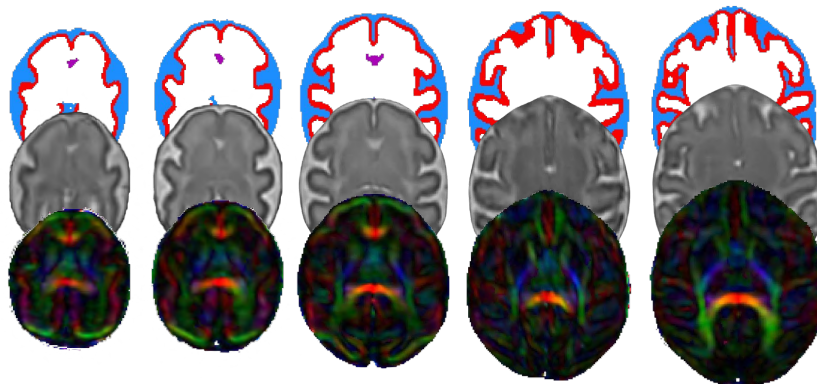
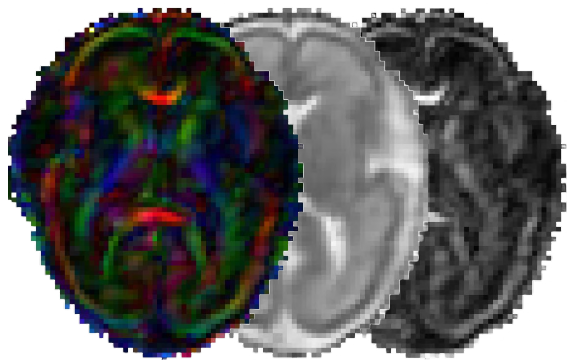


Processing and Analysis of Fetal Diffusion MRI

From Clinical Human Imaging to Longitudinal Baboon Research Data

Mattia Cazzolla



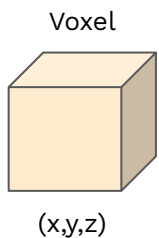
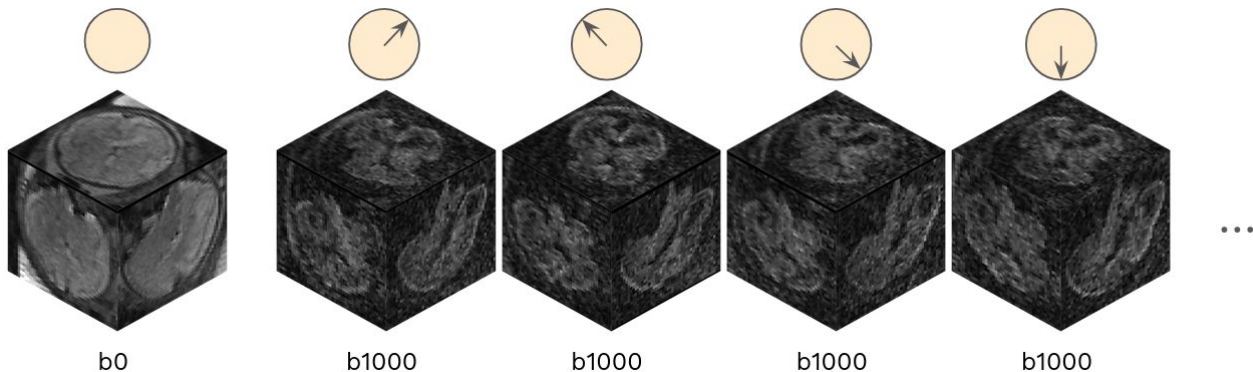
Outline

1. **Fetal Diffusion MRI:** opportunities and challenges
2. **MarsFet:** clinical human acquisitions
3. **BaboFet:** research baboon acquisitions

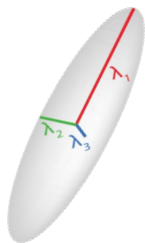
Fetal Diffusion MRI

Introduction

Diffusion MRI allow to study microstructural tissues information by measuring the **signal attenuation** caused by water **diffusion** in a specific direction



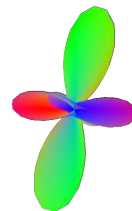
$$\left\{ \begin{array}{l} b=0: [I_0] \\ b=1000: [I_1, I_2, I_3, \dots, I] \end{array} \right.$$



Tensor model

$$S_{DWI} = S_{b=0} \times e^{(-b \times D)}$$

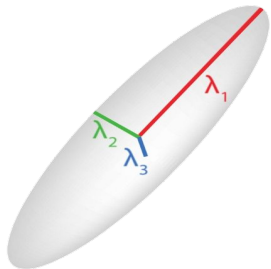
$$D = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{yx} & D_{yy} & D_{yz} \\ D_{zx} & D_{zy} & D_{zz} \end{bmatrix}$$



Higher order models

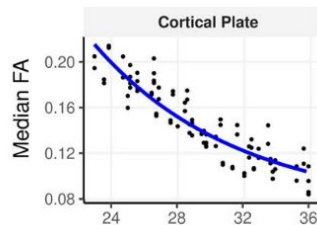
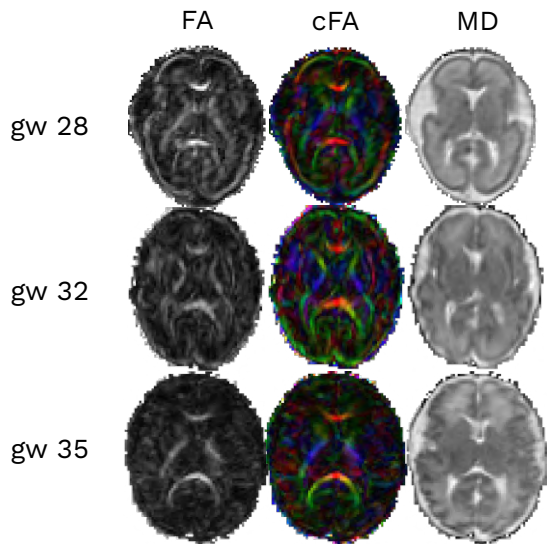
Fetal Diffusion MRI

Introduction

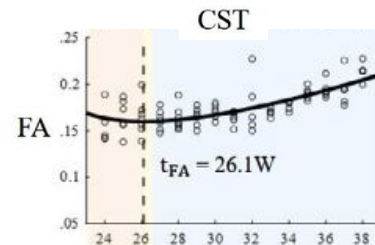


From the tensor can extract metrics:

- **Fractional Anisotropy** (dominant diffusion direction)
- **Mean Diffusivity** (proxy for water content)
- Axial and Radial Diffusivity



Calixto et al, Cerebral Cortex



Chen et al, Neuroimage

Do different cortical/white matter areas develop with different dynamic?

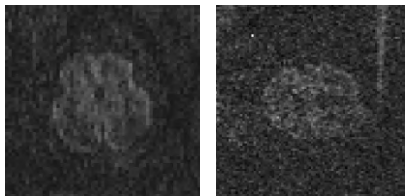
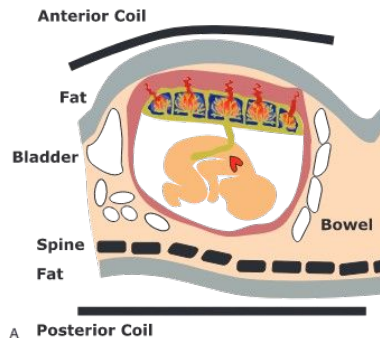
Fetal Diffusion MRI

Challenges - ROI

Coils

Maternal tissue between fetal brain and MRI coils

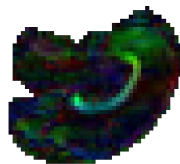
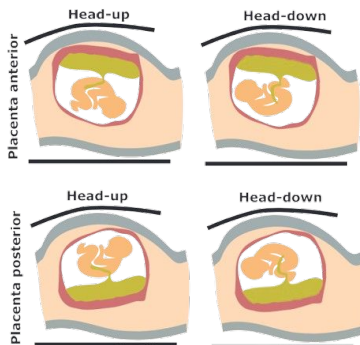
low SNR



Non standard orientation

Non standard orientation relative to scanner

wrong color maps



Brain extraction

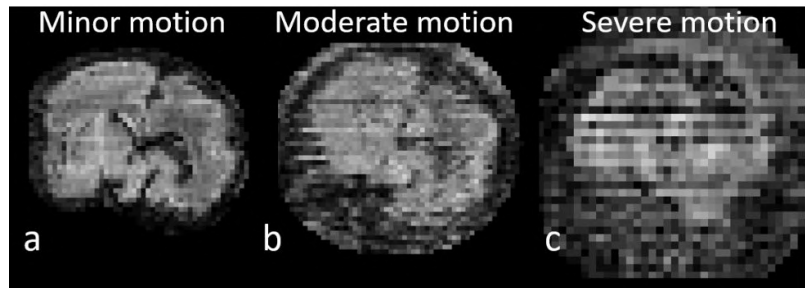
Brain needs to be located and extracted

need for specific tools



Fetal Diffusion MRI

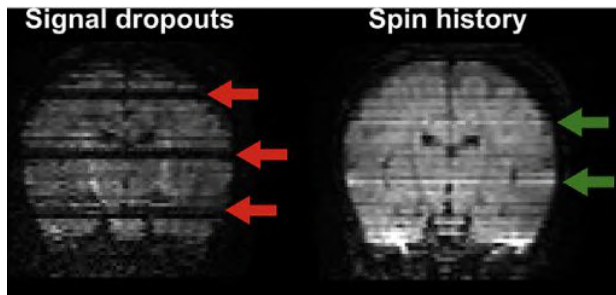
Challenges - Motion



Caused by:

- maternal breathing
- fetal motion

Motion can be assumed frozen during the readout of each slice.



