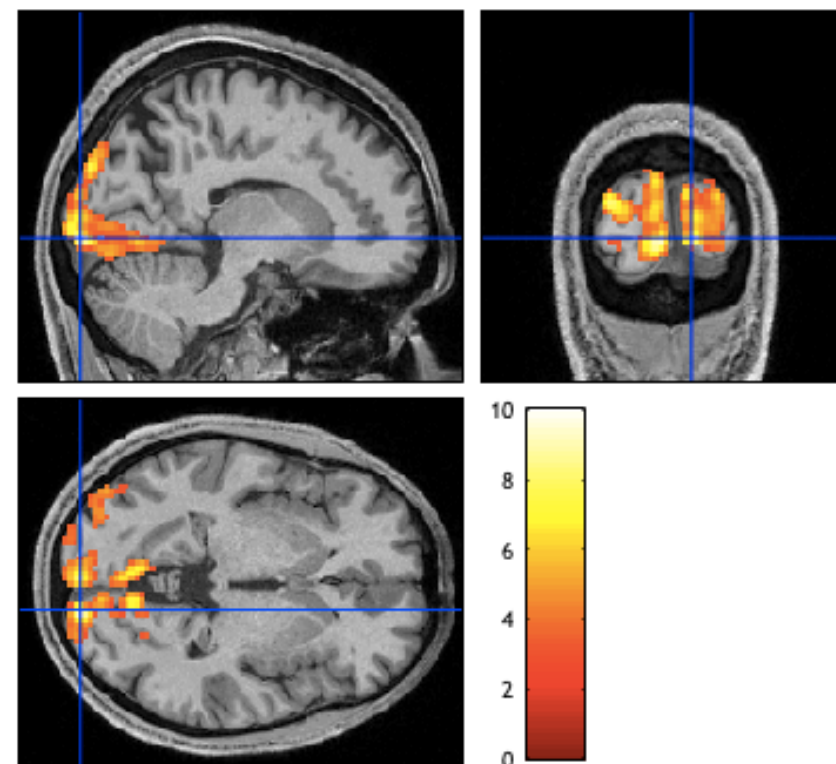
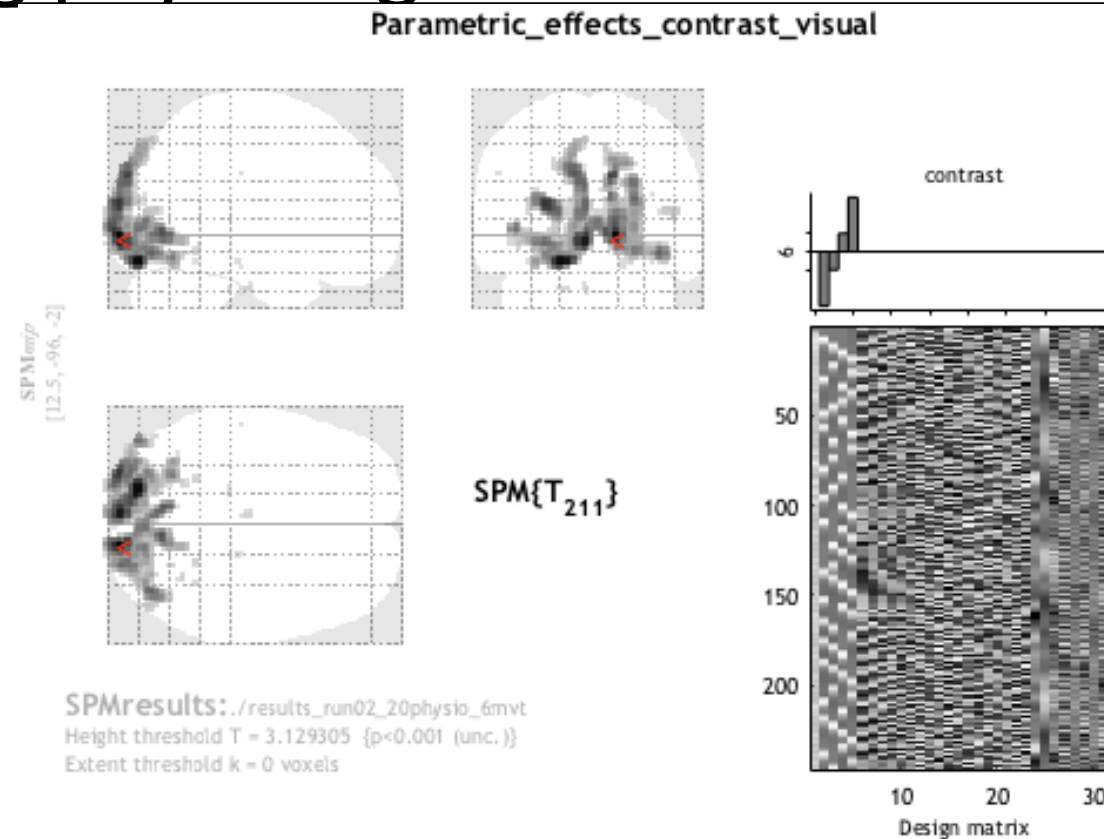
- Denoising physiological noise based on external recordings



Effects of movement parameters

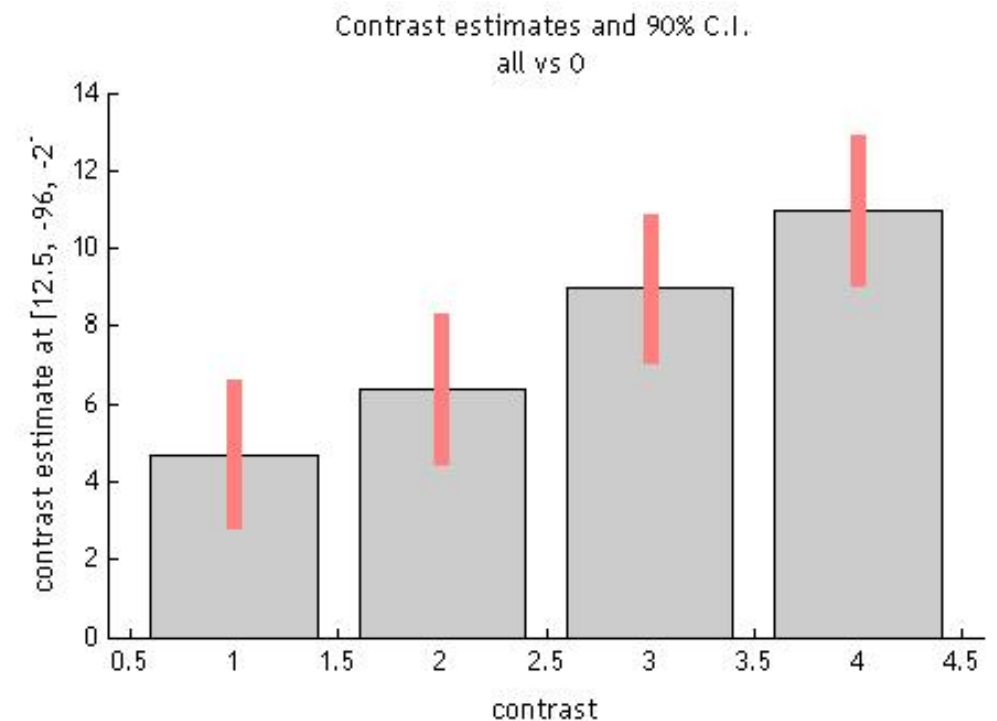
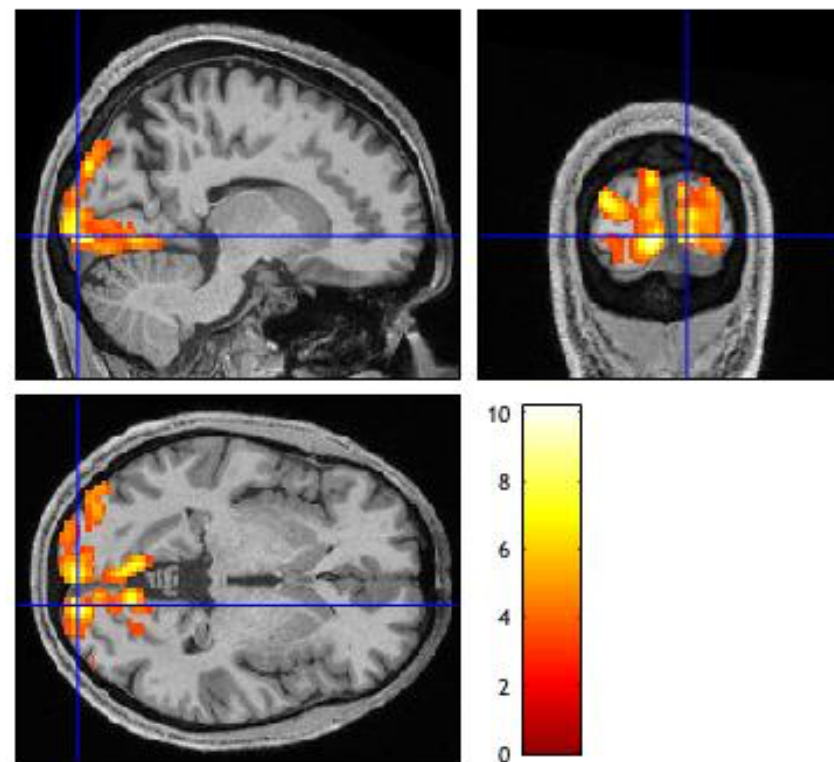
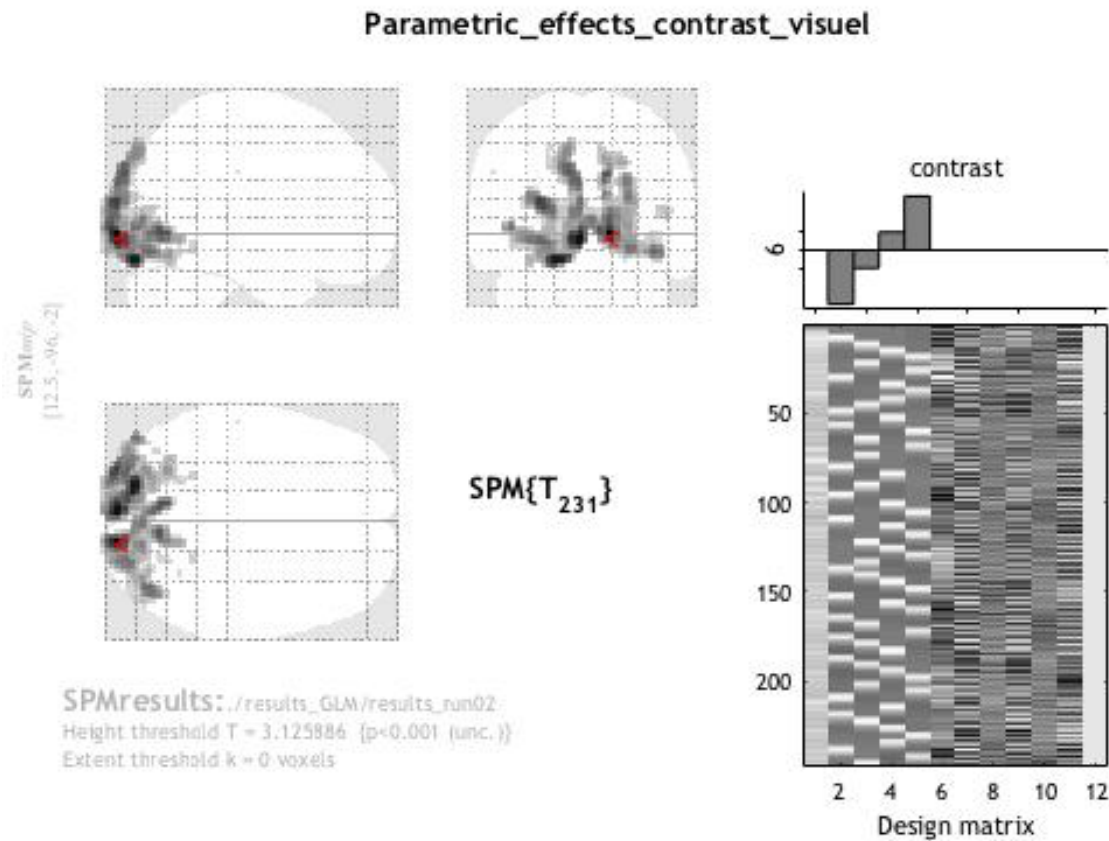
Denoising physiological-related noise

- Denoising physiological noise based on external recordings



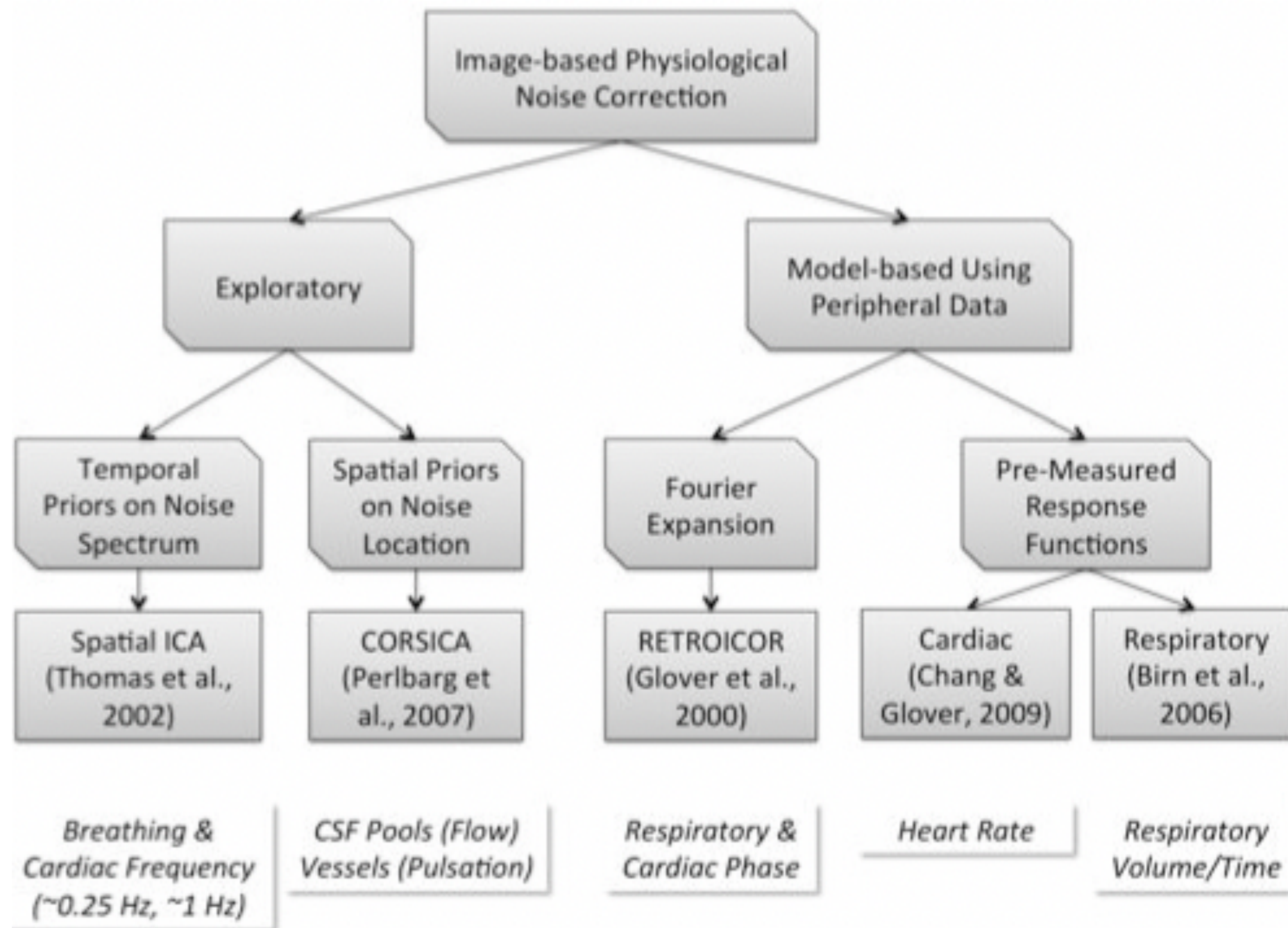
Denoising physiological-related noise

- « Good » subject \approx identical than without physio denoising



Denoising physiological-related noise

- Denoising physiological noise based on external recordings
- Data-driven denoising methods of physiological noise



Denoising physiological-related noise

- Data-driven denoising methods of physiological noise
 - based on **Principal Component Analysis (PCA)** of noise regions signals : white matter (WM) & Cerebro-Spinal Fluid (CSF)
 - CompCor (Behzadi et al., 2007)
 - based on **Independent Component Analysis (ICA)**
 - temporal ICA : PESTICA (Beall and Lowe, 2007)
 - spatial ICA : CORSICA (Perlberg & al, 2007)
 - spatial ICA : ICA-AROMA (Pruim & al, 2015) & FIX-ICA (Salimi-Khorshidi & al, 2014) : available in FSL

→ **Determine nuisance regressors for the GLM analysis**

Denoising physiological-related noise

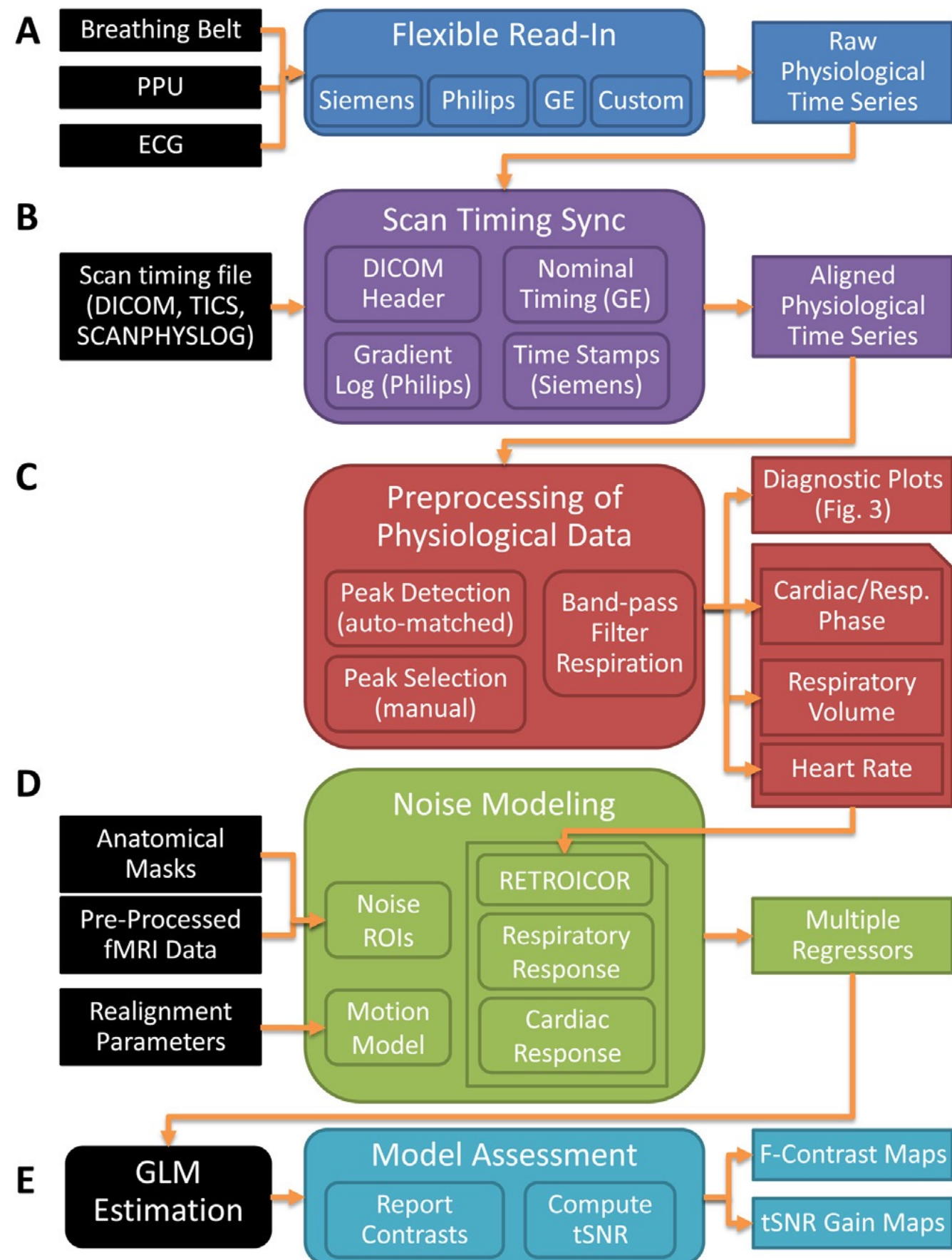
- Data-driven denoising methods of physiological noise
Based on Principal Component Analysis (PCA)
- Selection of noise regions signals :
 - Thresholding the tissues volume fraction map (at 0.99)
 - Performing a map erosion by two pixels
→ minimizing the effect of partial voluming with other tissue types.
- Extraction of EPI non-smoothed data in the noise regions
- Principal Component Analysis (PCA) on these EPI data

Denoising motion & physiological-related noise

TAPAS Physio Toolbox

The PhysIO Toolbox for Modeling
Physiological Noise in fMRI Data
Kasper & al.