Motion can cause:

- signal dropout
- slice cross-talks artifacts

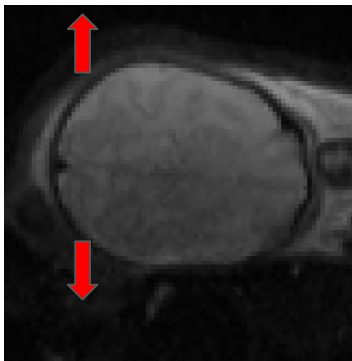
Fetal Diffusion MRI

Challenges - Geometrical distortions

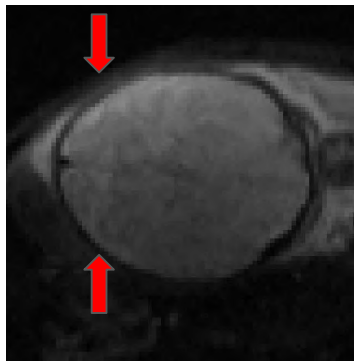
Fetal dMRI rely on EPI (Echo Planar Imaging) for efficient data acquisition.
But EPI suffer from local geometric distortions:

Magnetic Susceptibility

b0 with **AP** phase encoding

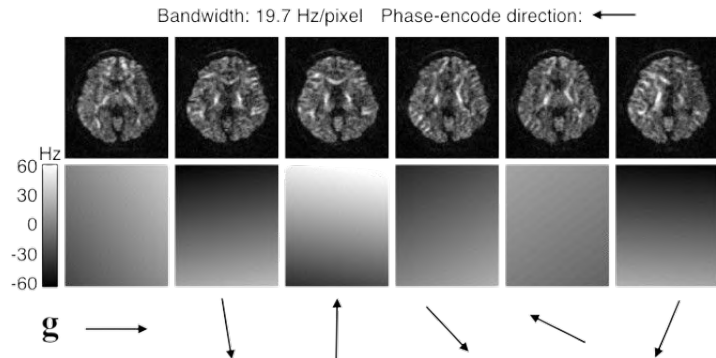


b0 with **PA** phase encoding



differences of **magnetic susceptibility** at
tissue/air interface

Eddy currents



rapid switch of diffusion gradients generate
currents in nearby conductors

Outline

1. **Fetal Diffusion MRI:** challenges and limitations
2. **MarsFet:** clinical human acquisitions
3. **BaboFet:** research baboon acquisitions

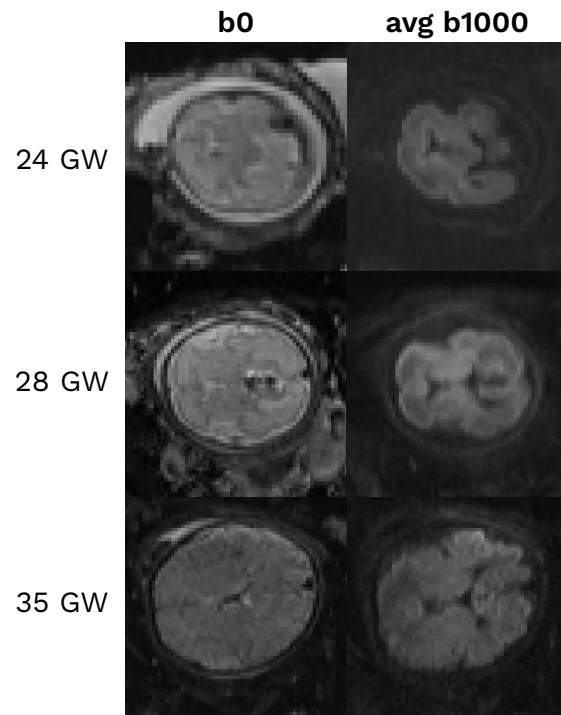
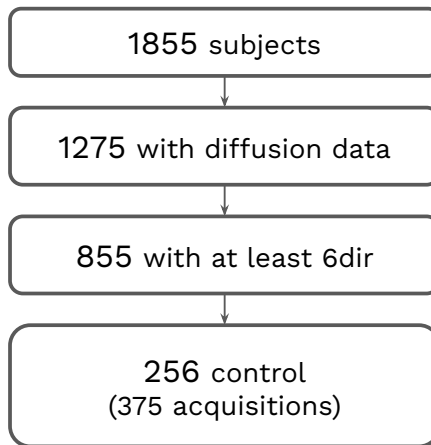
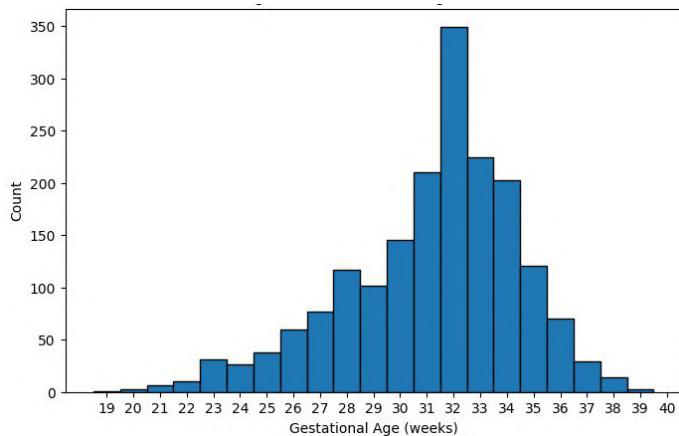
MarsFet

Dataset



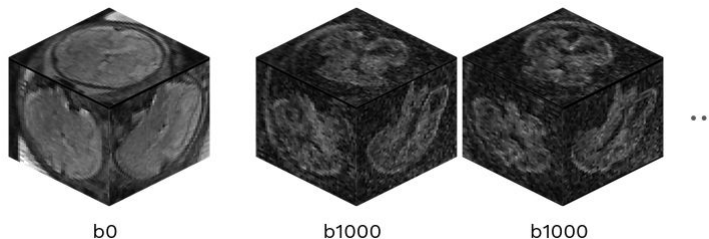
Large-scale fetal MRI dataset acquired during routine clinical examinations at *La Timone University Hospital* (Marseille, France) between 2008 and 2021.

- more than 1800 subjects
- pathological cases precisely annotated





Diffusion data



MarsFet cohort is an heterogeneous dataset due to the multiple acquisition protocols utilized.

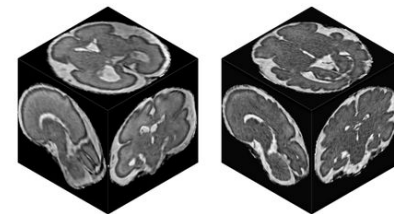
Variability:

- 4 different MRI scanners
- 1.5 and 3T
- 6, 12 or 30 directions
- TR and TE

Typical acquisition:

- one stack
- isotropic (2mm)
- single shell $b=1000 \text{ s.mm}^{-2}$
- no Reverse Phase Encoding

Anatomical data



Reconstructed T2w images are available but we decided not to use them

dHCP data

253 high quality fetal data

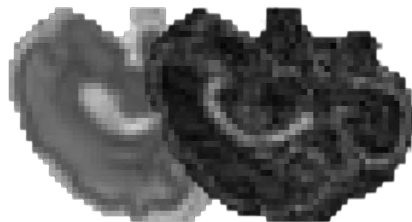
- b=0 (15 volumes)
- b=400 (46 volumes)
- b=1000 (80 volumes)
- SAFE sequence



dHCP pipeline

Code not available

1. Denoising
2. **Dynamic distortion correction**
3. Bias field correction
4. Brain mask
5. **Multi-shell reconstruction (SHARD)**

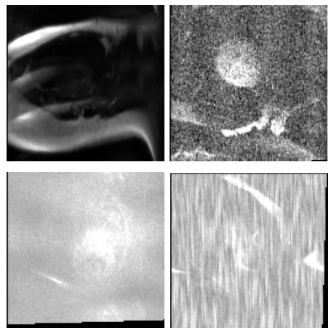


Need of pipeline
suitable for clinical
acquisitions

Initial QC

Visual inspection

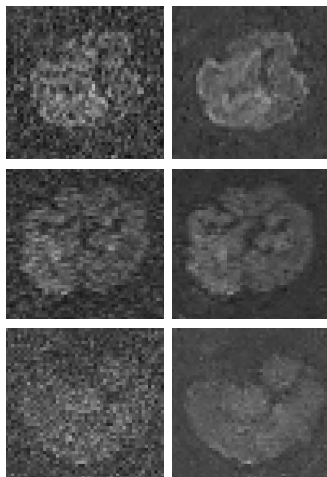
Exclusion of poor quality data (high noise and/or obvious artifacts)