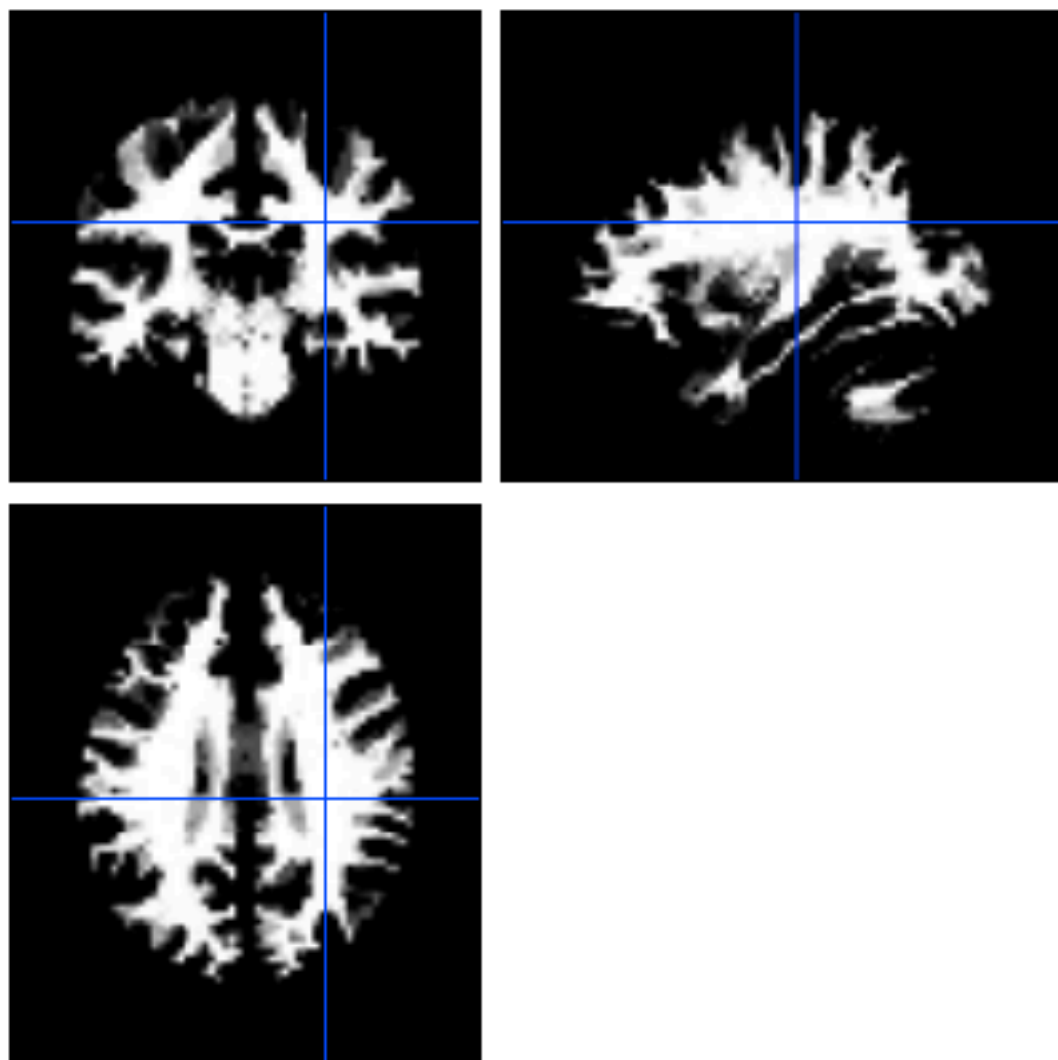
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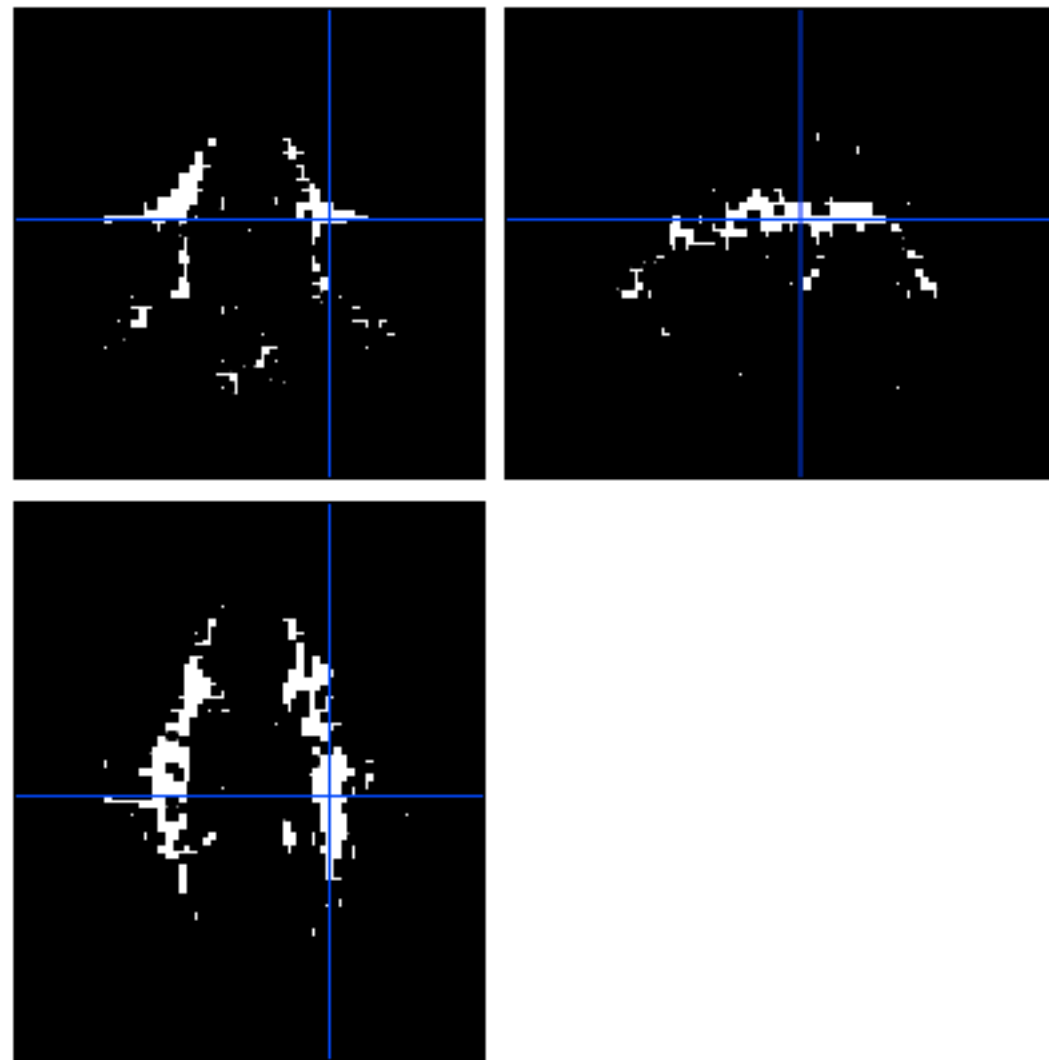
Denoising motion & physiological-related noise

- Masks/tissue probability maps characterizing where noise resides : ROI 1

White Matter



White Matter (thresholded & cropped)

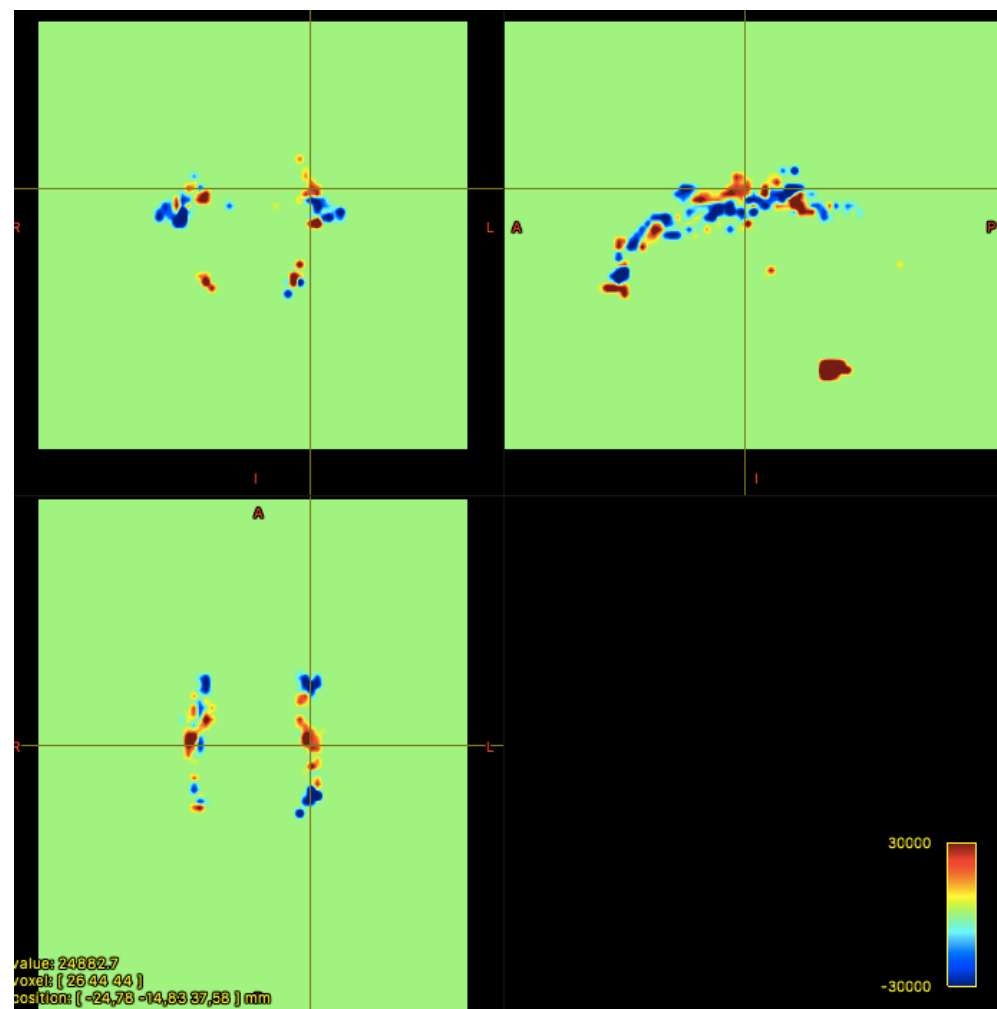


Denoising motion & physiological-related noise

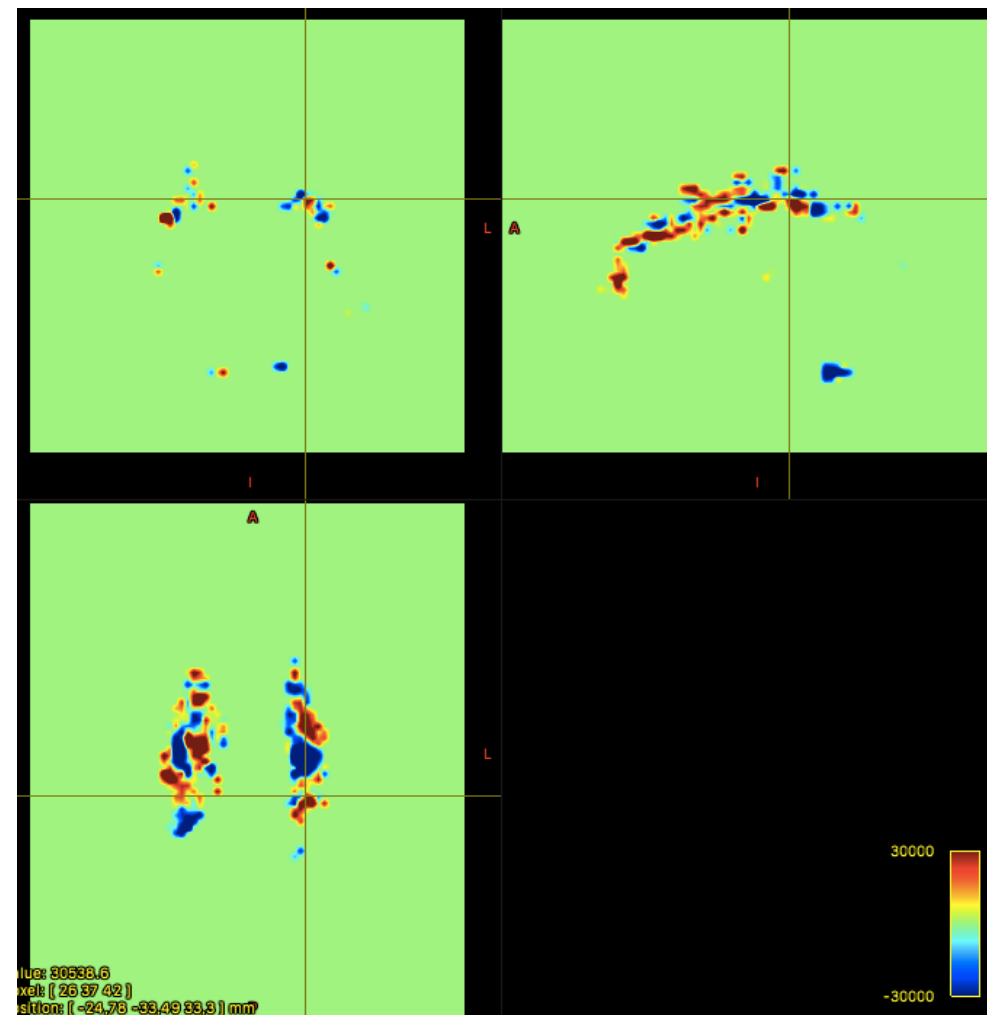
- Principal Component Analysis (PCA) of non-smoothed EPI data in WM (thresholded & cropped)

→ N Principal Spatial Components in WM

PC 1



PC 2

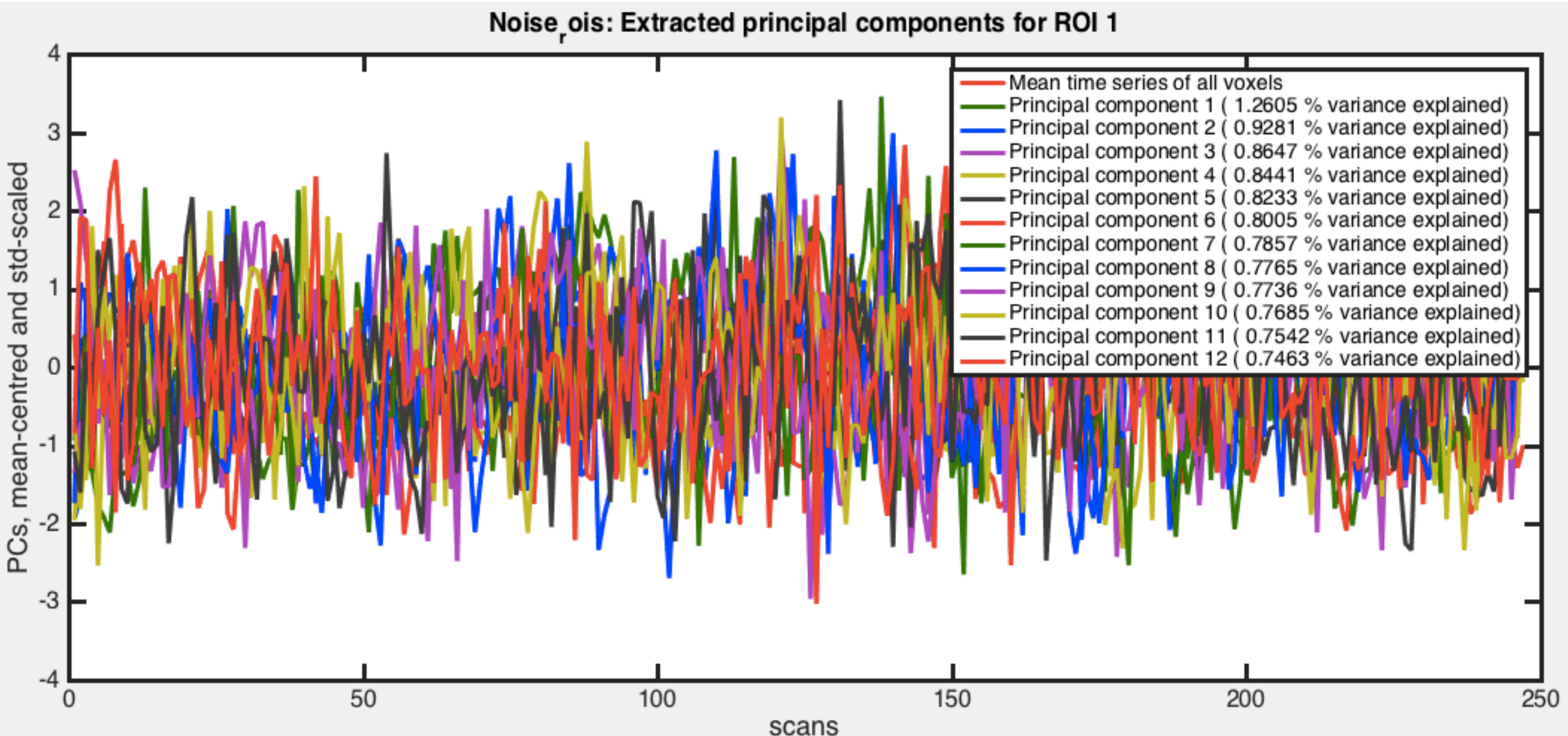


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Denoising motion & physiological-related noise

- Principal Component Analysis (PCA) of non-smoothed EPI data in WM (thresholded & cropped)