~ 50 acquisition removed

Denoising

Marchenko–Pastur PCA

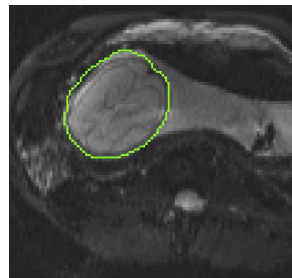


Brain extraction

FetalBET

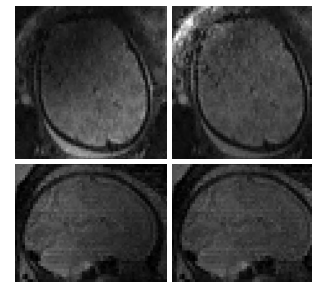


Brain mask extracted from the b0



Bias correction

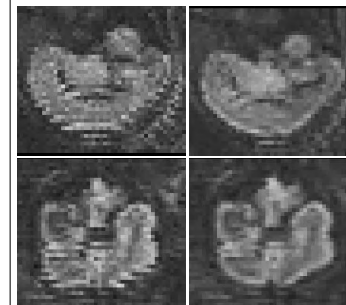
N4

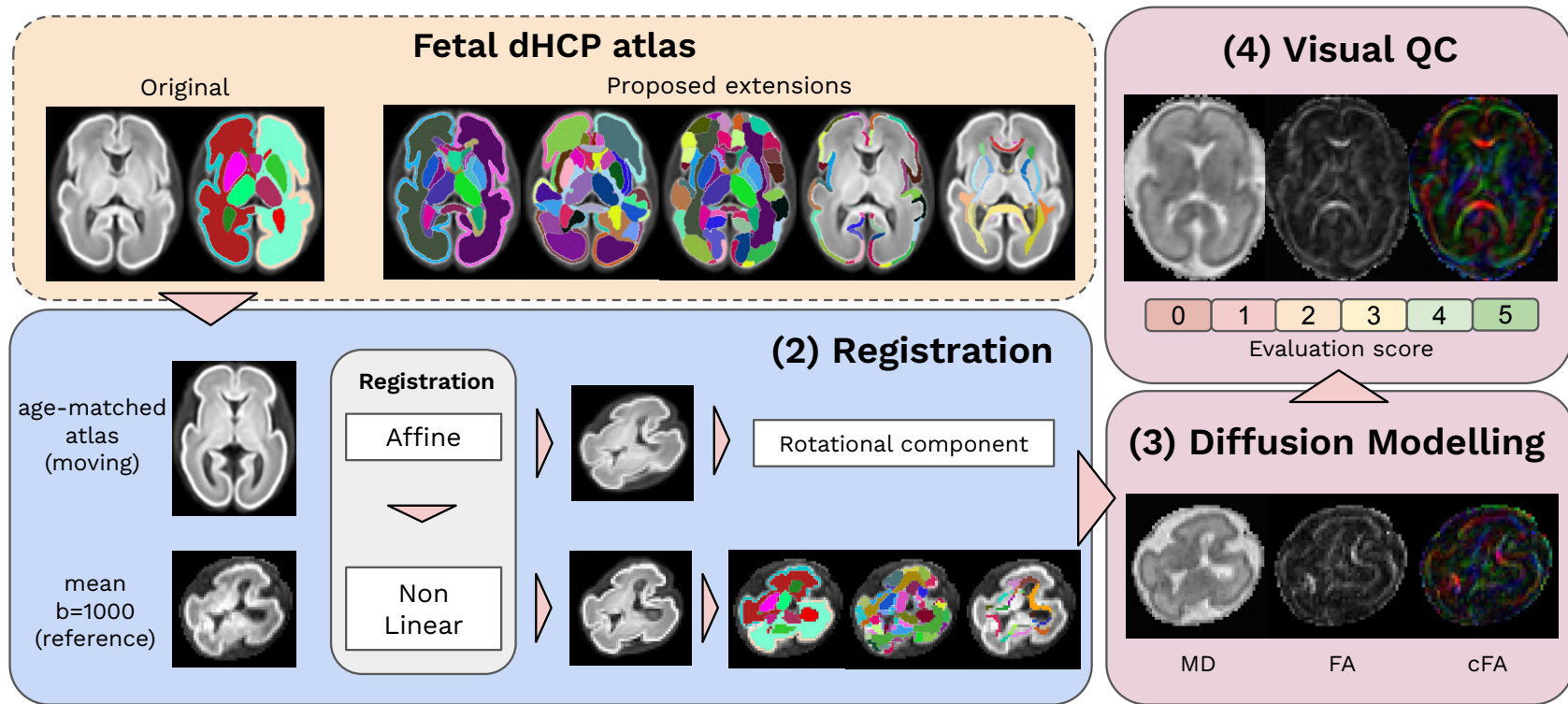


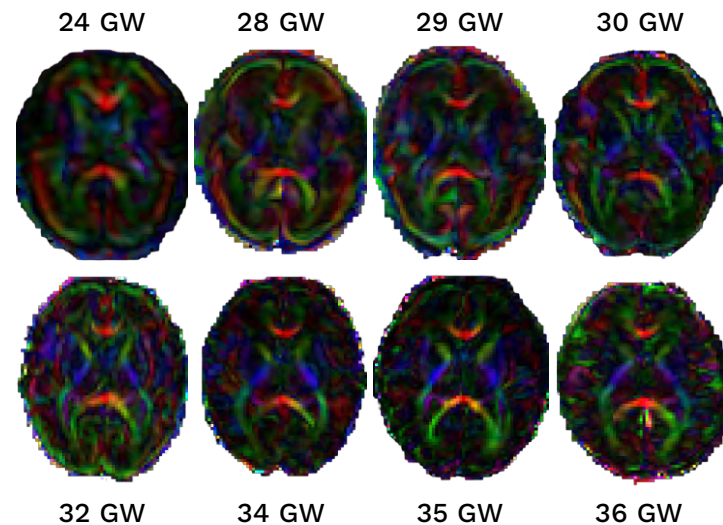
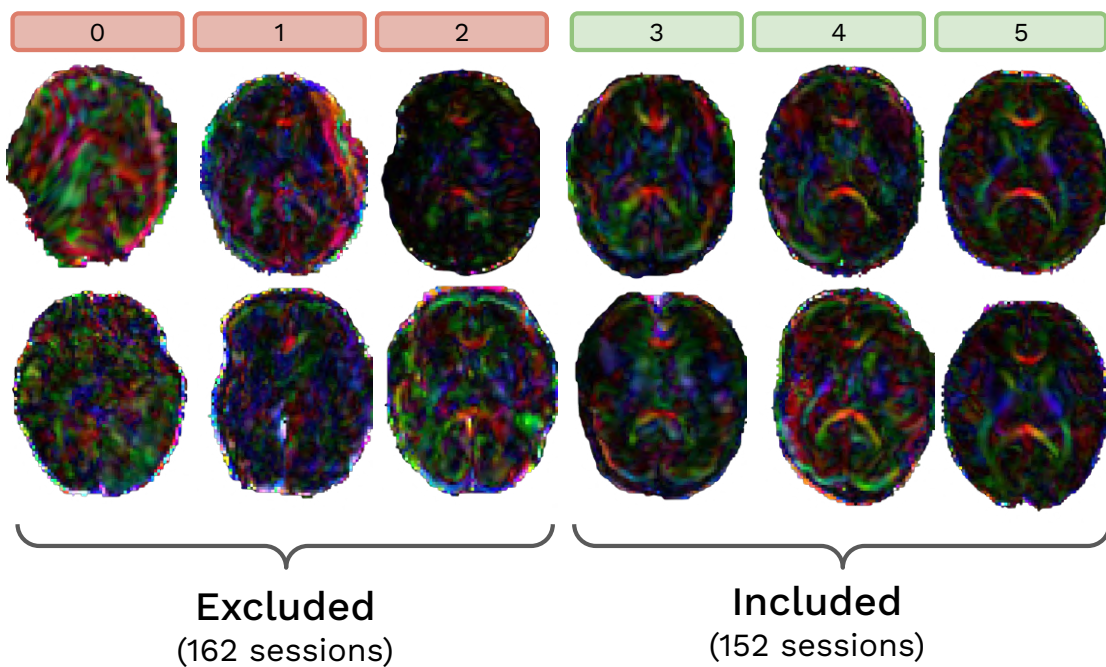
Motion Correction

FSL Eddy

- Slice2Volume
- outlier replacement





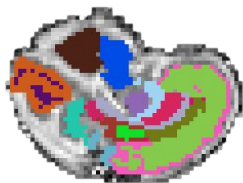
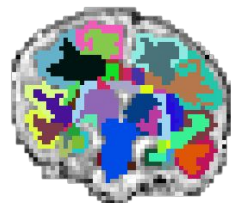
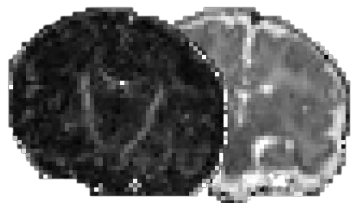
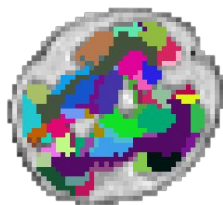