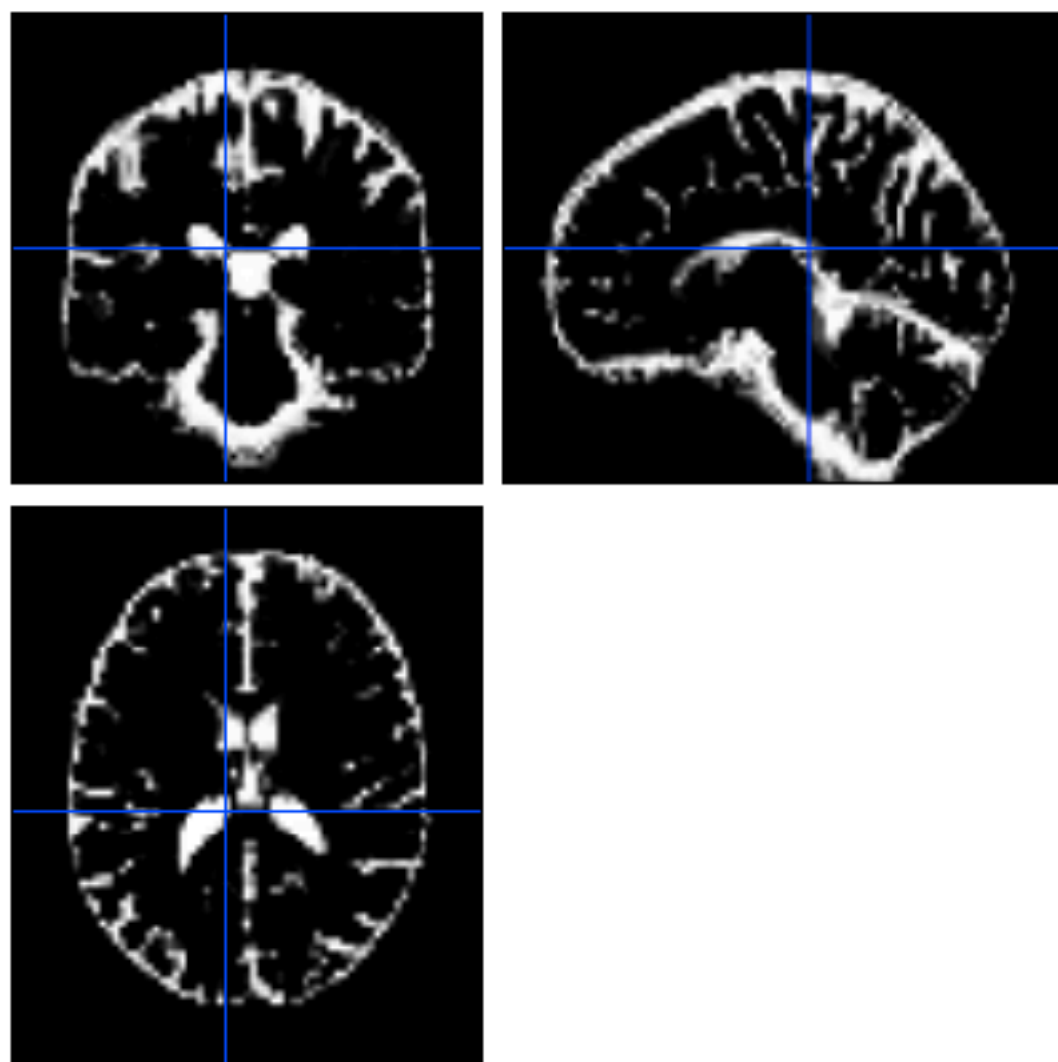
→ N Temporal Components : nuisance regressors



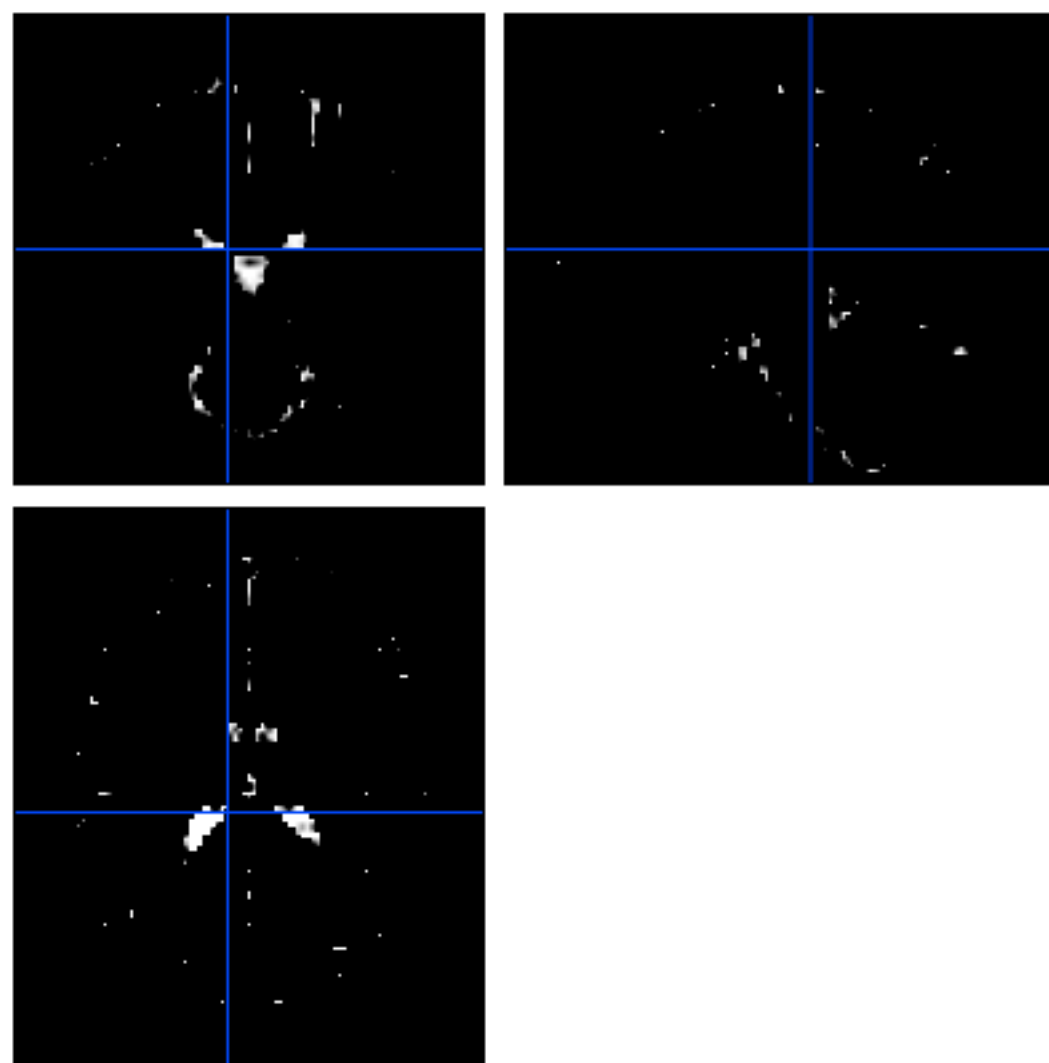
Denoising motion & physiological-related noise

- Masks/tissue probability maps characterizing where noise resides : ROI 2

Cerebro-Spinal Fluid (CSF)



CSF (thresholded)



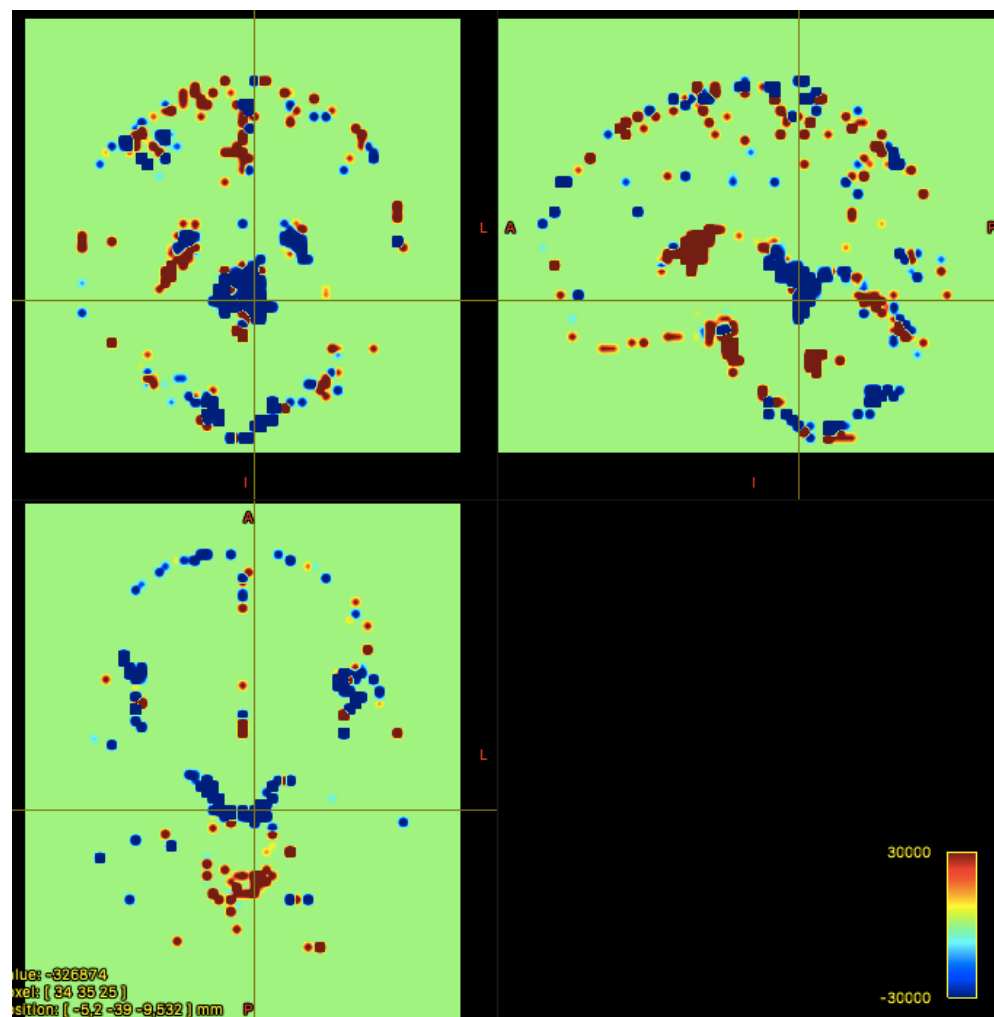
Denoising motion & physiological-related noise

- Principal Component Analysis (PCA) of non-smoothed EPI data in CSF

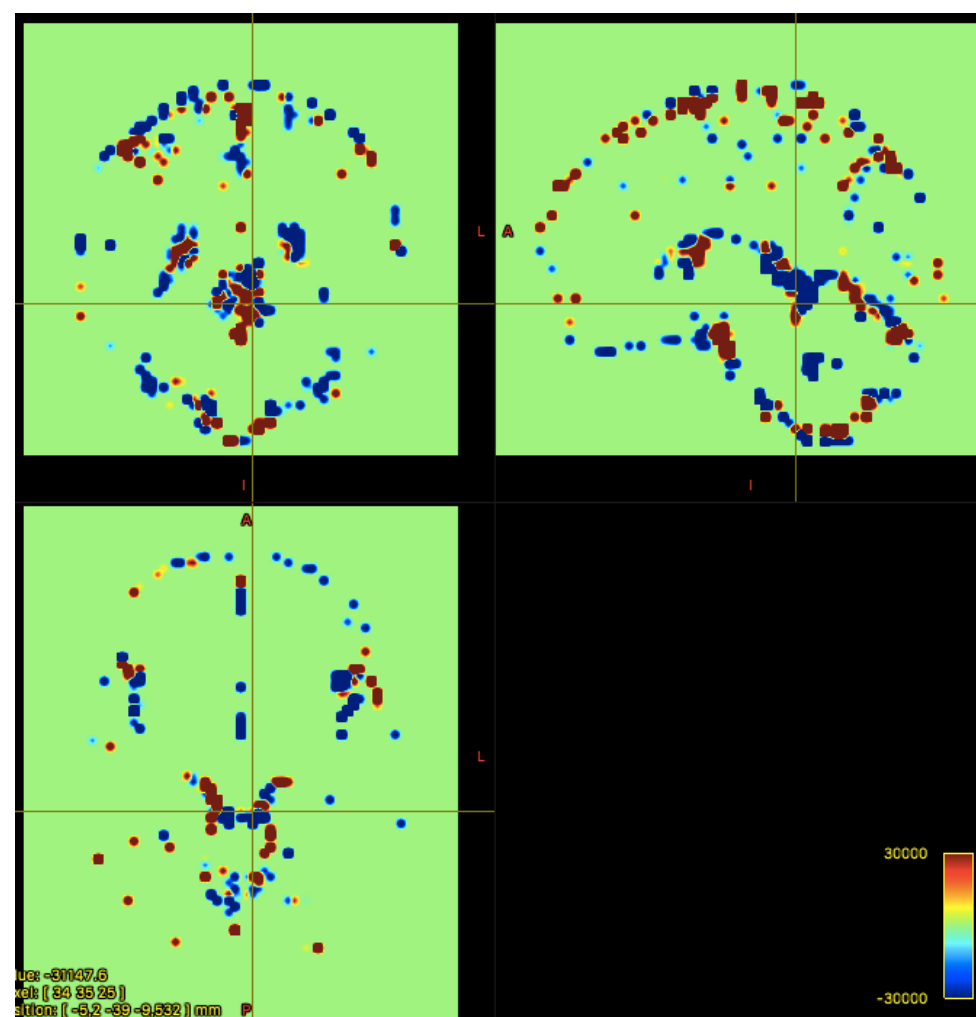
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→ N Principal Spatial Components in CSF

PC 1



PC 2

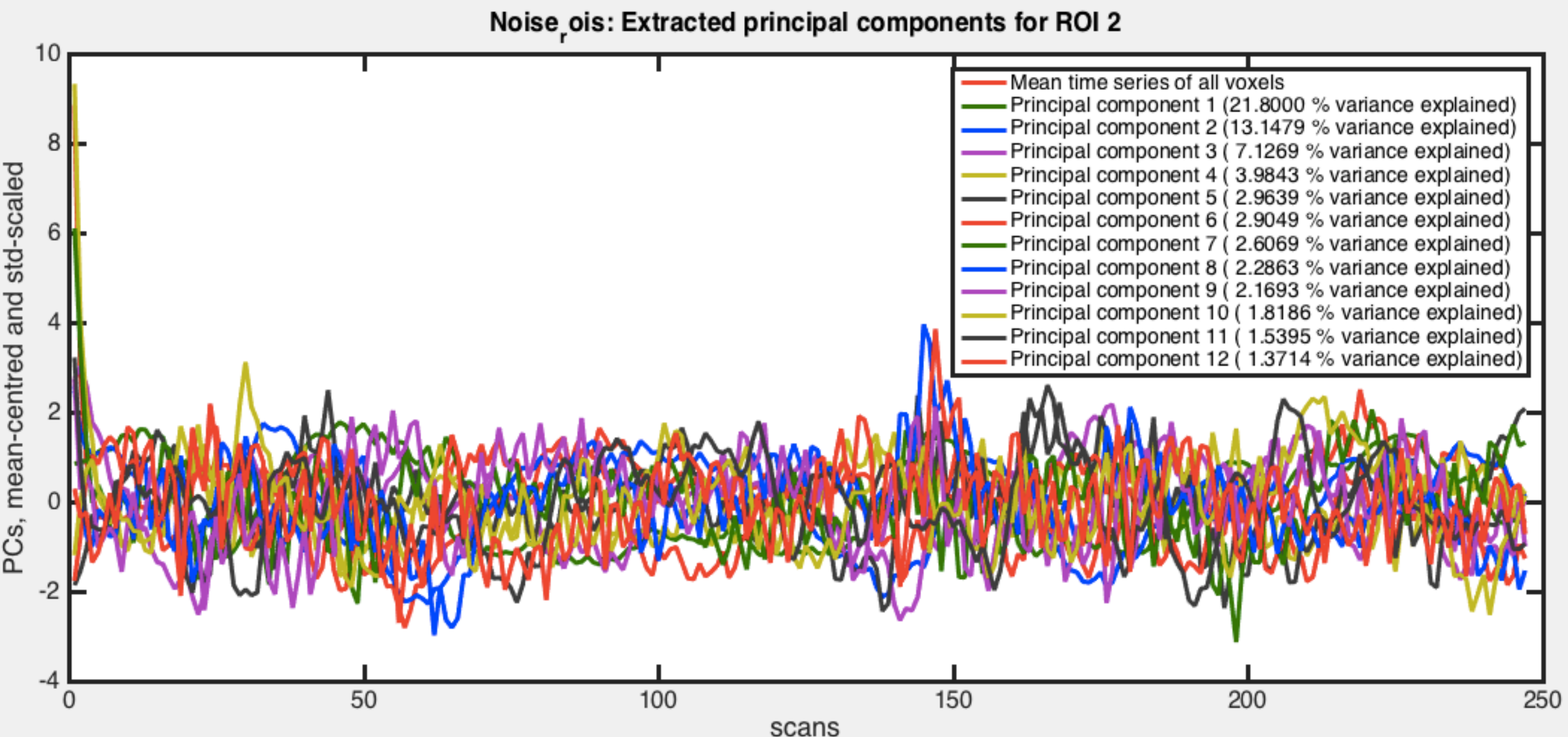


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Denoising motion & physiological-related noise

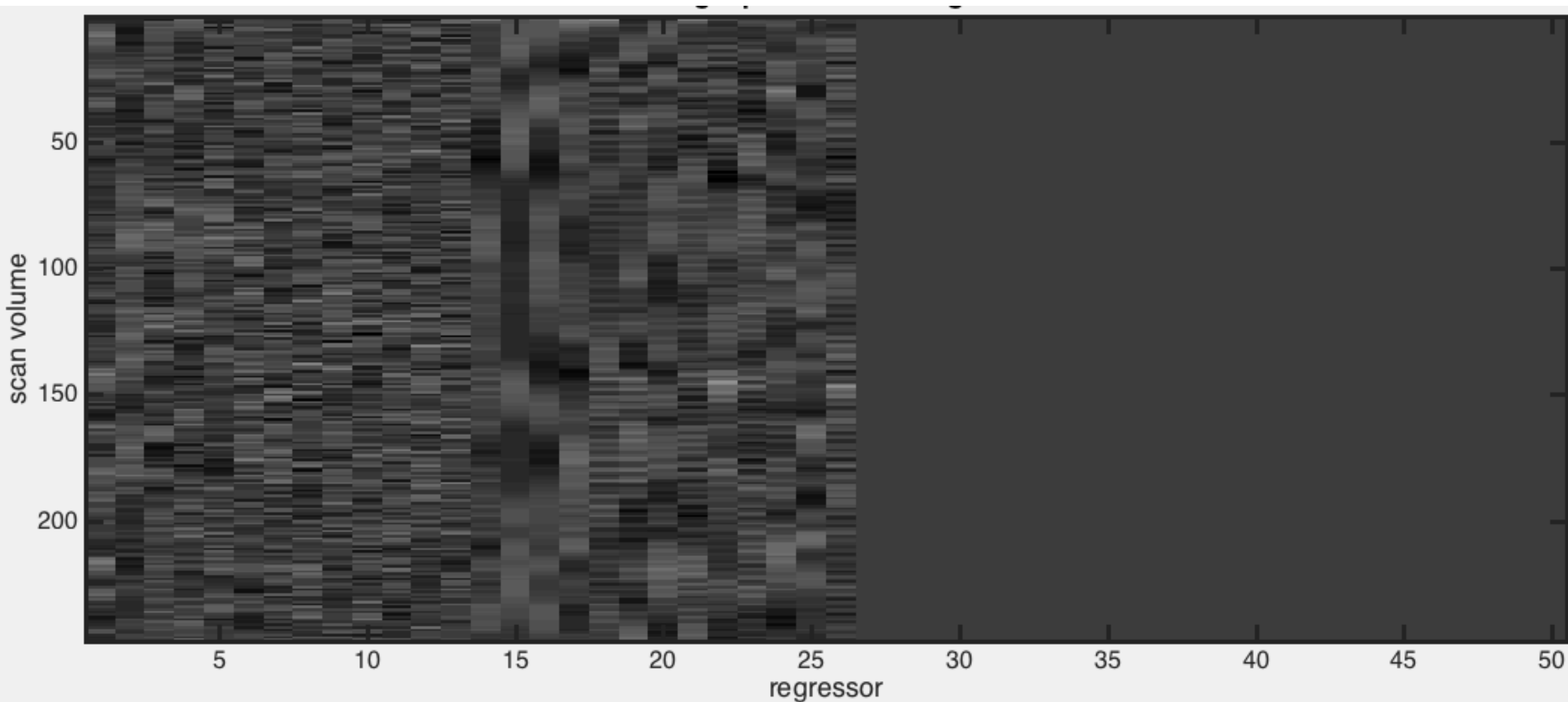
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→ N Temporal Components : nuisance regressors



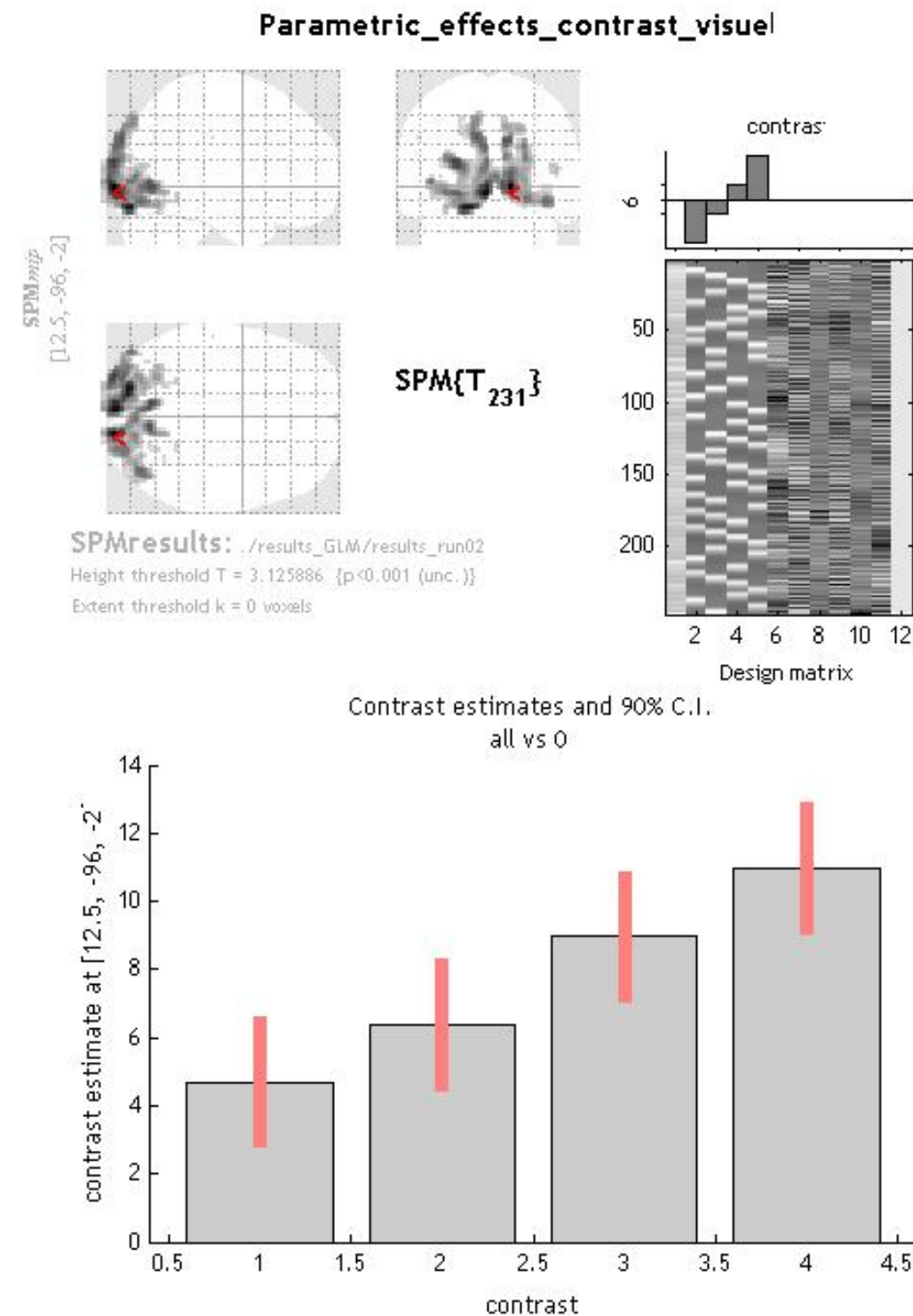
Denoising motion & physiological-related noise

- 12 PCs + 1 mean for WM, 12 PCs + 1 mean for CSF, 24 movement parameters



Denoising motion & physiological-related noise

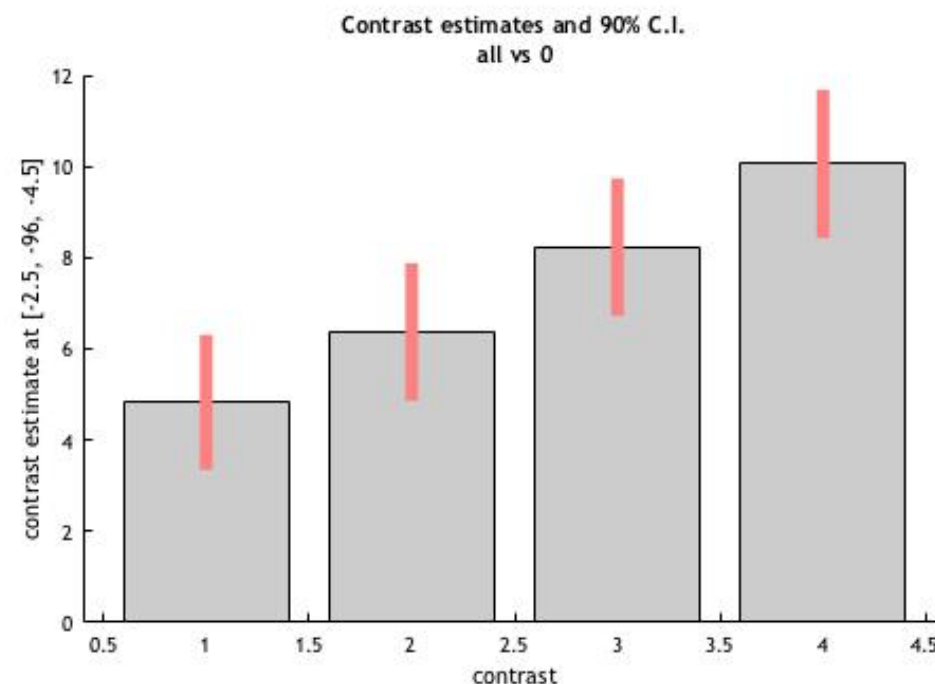
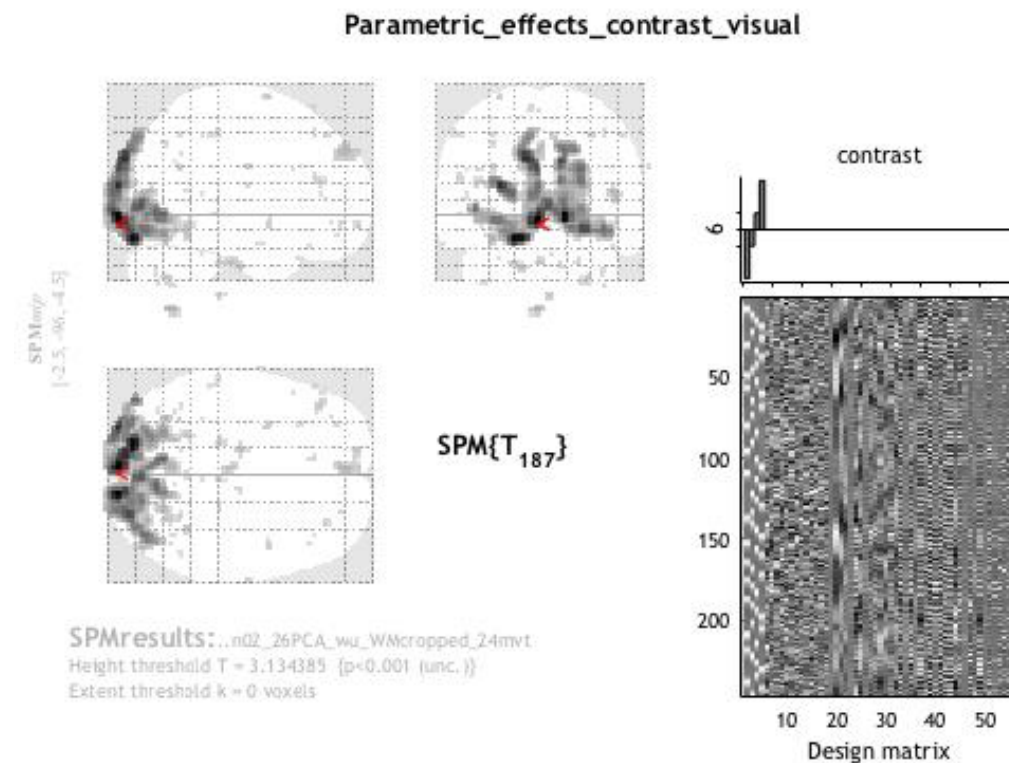
- Only 6 realign parameters



→ T max = 10.18

Denoising motion & physiological-related noise

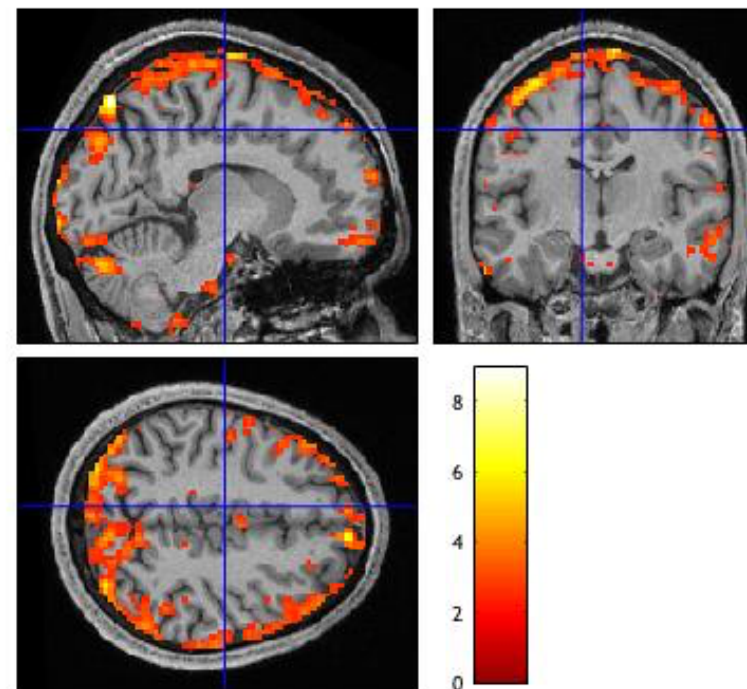
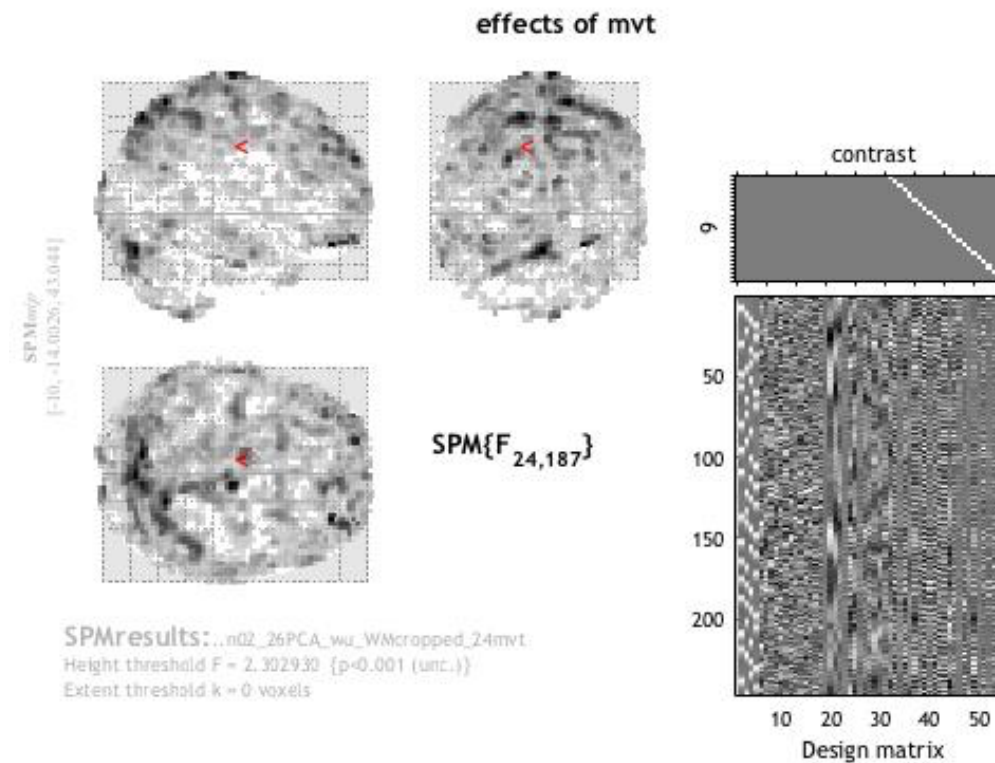
- 12 PCs + 1 mean for WM, 12 PCs + 1 mean for CSF, 24 movement parameters



→ $T_{\max} = 11.65$

Denoising motion & physiological-related noise

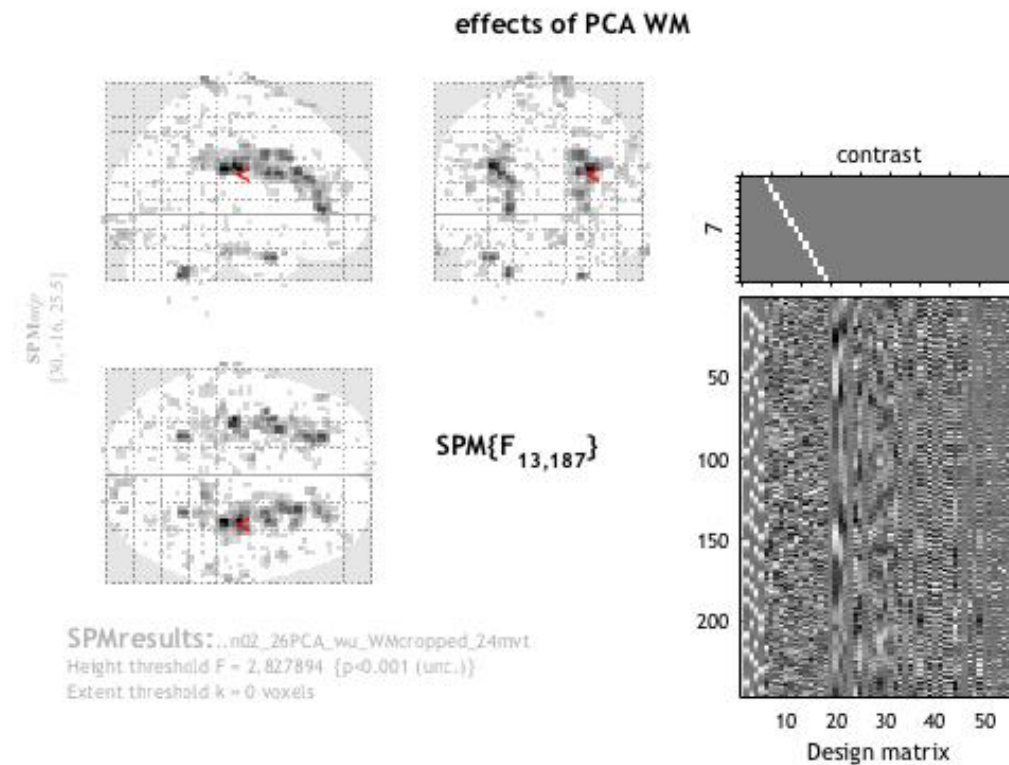
- 12 PCs + 1 mean for WM, 12 PCs + 1 mean for CSF, 24 movement parameters



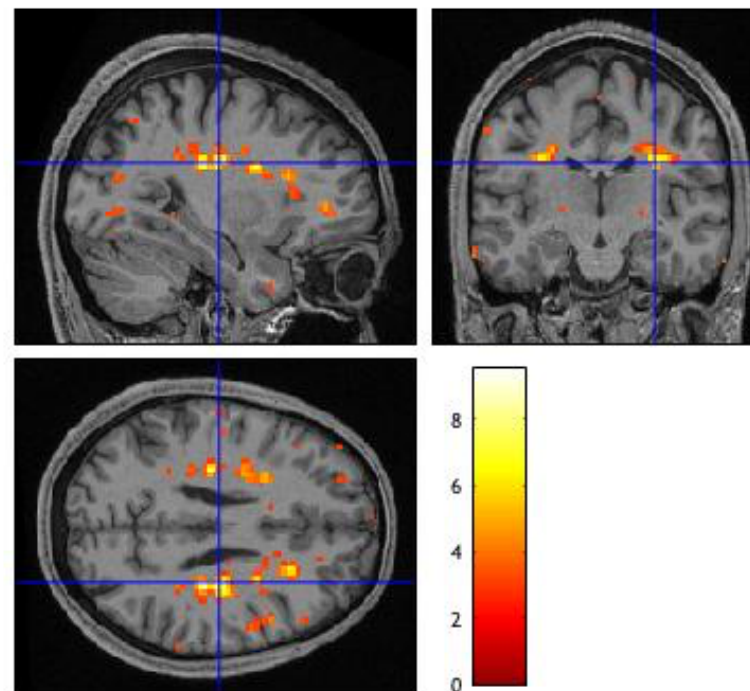
Effects of movement parameters

Denoising motion & physiological-related noise

- 12 PCs + 1 mean for WM, 12 PCs + 1 mean for CSF, 24 movement parameters

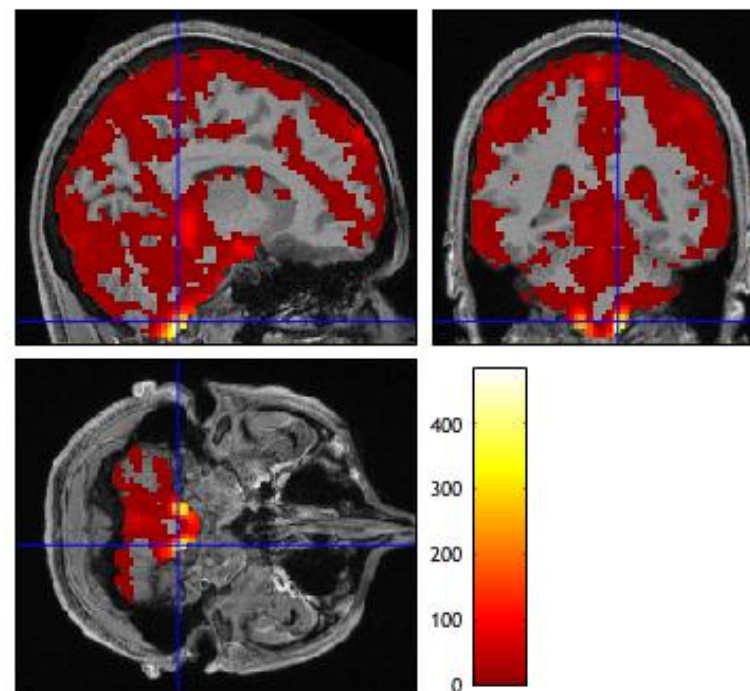
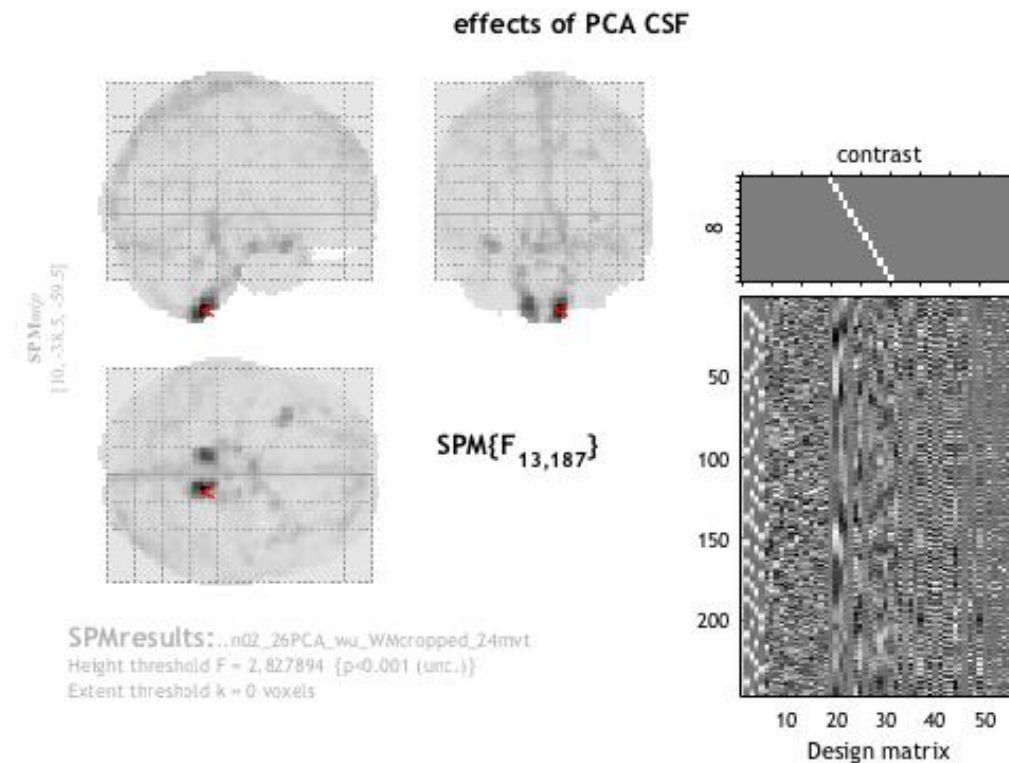