MarsFet

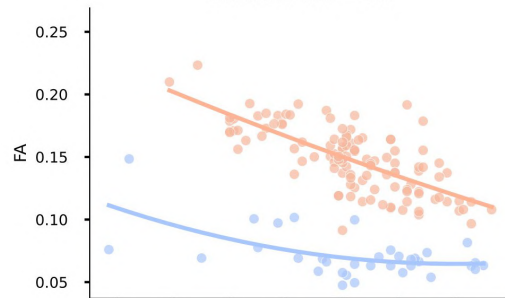
Trends

Tensor maps

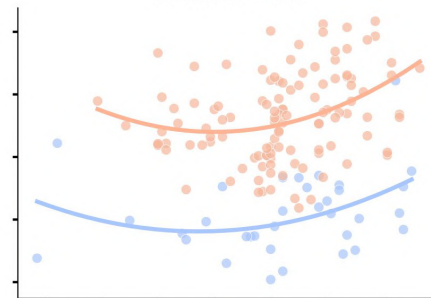
Parcellations



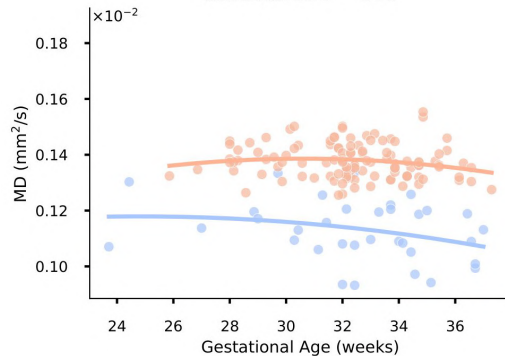
Cortical GM — FA



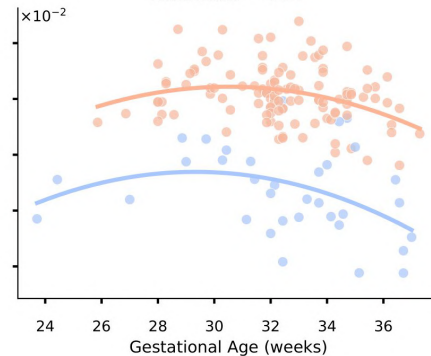
Isthmus — FA



Cortical GM — MD



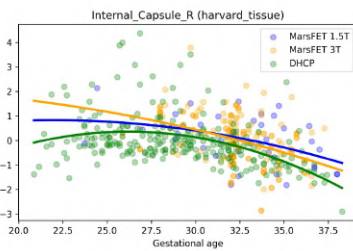
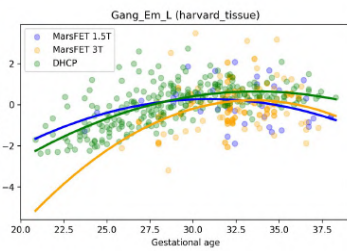
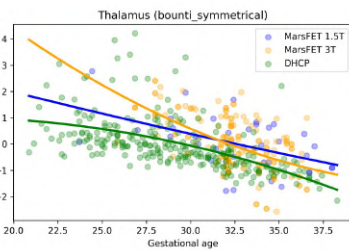
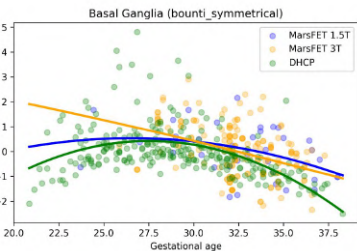
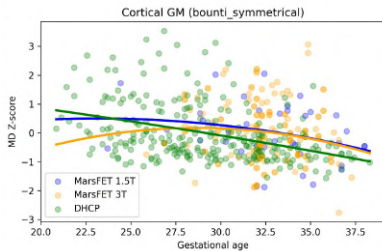
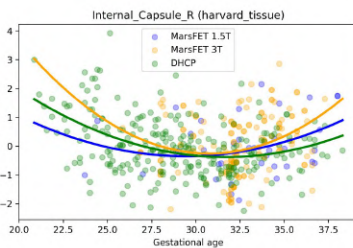
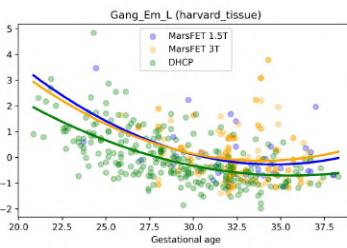
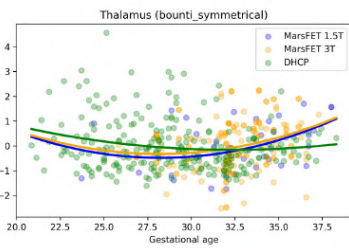
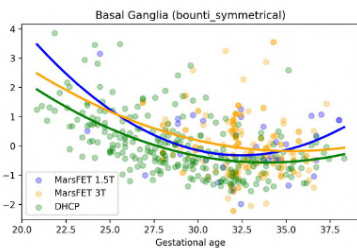
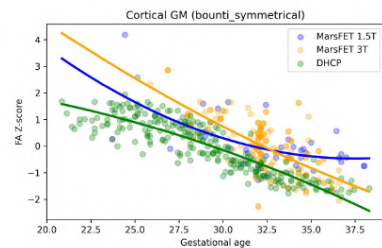
Isthmus — MD



— 1.5T — 3.0T

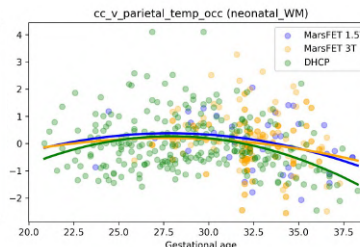
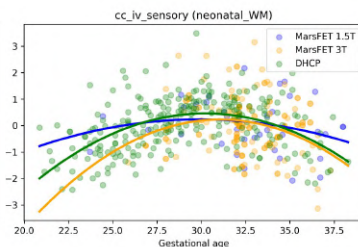
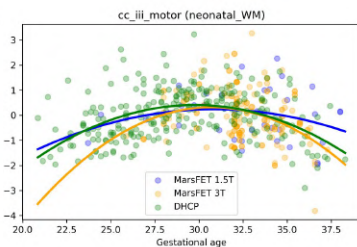
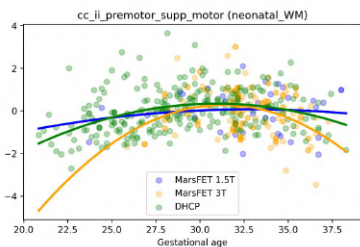
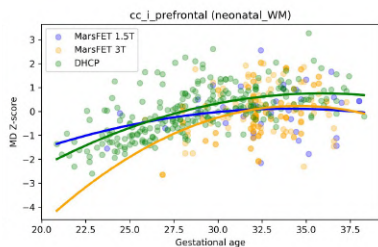
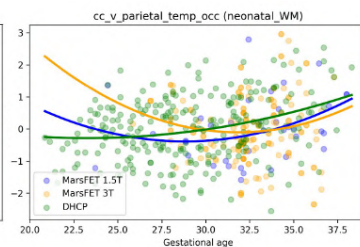
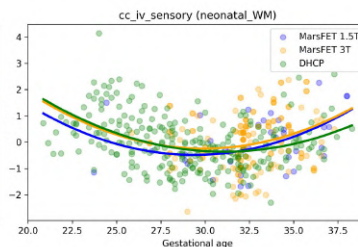
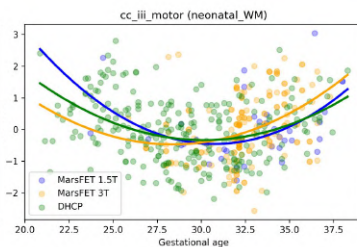
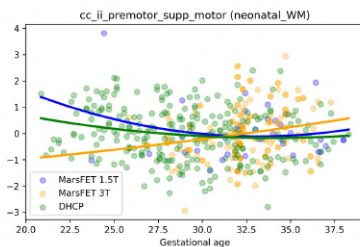
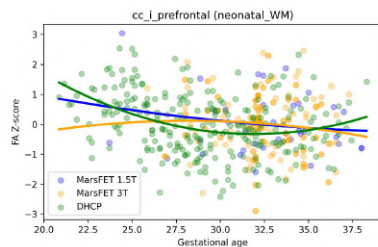
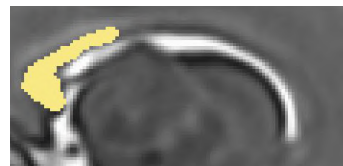
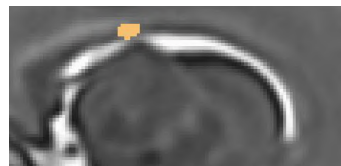
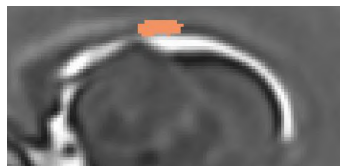
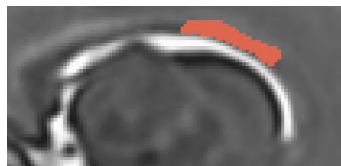
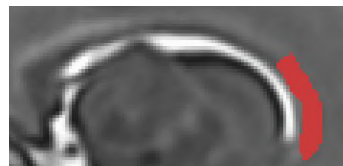
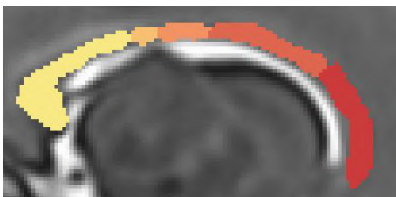
MarsFet