Effects of WM
nuisance regressors



Denoising motion & physiological-related noise

- 12 PCs + 1 mean for WM, 12 PCs + 1 mean for CSF, 24 movement parameters

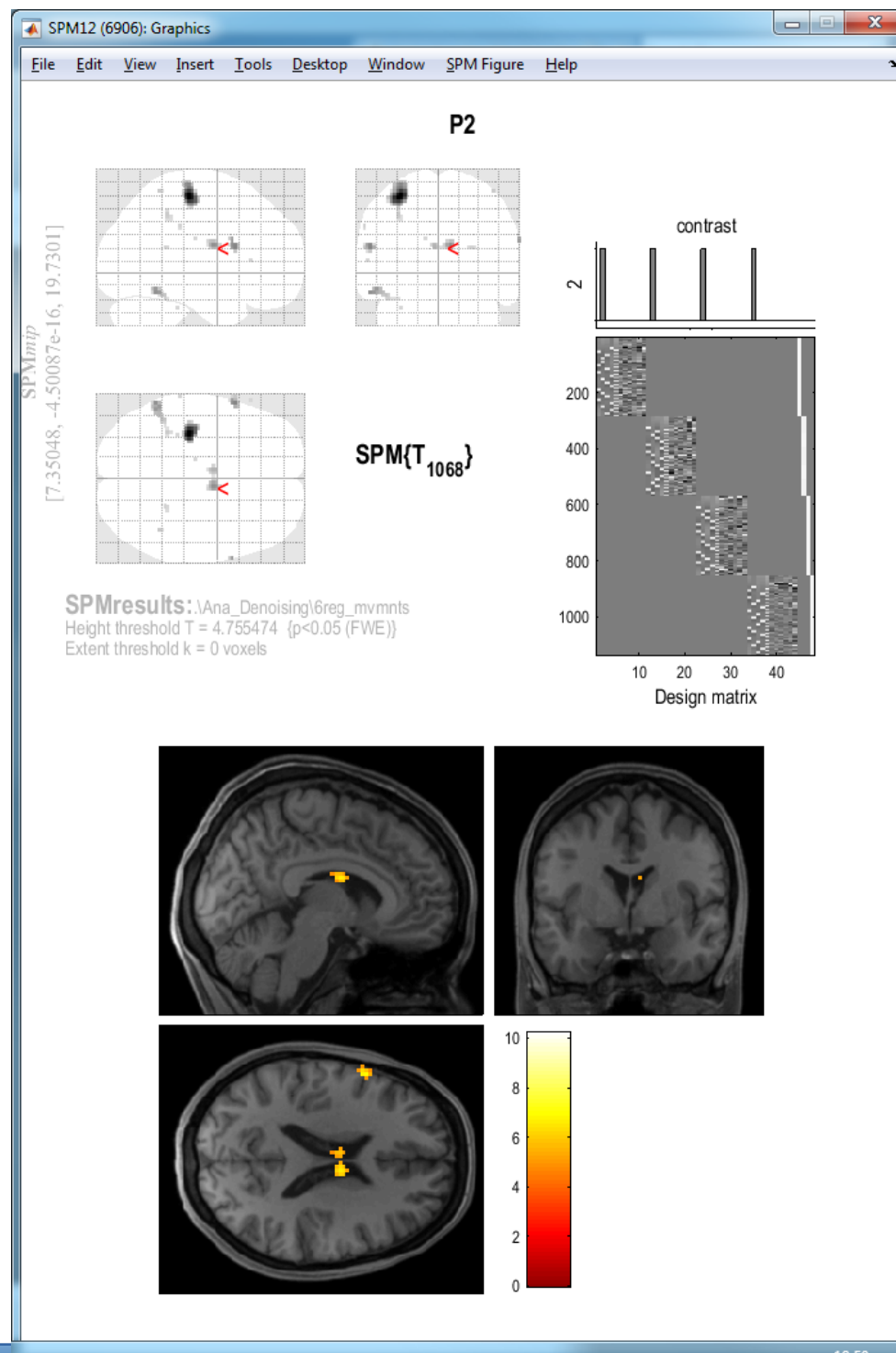


Effects of CSF
nuisance regressors

Denoising motion & physiological-related noise

- Other example : non-null contrast [1 0 0 ...], old subject, right hand stimulation

6 nuisance regressors : realign parameters $rp(t)$

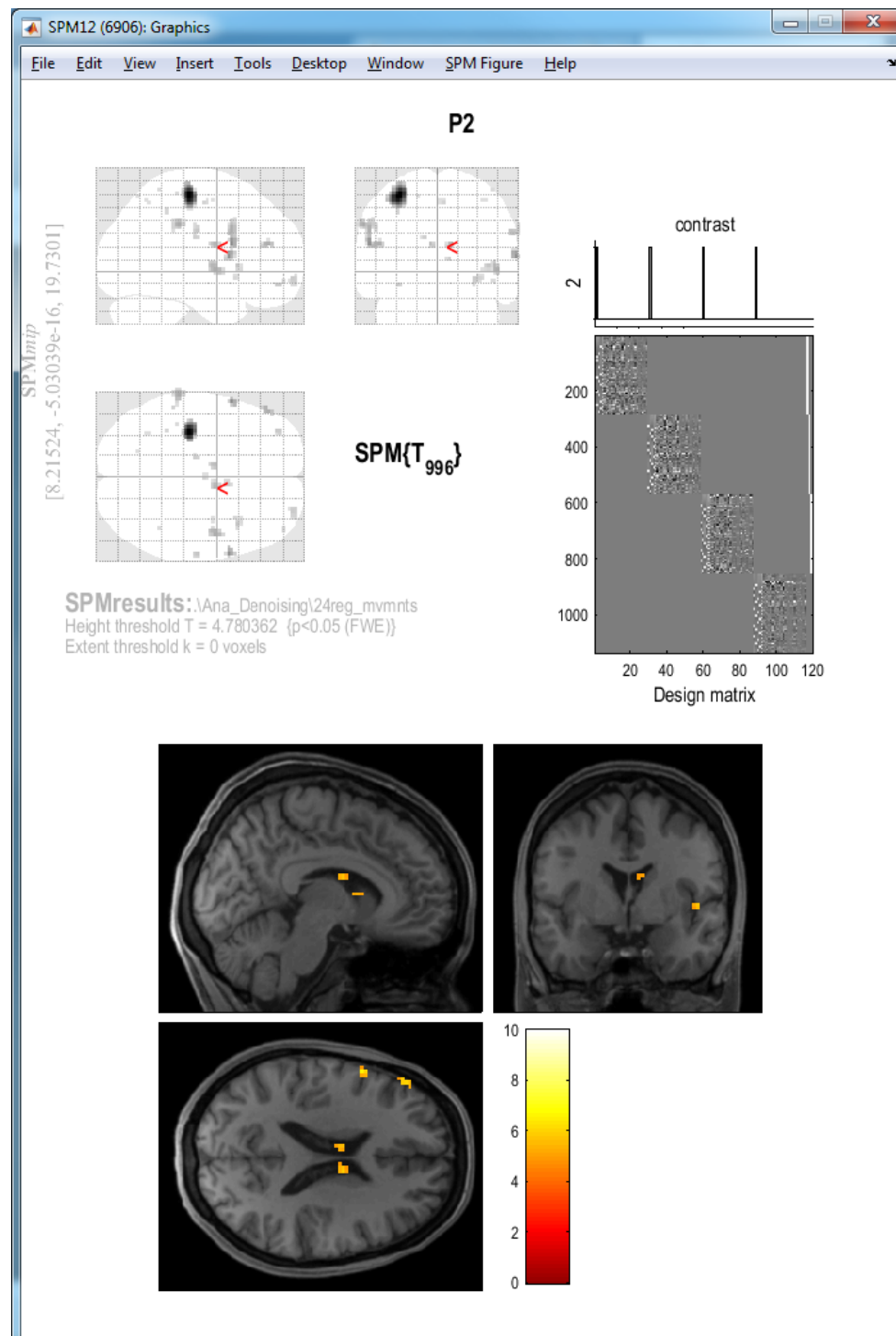


Thanks to Caroline Landelle

Denoising motion & physiological-related noise

- Other example : non-null contrast [1 0 0 ...], old subject, right hand stimulation

24 nuisance regressors : $rp(t)$, $rp^2(t)$, $rp(t-1)$, $rp^2(t-1)$

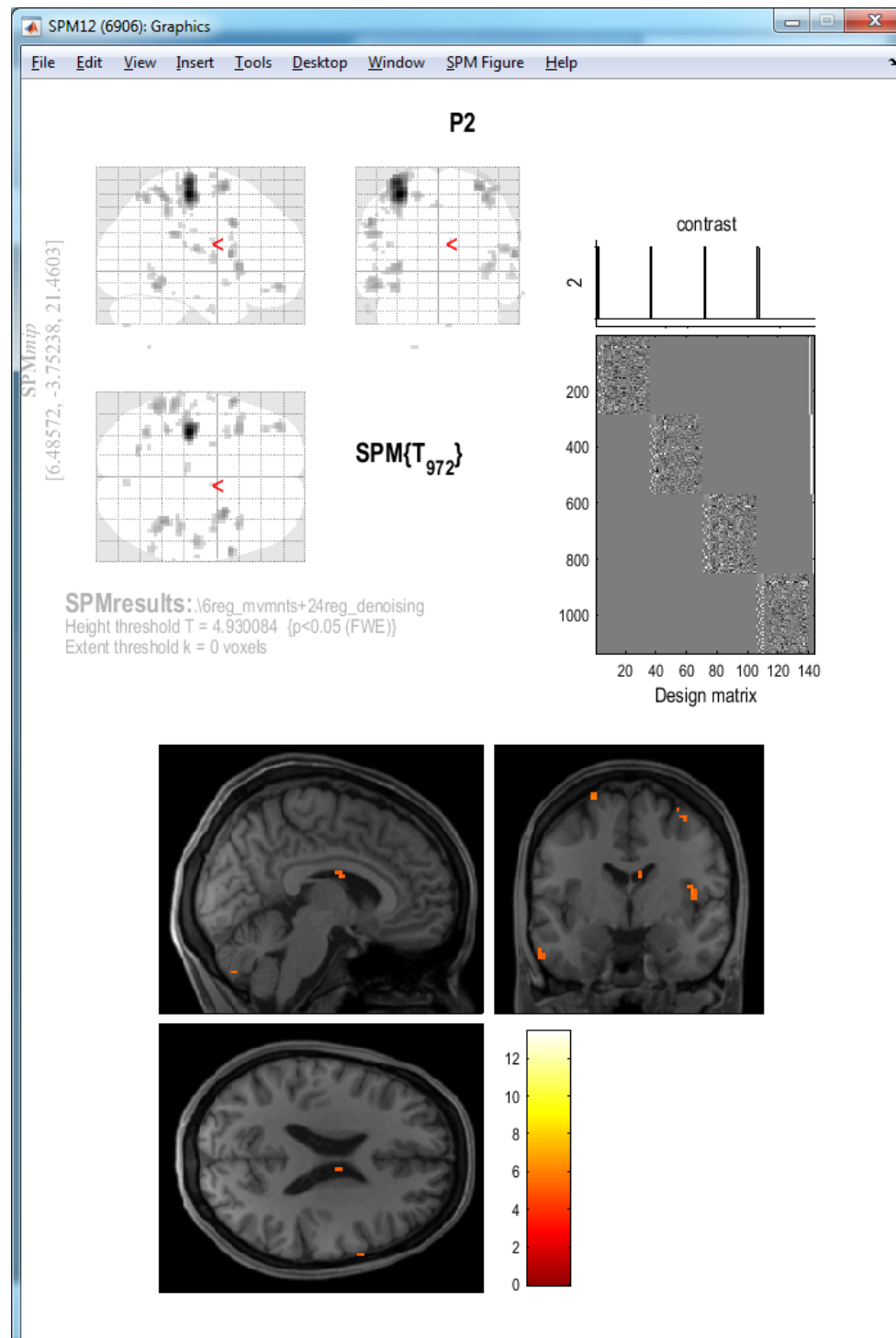


Thanks to Caroline Landelle

Denoising motion & physiological-related noise

- Other example : non-null contrast [1 0 0 ...], old subject, right hand stimulation

30 nuisance reg : 6 realign parameters $rp(t)$ + 12 PCA WM + 12 PCA CSF

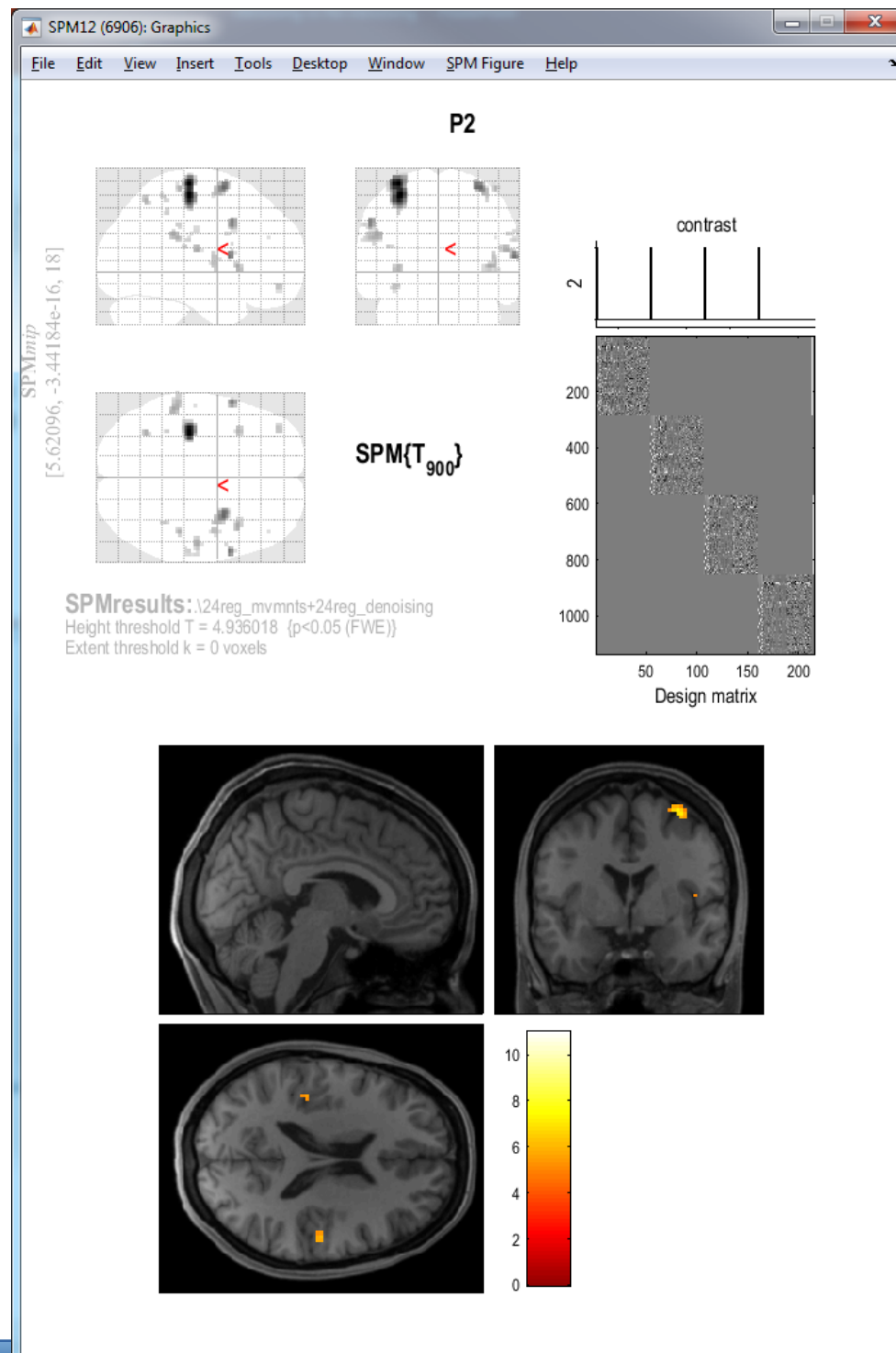


Thanks to Caroline Landelle

Denoising motion & physiological-related noise

- Other example : non-null contrast [1 0 0 ...], old subject, right hand stimulation

48 nuisance reg : $rp(t)$, $rp^2(t)$, $rp(t-1)$, $rp^2(t-1)$ + 12 PCA WM + 12 PCA CSF

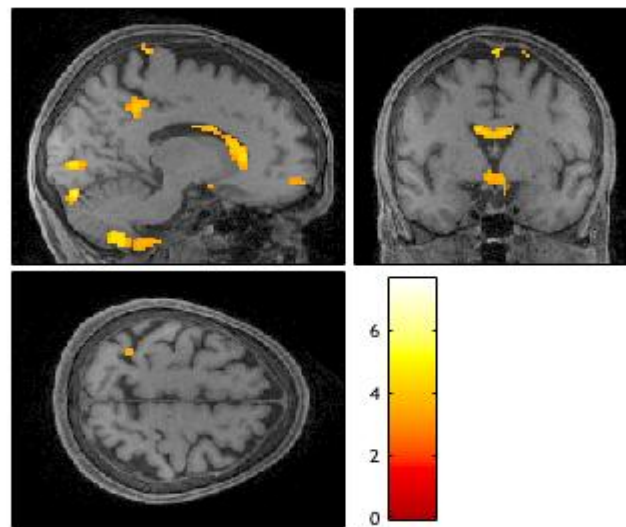


Thanks to Caroline Landelle

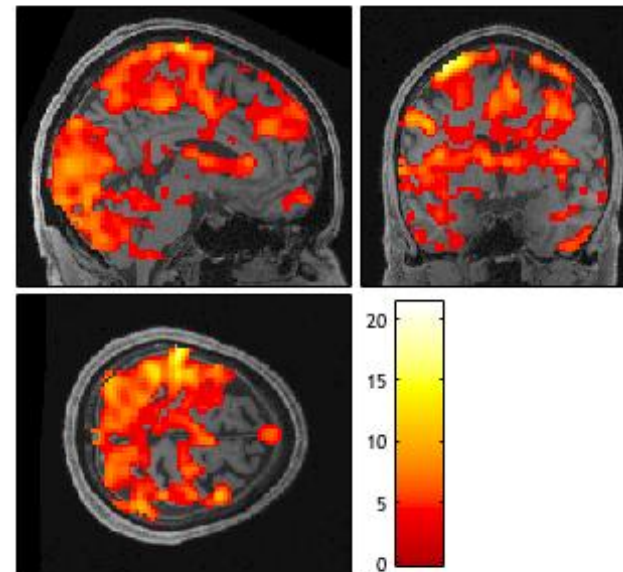
Denoising motion & physiological-related noise

- For some subjects, the denoising with 48 nuisance regressors ($rp(t)$, $rp^2(t)$, $rp(t-1)$, $rp^2(t-1)$, 12 PCA WM, 12 PCA CSF) is very efficient