dHCP comparison

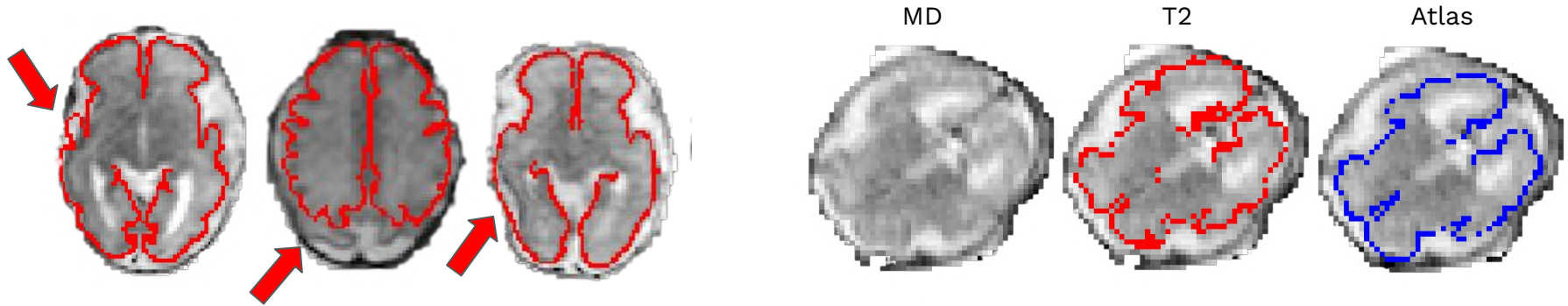


MarsFet

dHCP comparison



Improve parcellations in diffusion space using the subject reconstructed T2



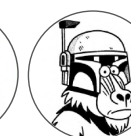
Need good quality anatomical reconstruction and segmentations

Outline

1. **Fetal Diffusion MRI:** challenges and limitations
2. **MarsFet:** clinical human acquisitions
3. **BaboFet:** research baboon acquisitions



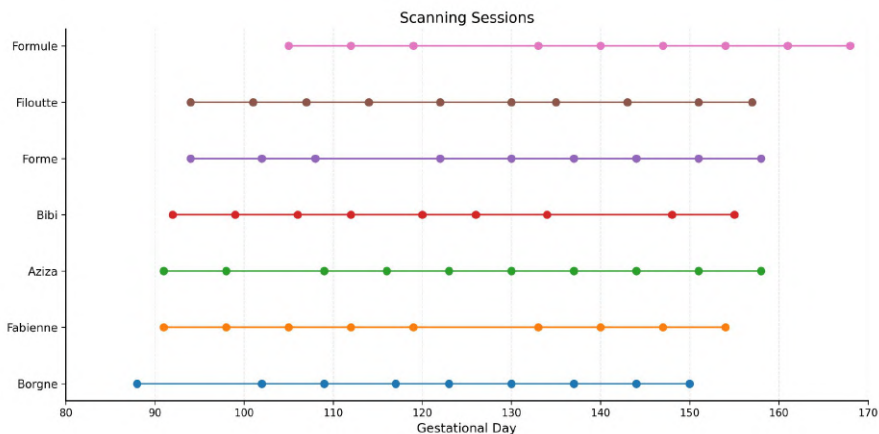
L. Renaud



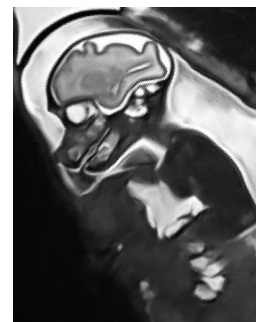
M. Clémenceau

Dataset of 7 pregnant baboons scanned longitudinally, once a week for 10 weeks, between 13wGA and 24wGA, acquired at CERIMED (Marseille, France).

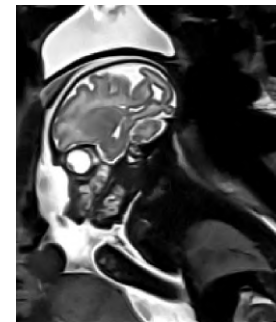
- **Anatomical:** 2D T2 HASTE 0.63x0.63x2 mm³
- **Diffusion:** 2D Spin Echo EPI, 1.1x1.1x3 mm³, 30 directions, b=1000s.mm⁻²
- **Functional:** 2D Gradient-recalled Echo EPI, 2.5x2.5x2.5 mm³, TR/TE=2000/30ms



14w



18w



22w



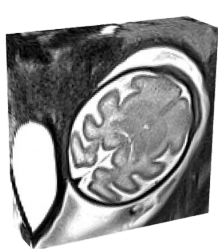
L. Renaud



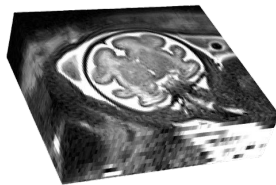
M. Clémenceau

Six 2D stacks of thick slices, 2 per plane with half voxel overlap.
Allow for super-resolution reconstruction

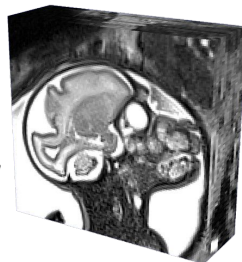
Anatomical



Axial



Coronal

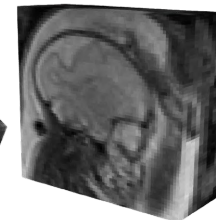
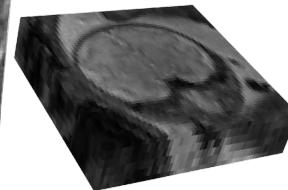
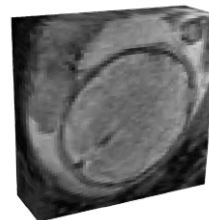


Sagittal

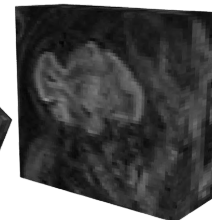
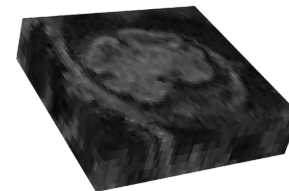
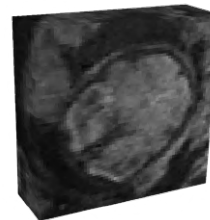
x2

Diffusion

b0



dwi

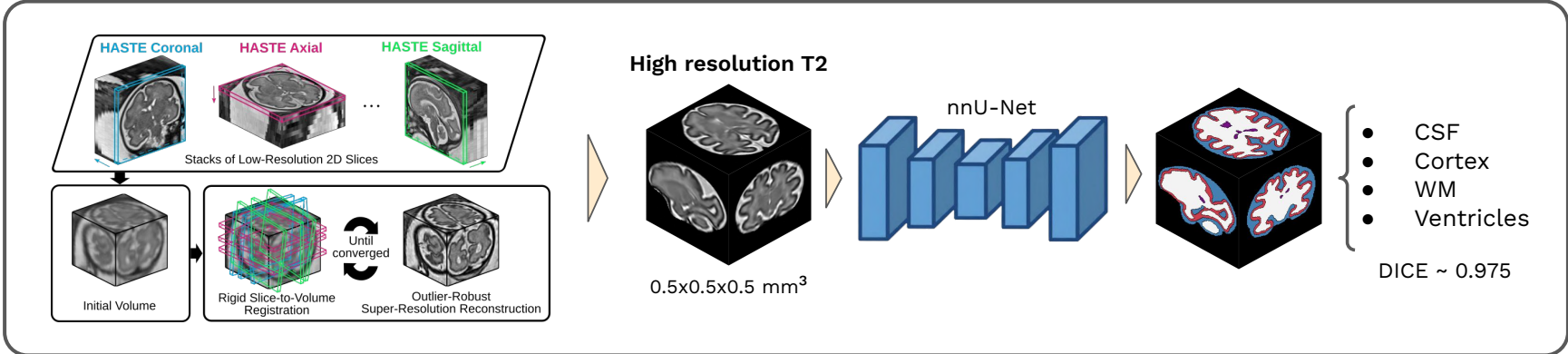


Axial

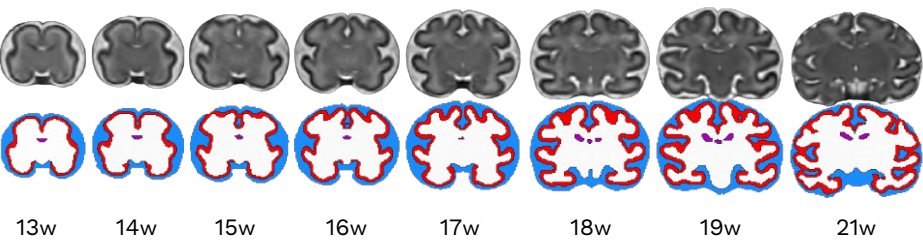
Coronal

Sagittal

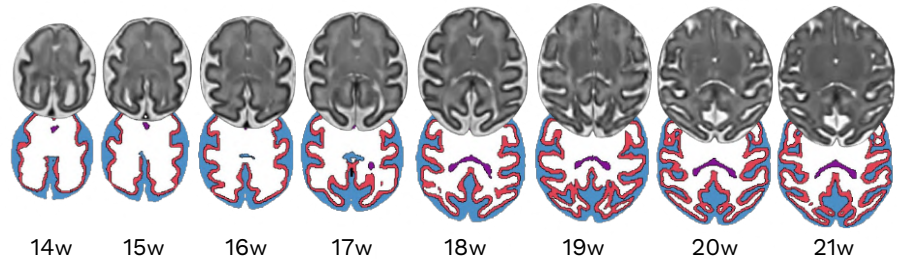
x2



Sub-Bibi



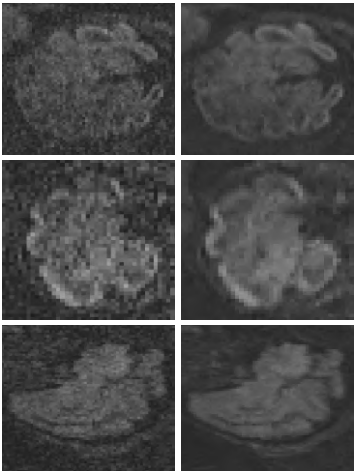
Sub-Borgne



Ebner et al., "An automated framework for localization, segmentation and super-resolution reconstruction of fetal brain MRI", Neuroimage, 2020
Isensee et al., "nnU-Net: a self-configuring method for deep learning-based biomedical image segmentation," Nature Methods, 2021

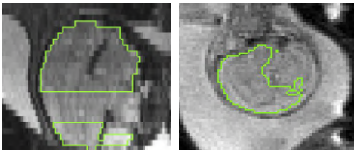
Denoising

Marchenko-Pastur PCA
and
Gibbs ringing removal



Brain extraction

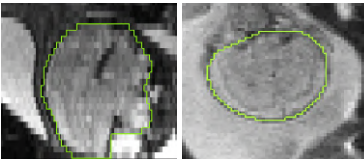
FetalBET struggles with baboons



Trained **nnUNet** on 359
b0 volumes

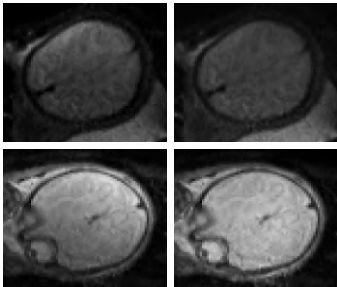


Dice: 0.959 ± 0.017

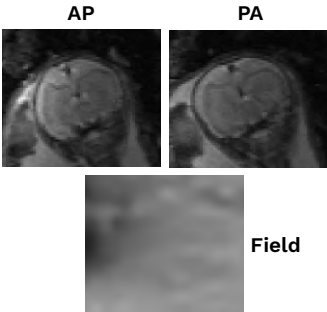


Bias and Distortion correction

N4 Bias correction



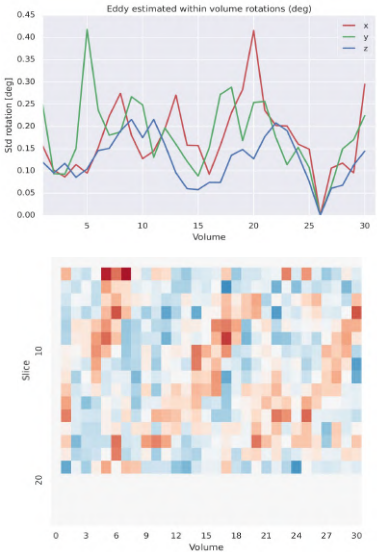
Topup



Motion Correction

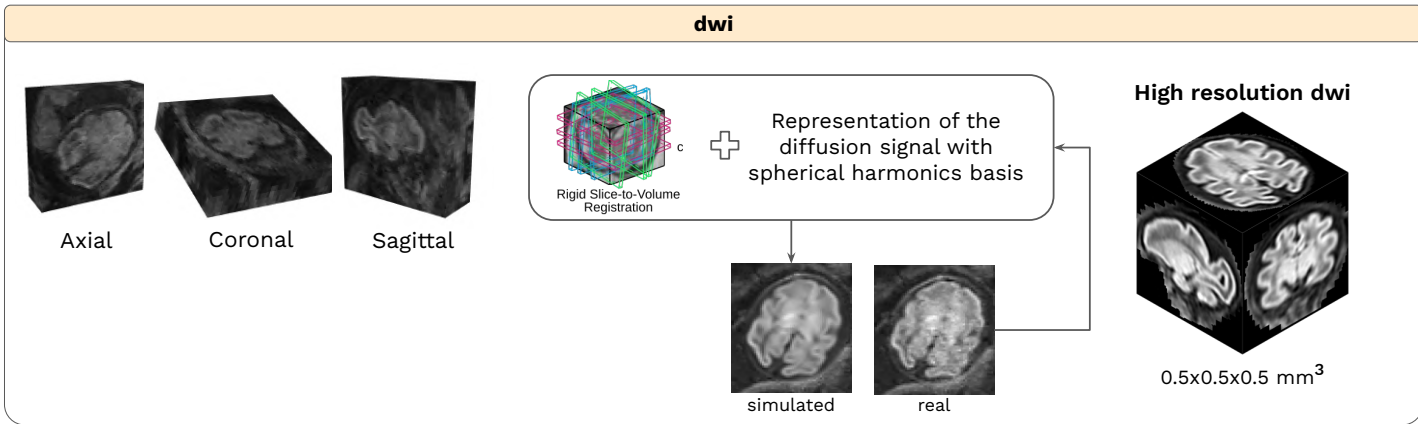
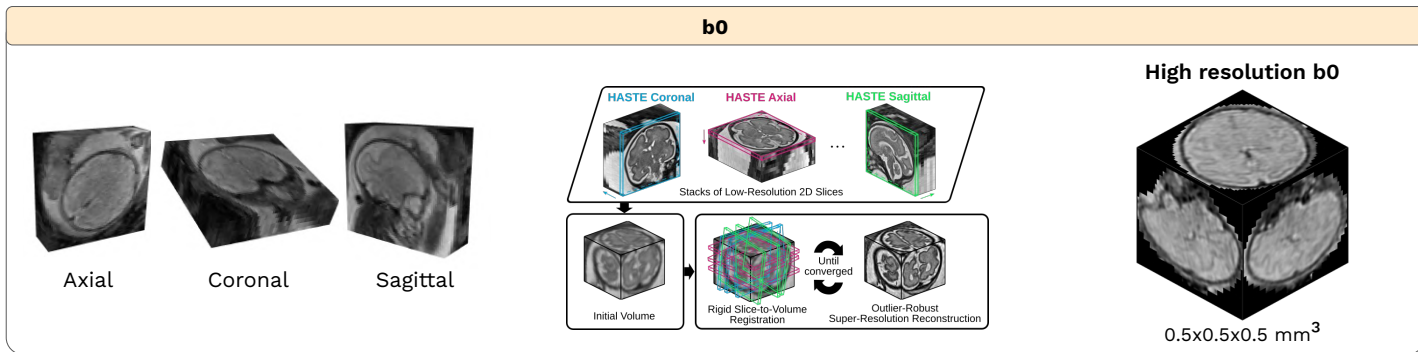
FSL Eddy

- Slice2Volume
- outlier replacement



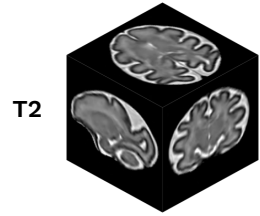
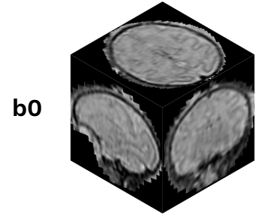
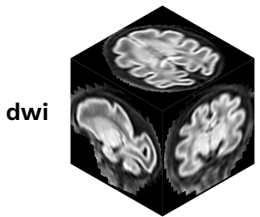
BaboFet