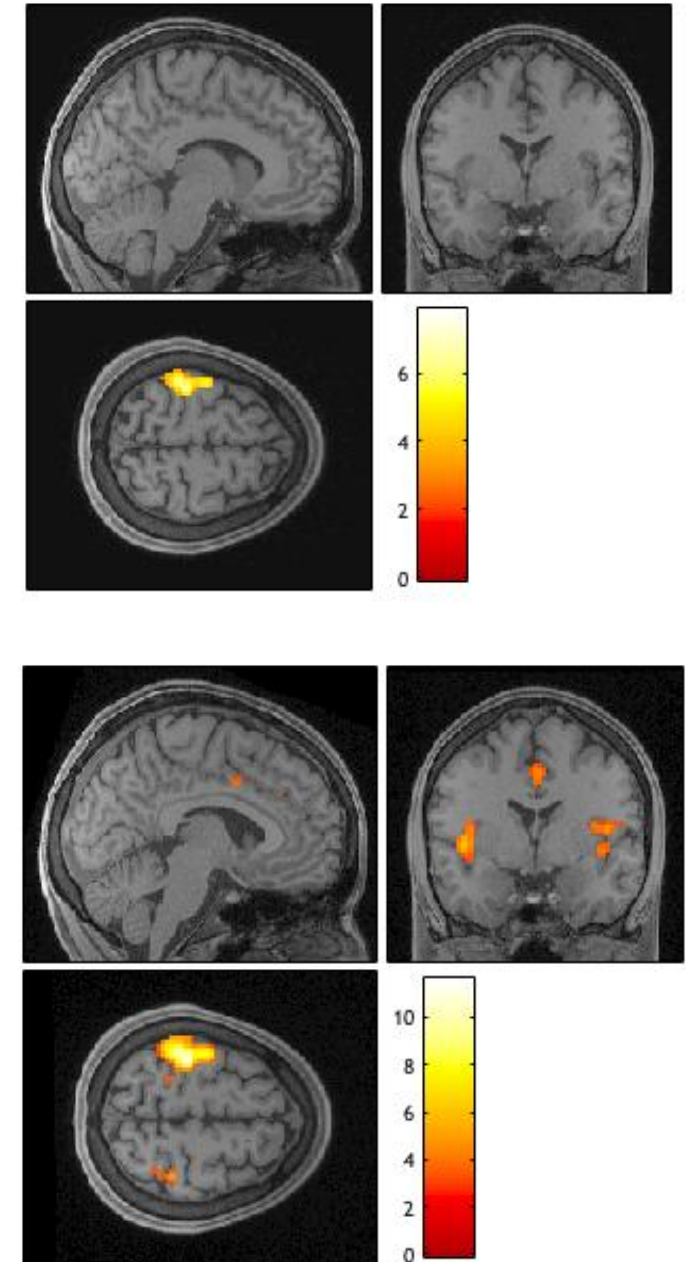
Loss of ventricular
noising activity



Loss of all brain
noising activity



Greater statistical
values



Before

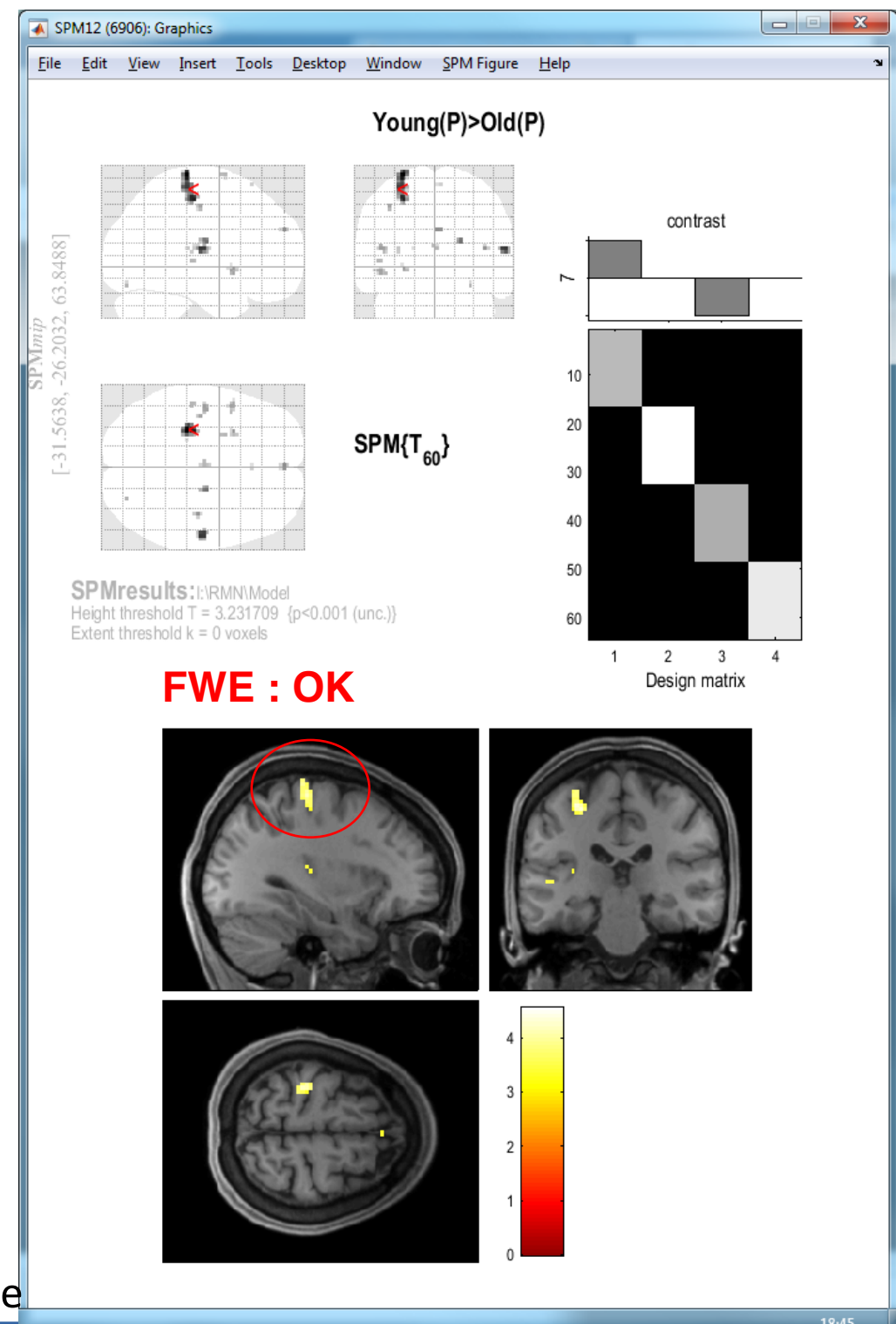
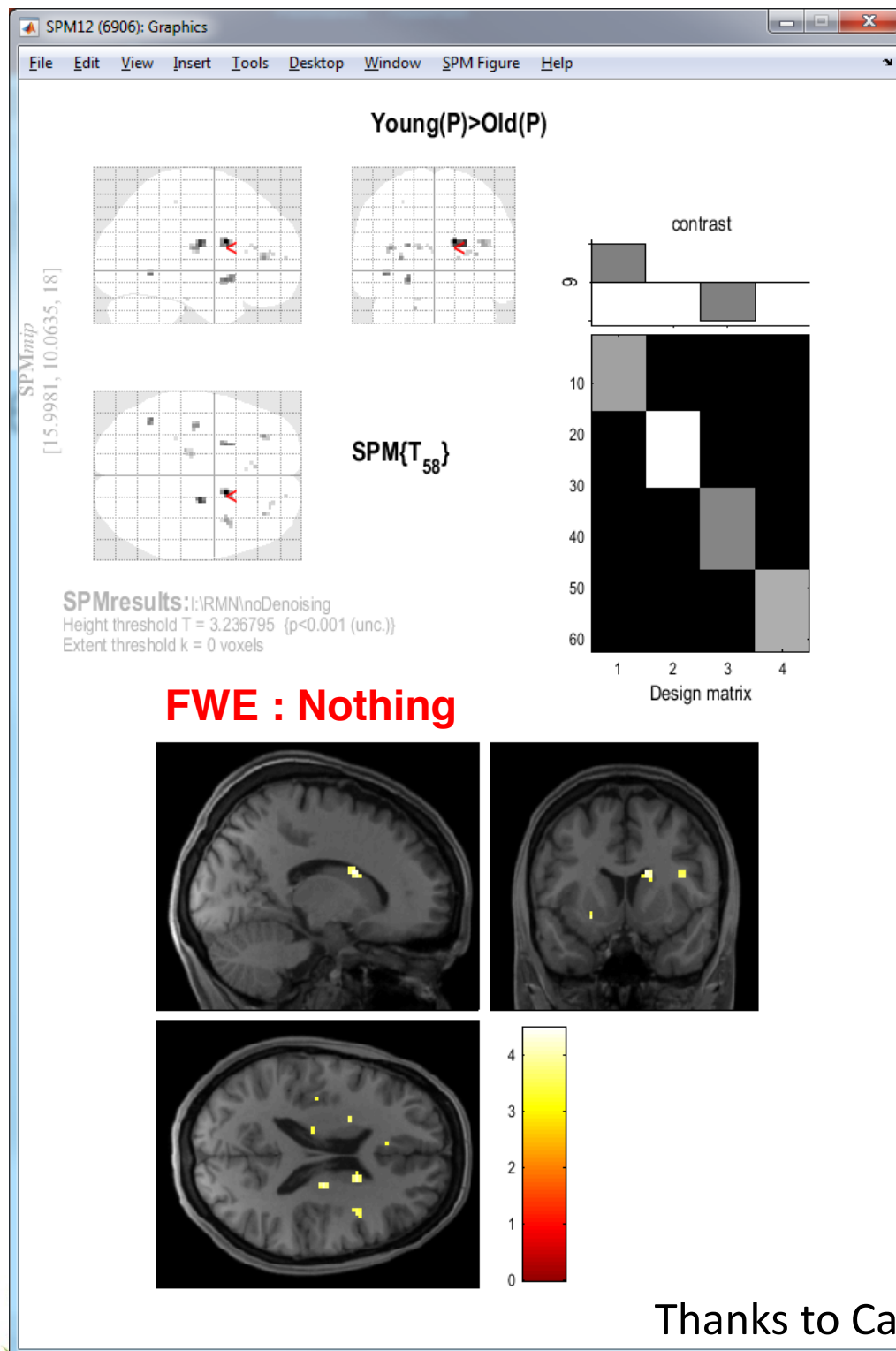
Denoising

After

Thanks to Caroline Landelle

Denoising motion & physiological-related noise

- For inter-group comparison, the denoising with 48 nuisance regressors ($rp(t)$, $rp^2(t)$, $rp(t-1)$, $rp^2(t-1)$, 12 PCA WM, 12 PCA CSF) is very efficient



Thanks to Caroline Landelle

Denoising physiological-related noise

- Data-driven denoising methods of physiological noise

Based on Principal Component Analysis (PCA) of noise regions signals : white matter (WM) & Cerebro-Spinal Fluid (CSF)

→ Questions :

- Precise definition of noise region signals (minimizing the effect of partial voluming with other tissue types)
- PCA to be performed on non-smoothed EPI data
- Number of PCs for each tissue ? % of variance explained ?
- **Need to orthogonalize the nuisance regressors from the task-related regressors**

Denoising physiological-related noise

- Data-driven denoising methods of physiological noise

Based on Independent Component Analysis (ICA)

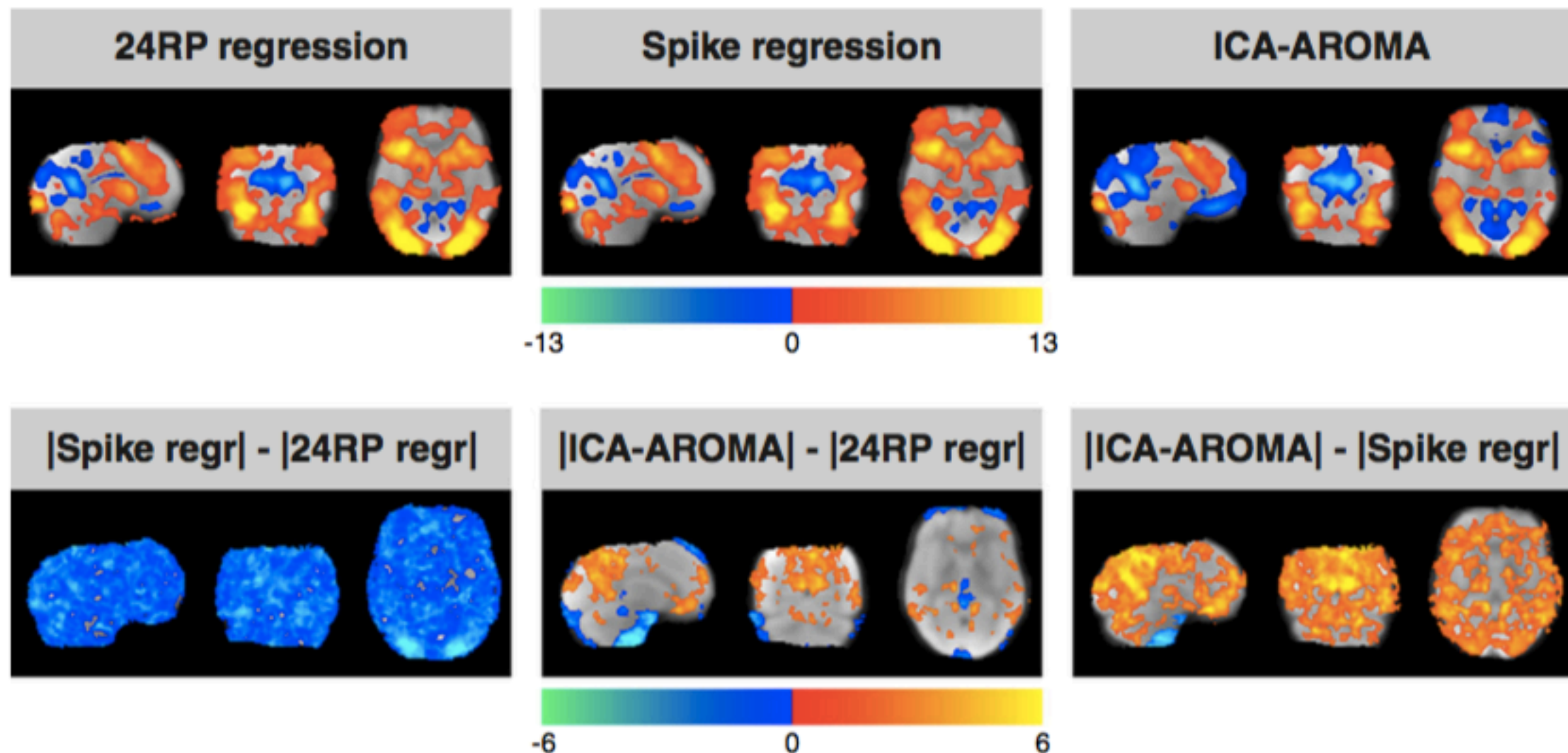
- temporal ICA : PESTICA (Beall and Lowe, 2007)
- spatial ICA : CORSICA (Perlberg & al, 2007)
- spatial ICA : ICA-AROMA (Pruim & al, 2015) & FIX-ICA (Salimi-Khorshidi & al, 2014) : available in FSL

→ Question :

Choice of the components to be removed to the EPI data ?

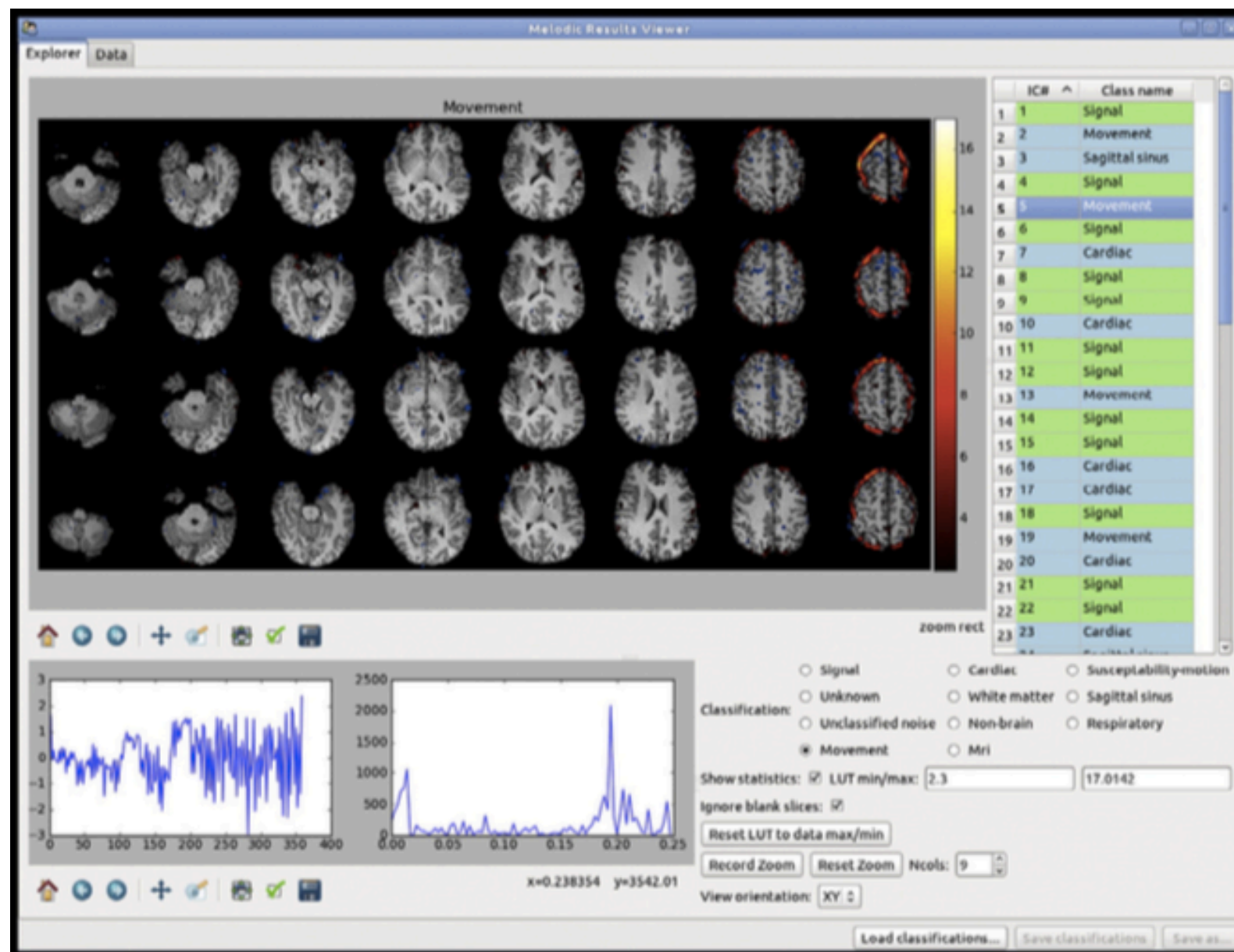
Denoising physiological-related noise

- Data-driven denoising methods of physiological noise
Based on Independent Component Analysis (ICA)
 - ICA-AROMA (Pruim & al, 2015) : available in FSL
 - remove motion-related ICA components from FMRI data



Denoising physiological-related noise

- Data-driven denoising methods of physiological noise
Based on Independent Component Analysis (ICA)
- FIX-ICA (Salimi-Khorshidi & al, 2014) : available in FSL
→ aims to auto-classify ICs into "good" vs "bad" components

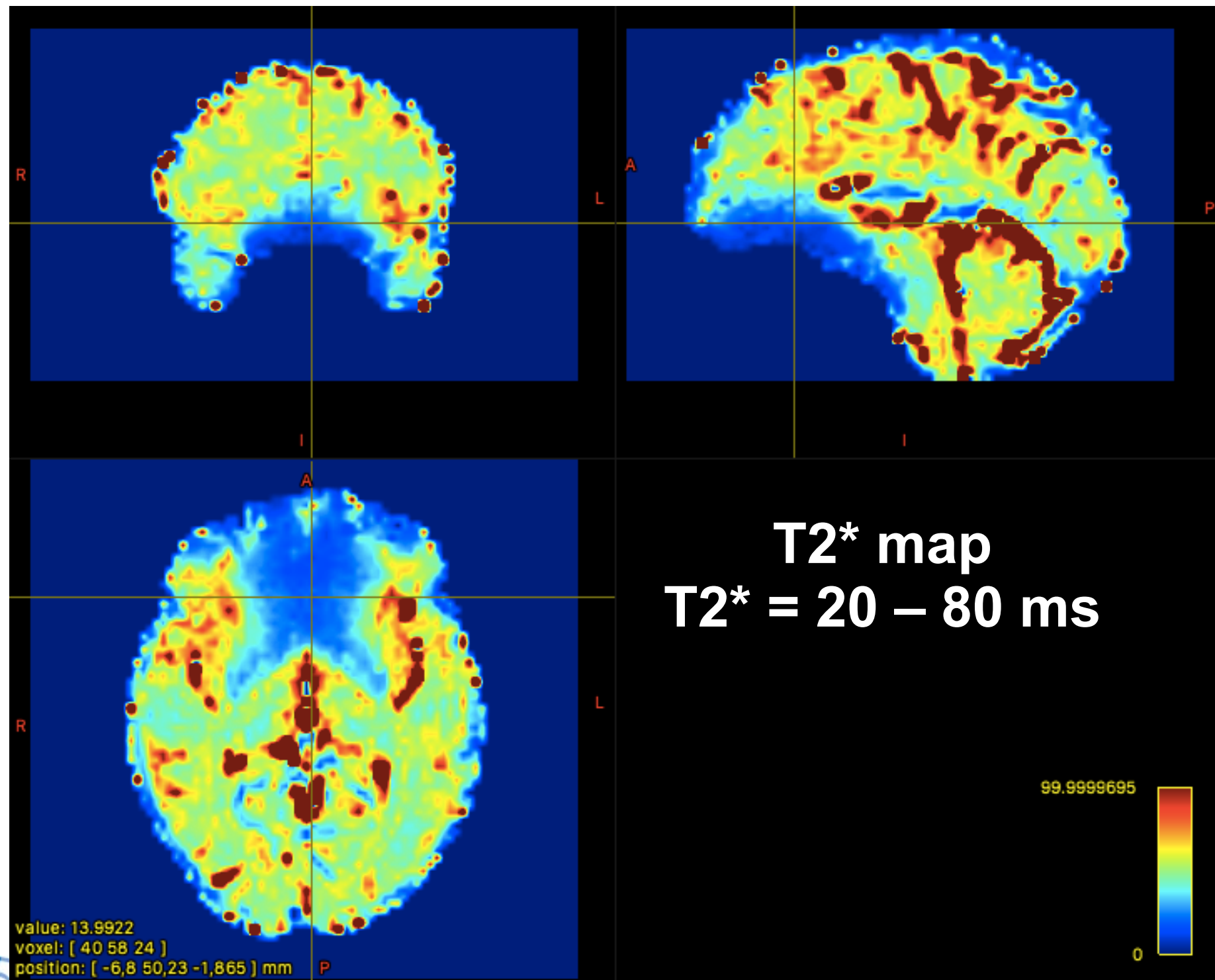


Denoising physiological-related noise

- Data-driven denoising methods of physiological noise
Based on Independent Component Analysis (ICA)
- FIX-ICA (Salimi-Khorshidi & al, 2014) : available in FSL
→ aims to auto-classify ICs into "good" vs "bad" components
- Example : FMRI's ICA-based Xnoiseifier – FIX (FSL)
http://www.fmrib.ox.ac.uk/analysis/FIX-training/fix_eg.html

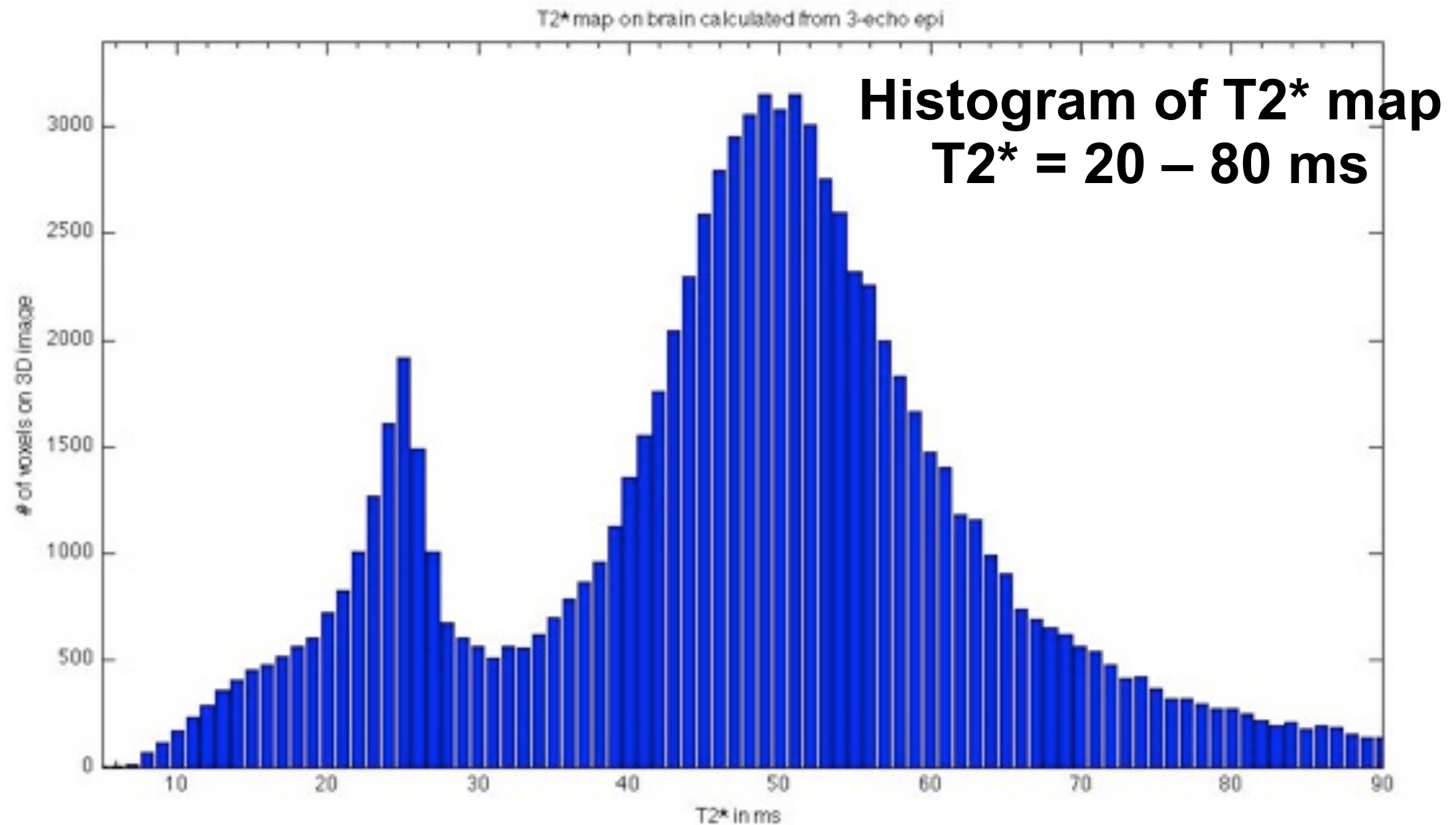
Next step : Multi-Echo acquisitions

- A single-echo EPI ($TE \approx 30$ ms) is sub-optimal because of the huge variability of $T2^*$ across brain regions



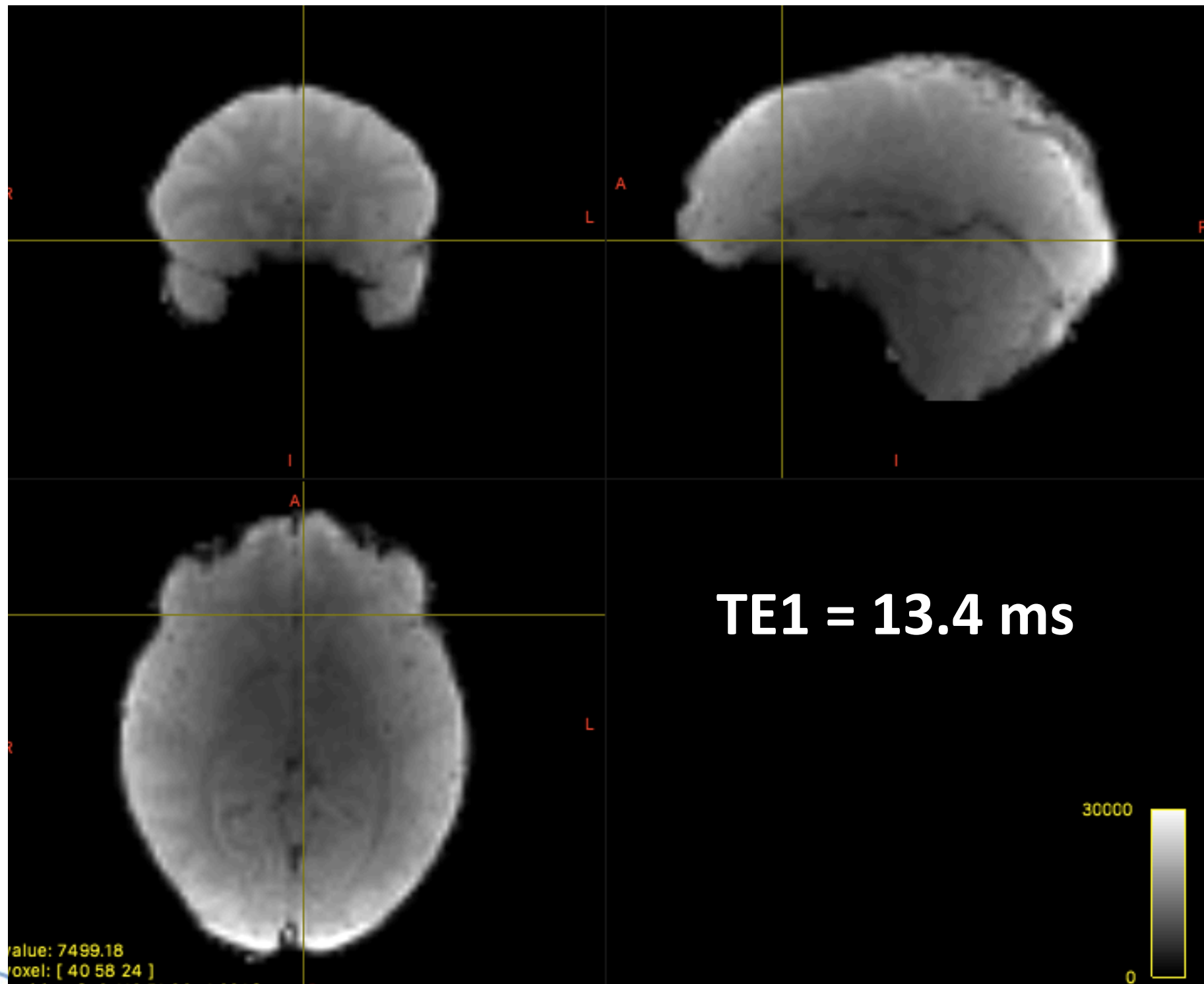
Next step : Multi-Echo acquisitions

- A single-echo EPI ($TE \approx 30$ ms) is sub-optimal because of the huge variability of $T2^*$ across brain regions



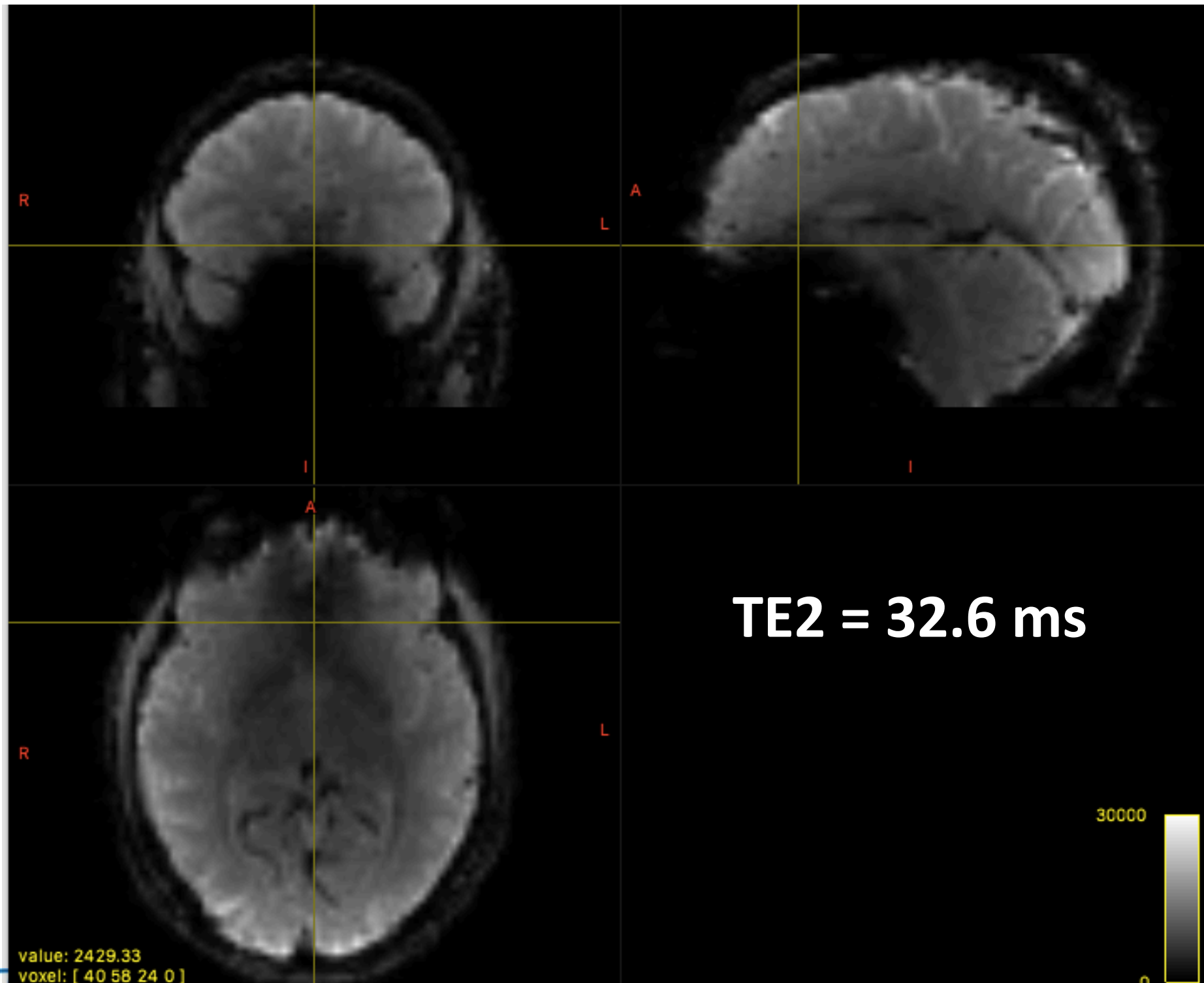
Next step : Multi-Echo acquisitions

- EPI Multi-bande Multi-Echo (MB 3 ME 3, iPAT 2, TR 1425 ms)



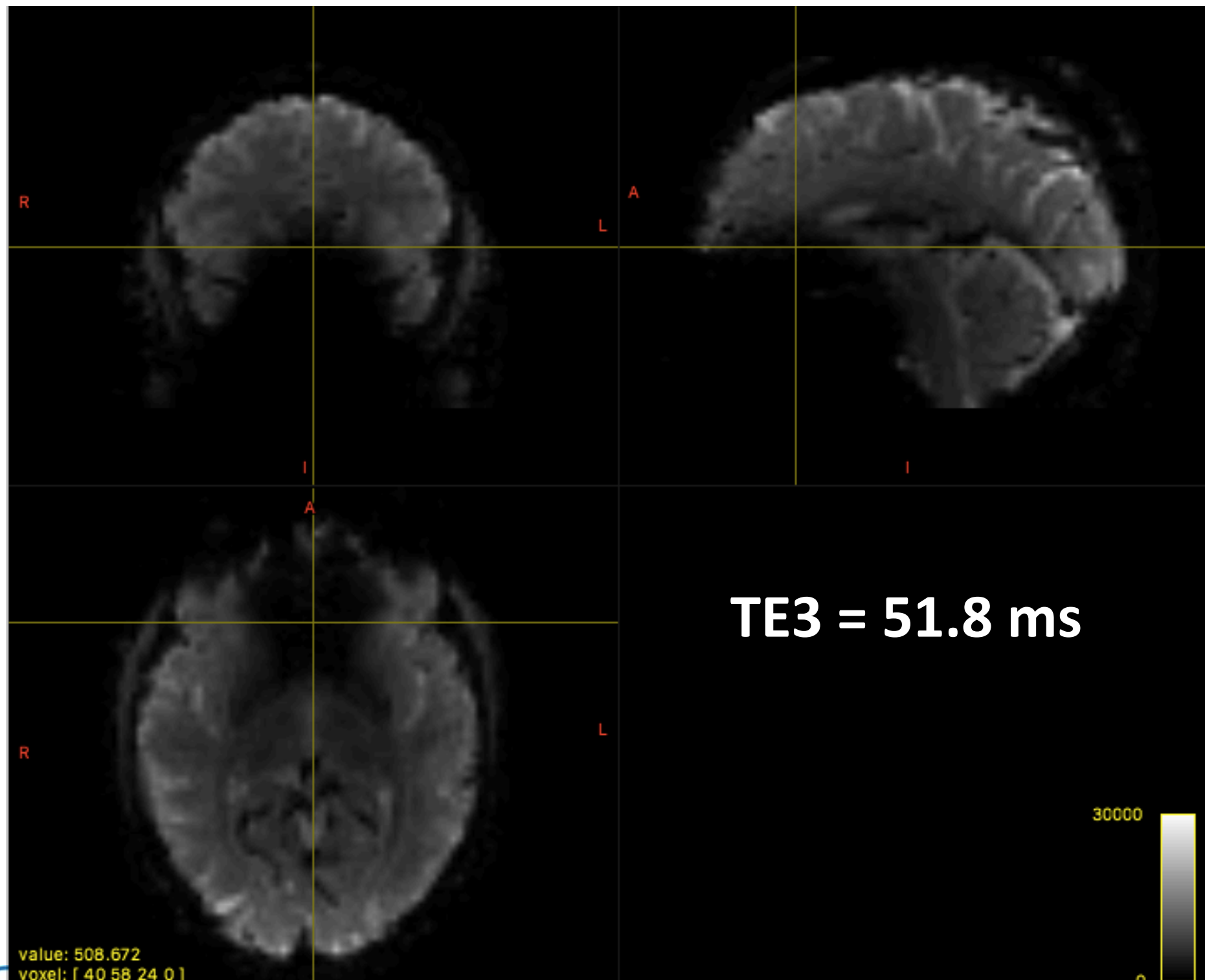
Next step : Multi-Echo acquisitions

- EPI Multi-bande Multi-Echo (MB 3 ME 3, iPAT 2, TR 1425 ms)