Super-resolution reconstruction

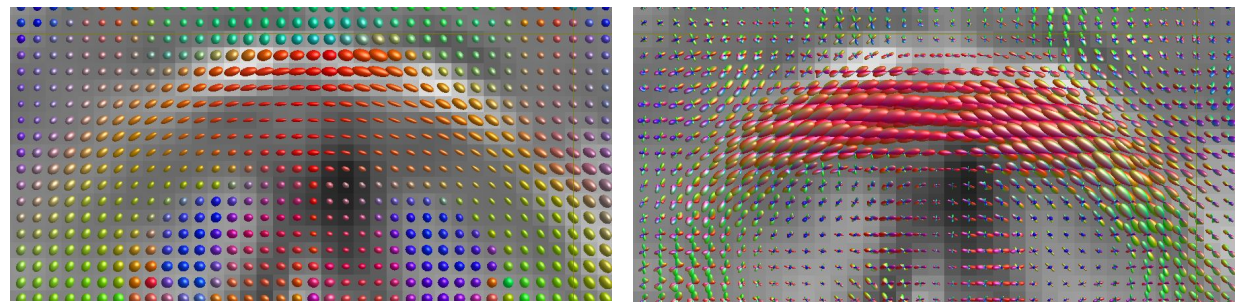


Spatially aligned

Rigid registration
 $b_0 \rightarrow T_2 \rightarrow dwi$

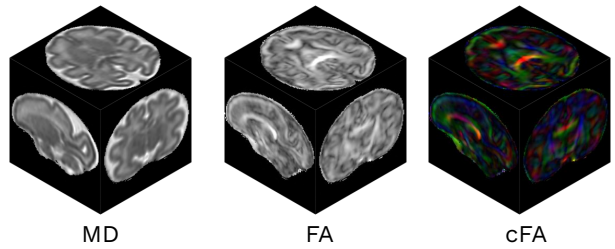


Diffusion models

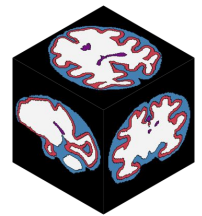


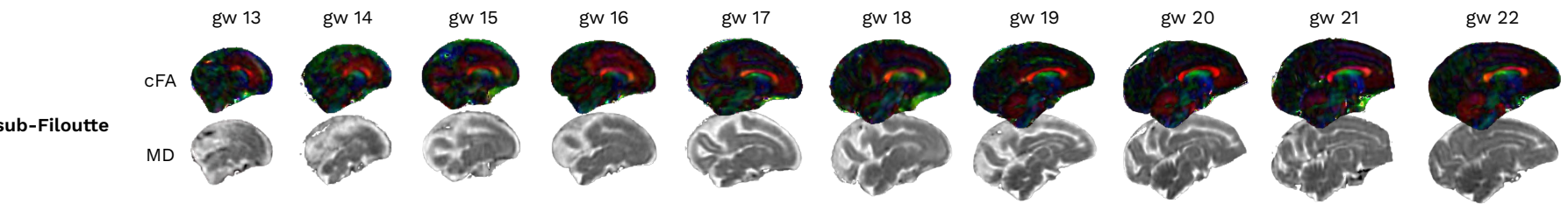
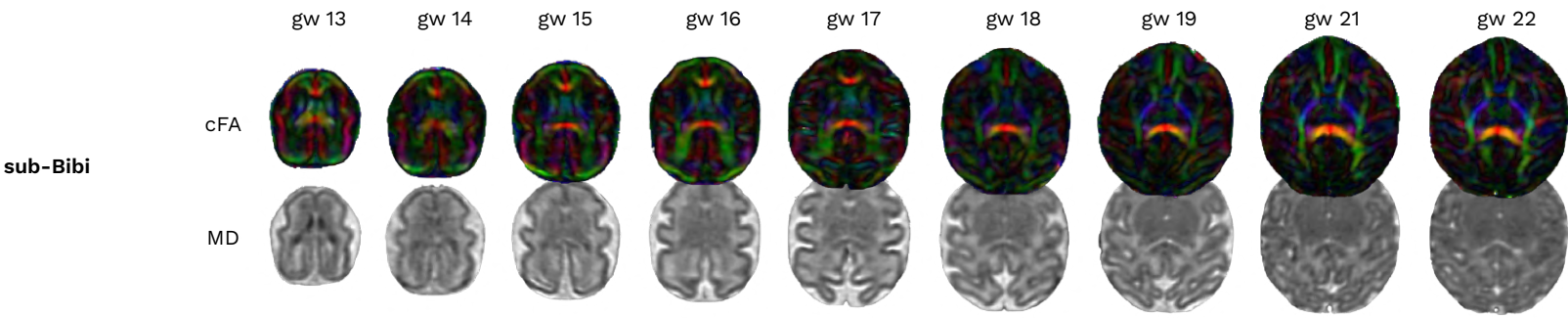
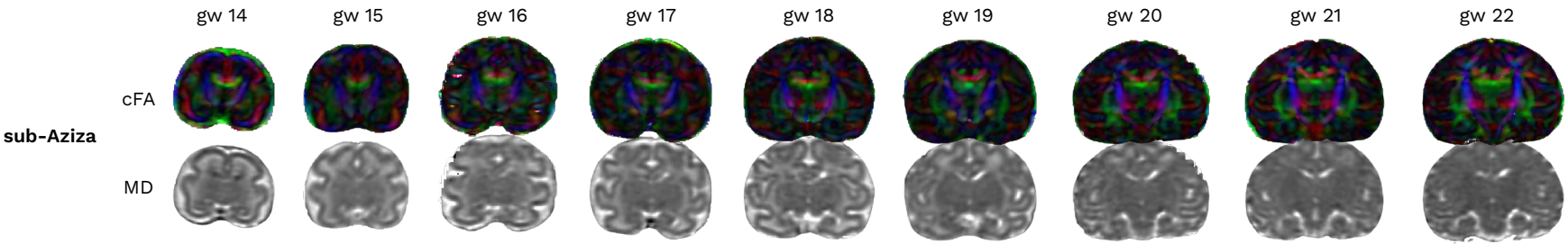
with Constrained Spherical Deconvolution