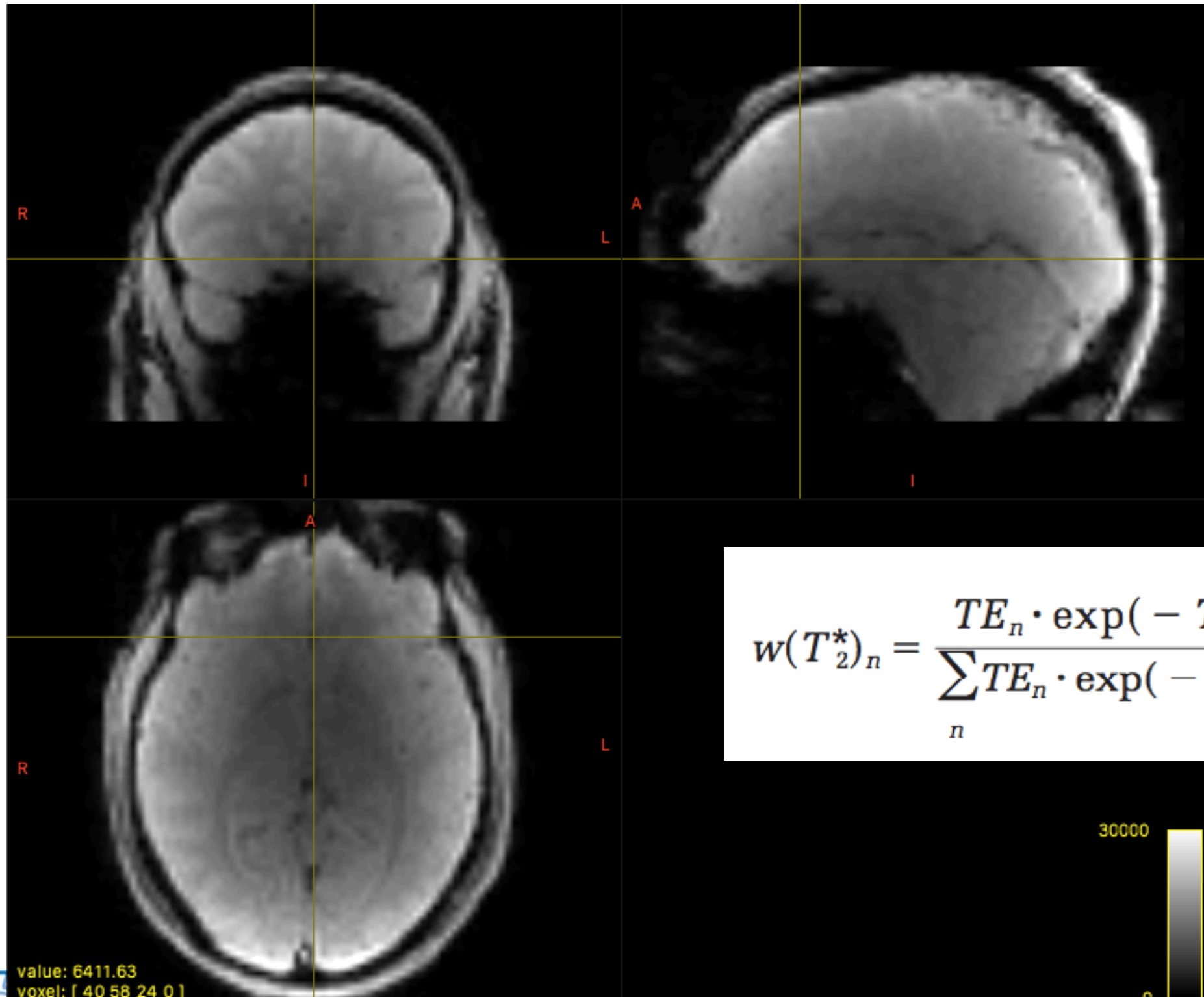
Next step : Multi-Echo acquisitions

- EPI Multi-bande Multi-Echo (MB 3 ME 3, iPAT 2, TR 1425 ms)



Next step : Multi-Echo acquisitions

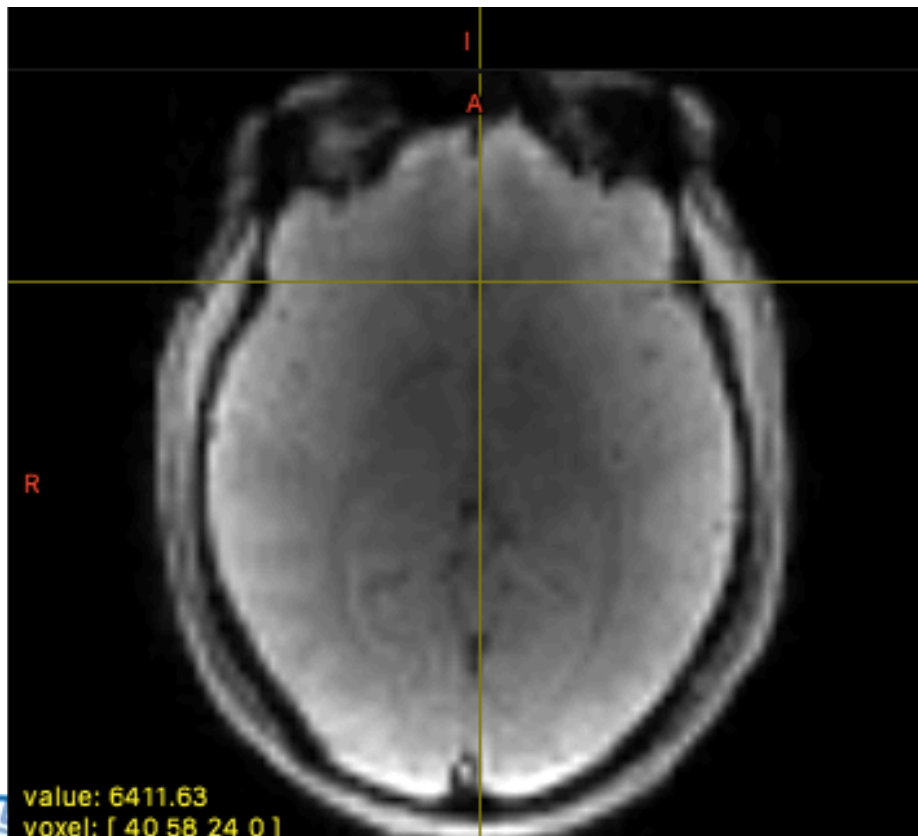
- --> 1/ Multi-Echo combination (Poser & al, 2006)



Next step : Multi-Echo acquisitions

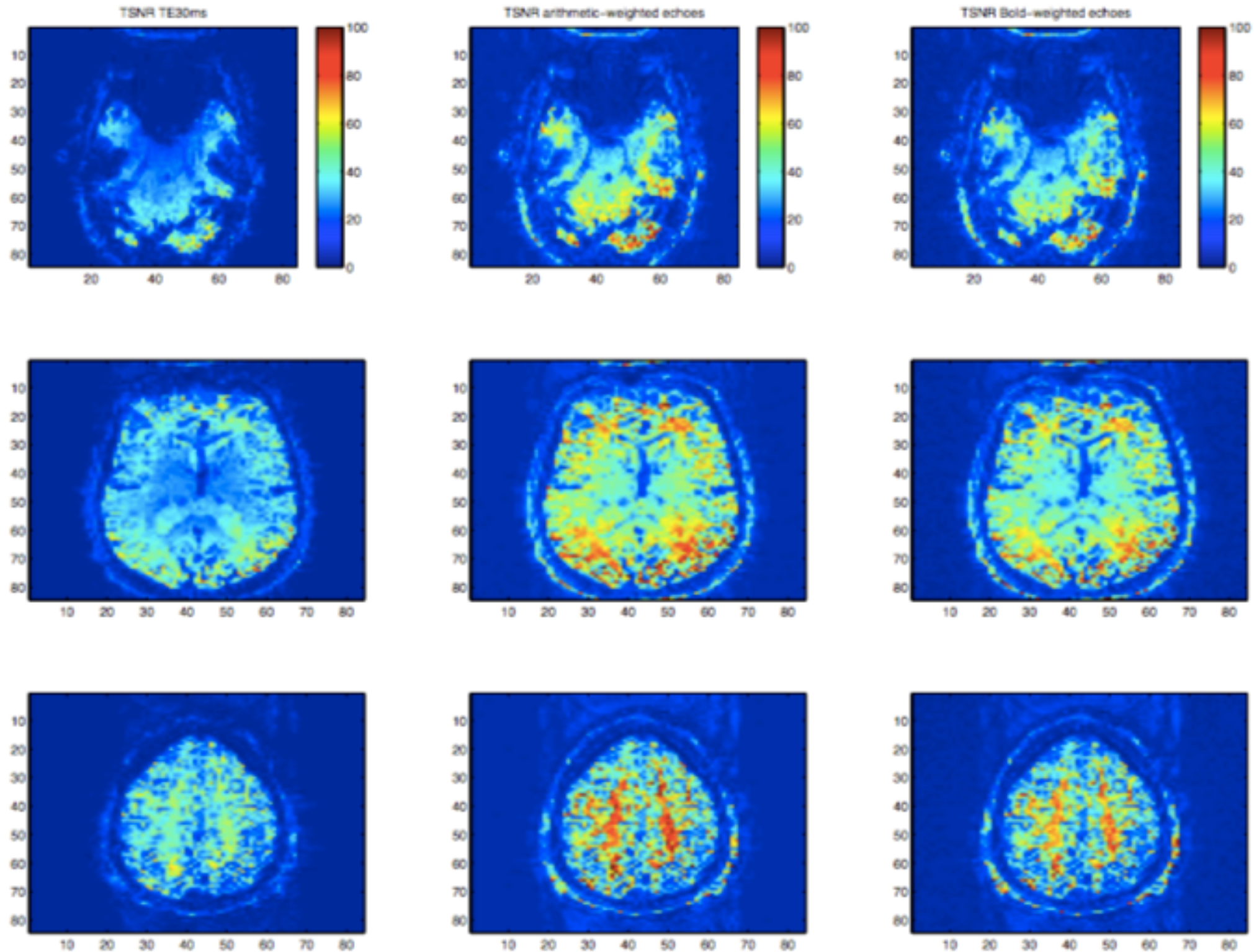
- → 1/ Multi-Echo combination (Poser & al, 2006)

Multi-echo fMRI offers clear advantages for imaging brain regions such as the orbitofrontal cortex and inferior temporal lobes, which are prone to susceptibility distortions and signal dropouts



Next step : Multi-Echo acquisitions

- 1/ Multi-Echo combination (Poser & al, 2006)



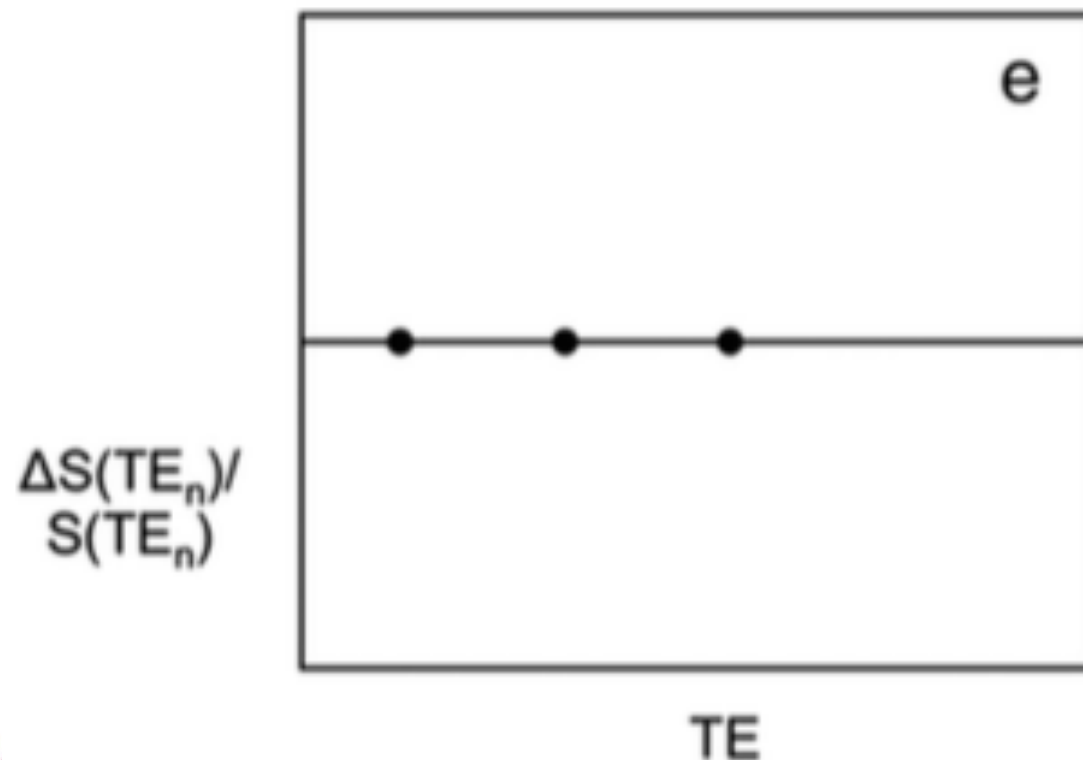
Next step : Multi-Echo acquisitions

- → 2/ Multi-Echo acquisitions for denoising
 - Signals can be recorded at a short TE which is assumed to have minimal $T2^*$ - weighting and mainly sensitive to fluctuations in the net magnetization S_0 .
- The short TE signal can then be regressed out from time series acquired at a longer TE that is optimized for BOLD sensitivity (Bright and Murphy, 2013; Buur et al., 2008).

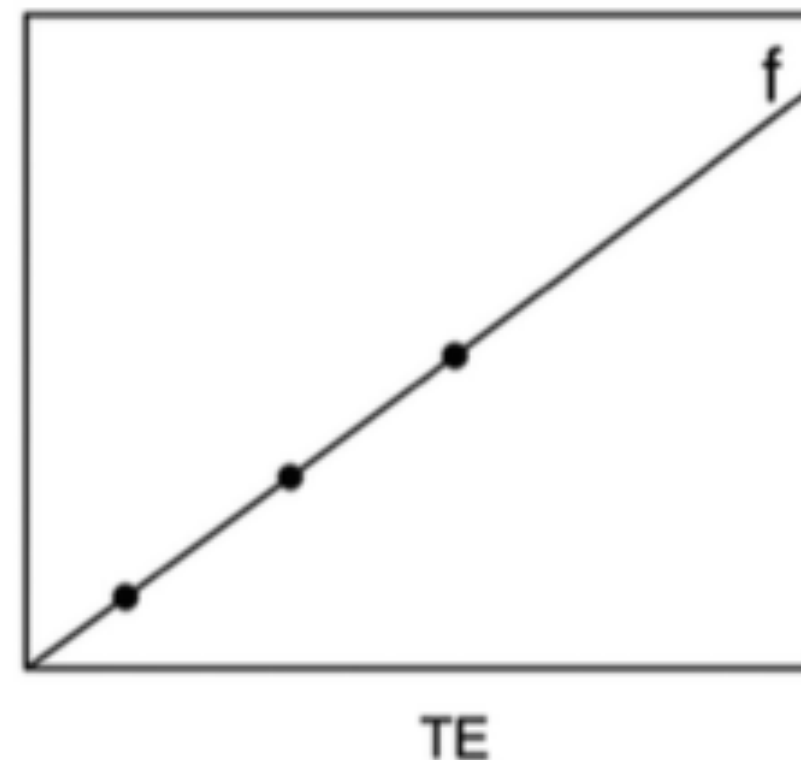
Next step : Multi-Echo acquisitions

- 2/ Multi-Echo acquisitions for denoising
Kundu et al. (2012) proposed a multi-echo denoising strategy based on independent component analysis (ME-ICA).
This method exploits the fact that BOLD components must exhibit a linear dependence with TE, whereas non-BOLD components must exhibit no dependence with TE.

ΔS_0 : non-BOLD

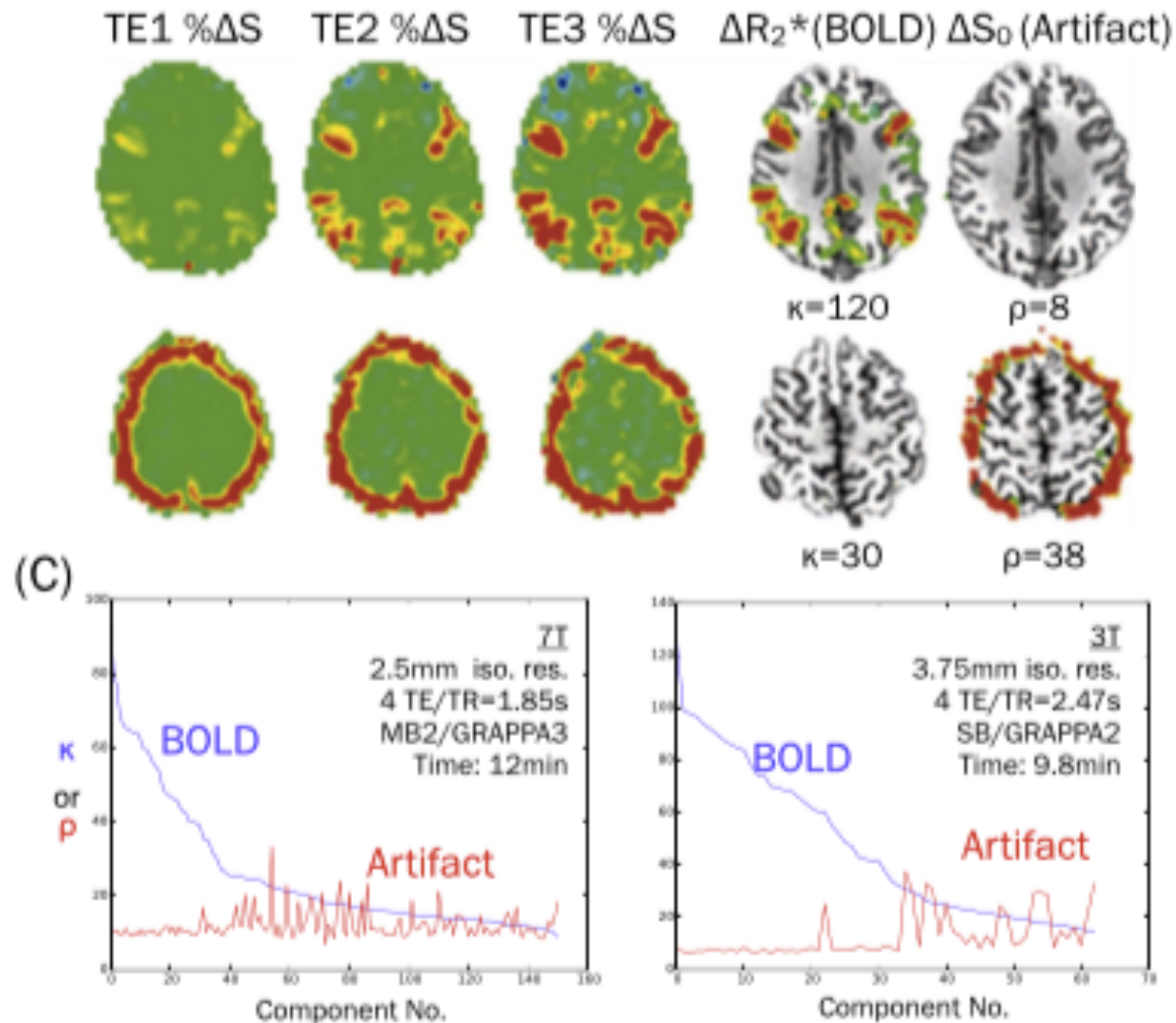


ΔR_2^* : BOLD



Next step : Multi-Echo acquisitions

- 2/ Multi-Echo acquisitions for denoising
Kundu et al. (2012) proposed a multi-echo denoising strategy based on independent component analysis (ME-ICA).



General Conclusion

- **Denoising BOLD fMRI data is crucial !**
- **It has to be done with a lot of care ...**

References

- Special issue of NeuroImage 2017

NeuroImage 154 (2017) 128–149



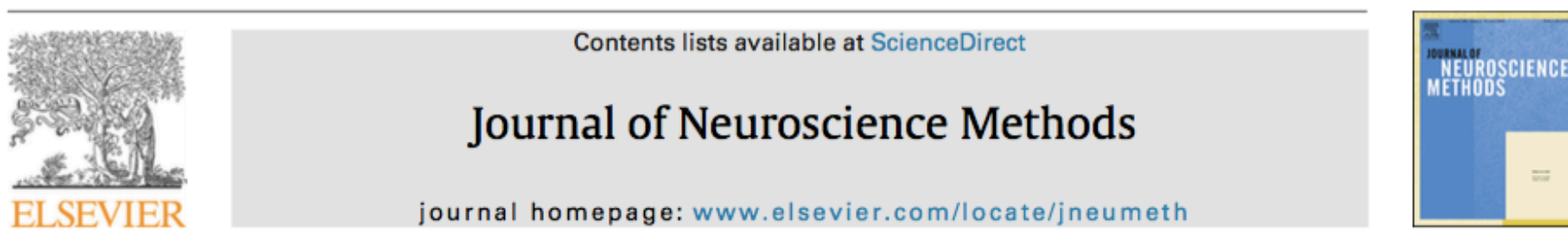
Methods for cleaning the BOLD fMRI signal

César Caballero-Gaudes^{a,*}, Richard C. Reynolds^b



- PhysIO Toolbox

Journal of Neuroscience Methods 276 (2017) 56–72



The PhysIO Toolbox for Modeling Physiological Noise in fMRI Data

Lars Kasper^{a,b,*}, Steffen Bollmann^c, Andreea O. Diaconescu^a, Chloe Hutton^d,
Jakob Heinzle^a, Sandra Iglesias^a, Tobias U. Hauser^{d,e}, Miriam Sebold^f,
Zina-Mary Manjaly^g, Klaas P. Pruessmann^b, Klaas E. Stephan^{a,d,h}