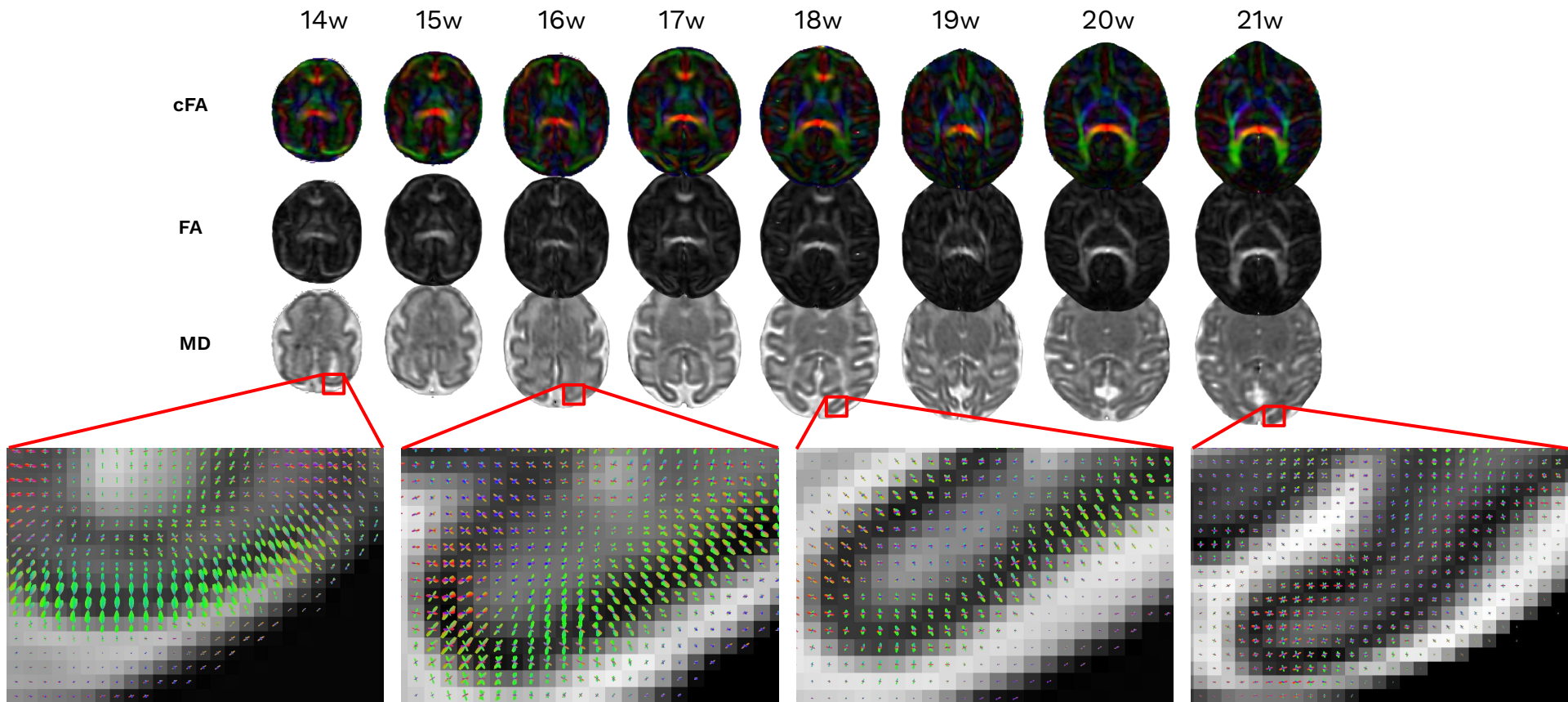
Metrics are derived from the tensor



Propagate the T2w masks

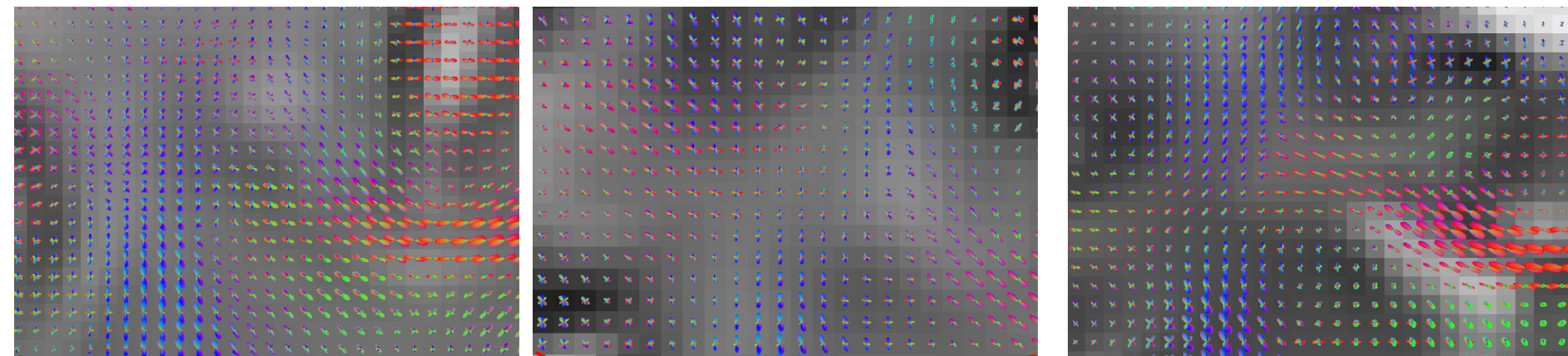






BaboFet

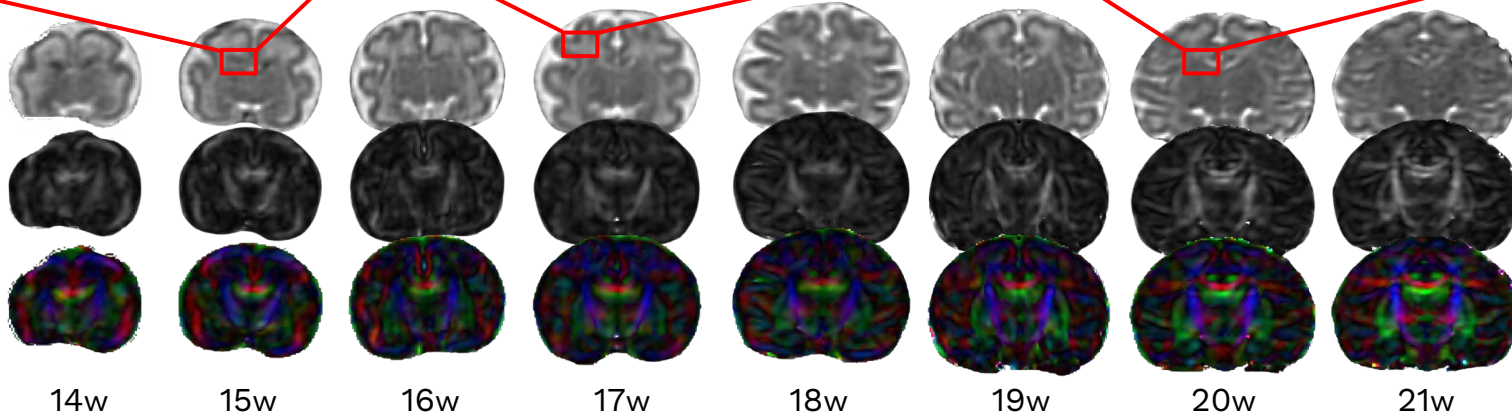
Results - crossing fibers

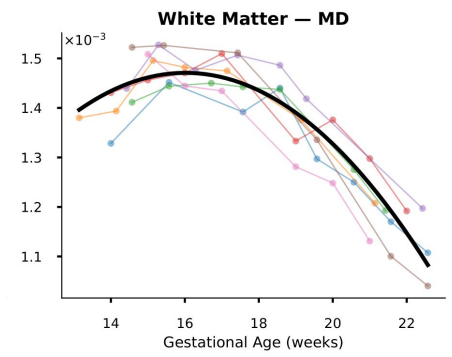
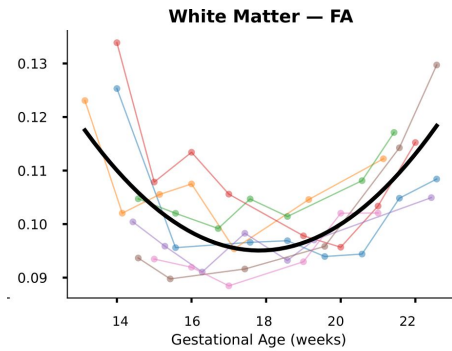
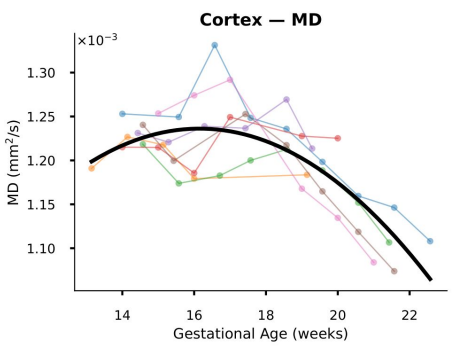
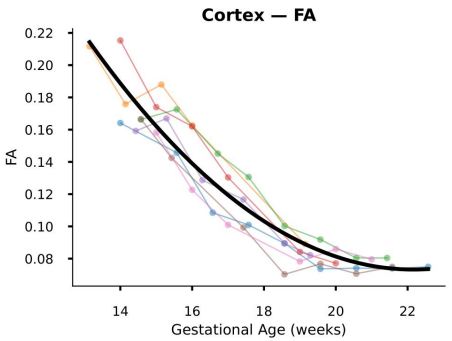
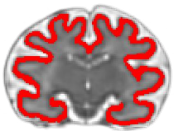


cFA

FA

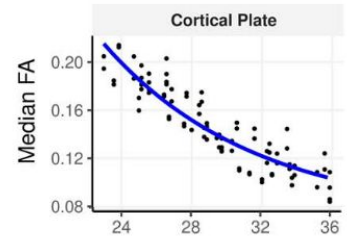
MD



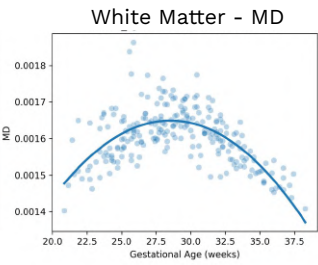
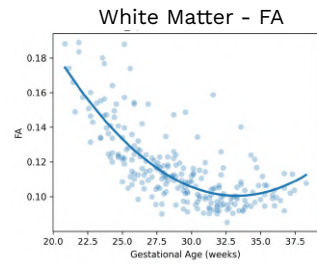


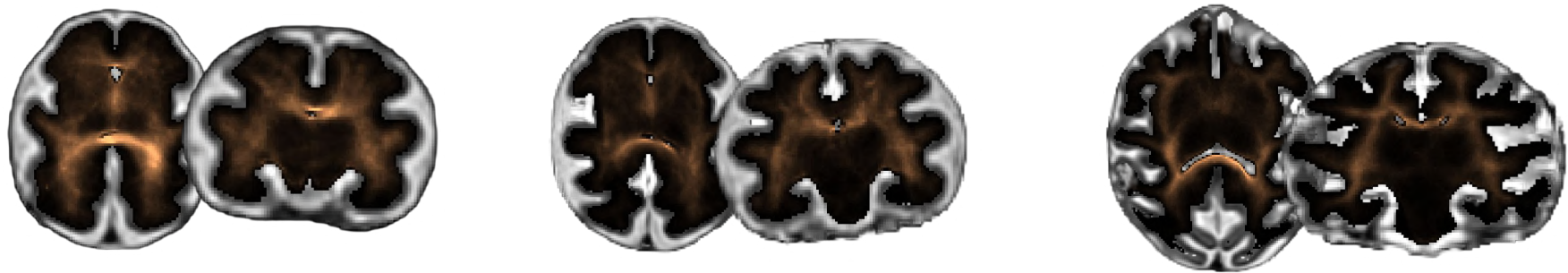
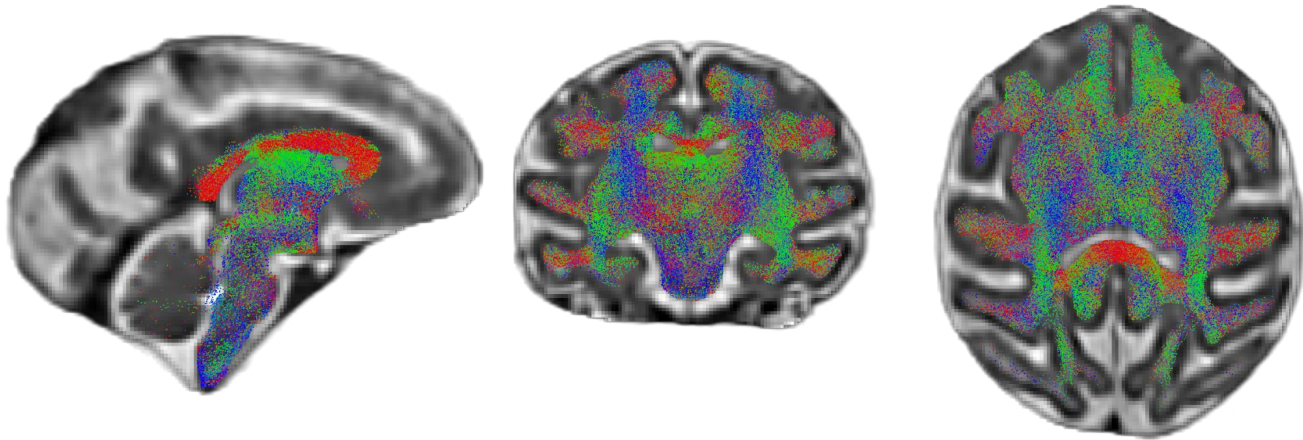
Literature

Calixto et al, Cerebral Cortex



dHCP trends





THE PEOPLE



G. Auzias



O. Coulon



F. Rousseau



J. Sein



N. Girard



B. Leroux



D. Menieur



H. Dienye



M. Clémenceau



L. Renaud



L. Velly



A. Le Troter



B. Nazarian



J.-L. Anton



A. Manchon



M. Milh

THANK YOU!