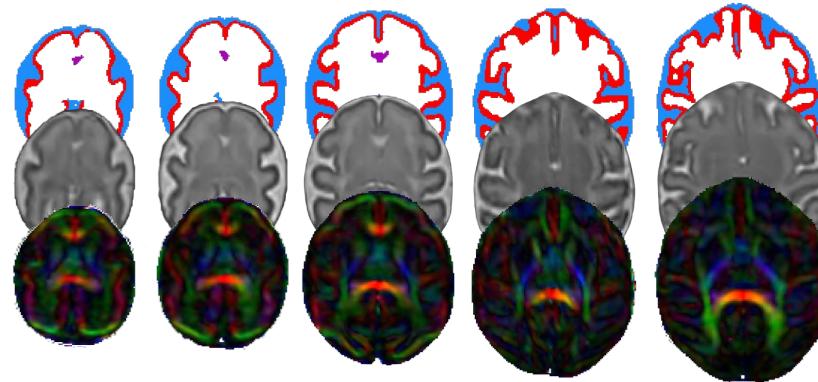
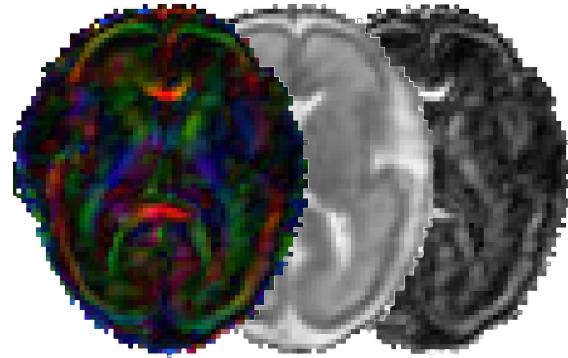


Processing and Analysis of Fetal Diffusion MRI

From Clinical Human Imaging to Longitudinal Baboon Research Data

Mattia Cazzolla



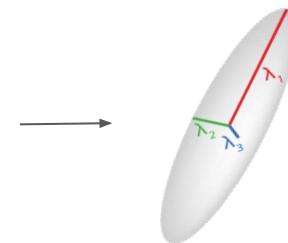
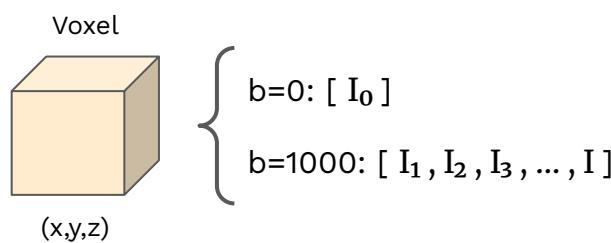
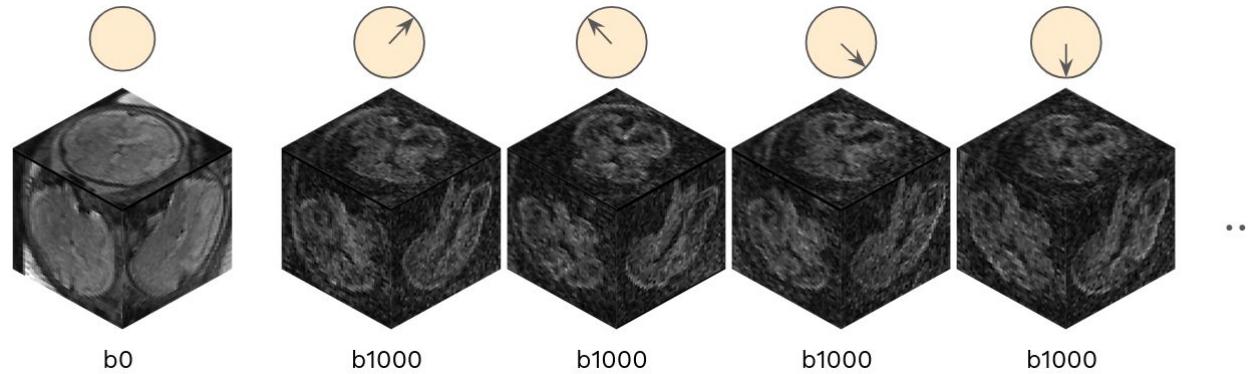
Outline

1. **Fetal Diffusion MRI:** opportunities and challenges
2. **MarsFet:** clinical human acquisitions
3. **BaboFet:** research baboon acquisitions

Fetal Diffusion MRI

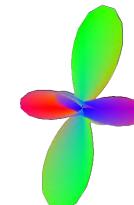
Introduction

Diffusion MRI allow to study microstructural tissues information by measuring the **signal attenuation** caused by water **diffusion** in a specific direction



Tensor model

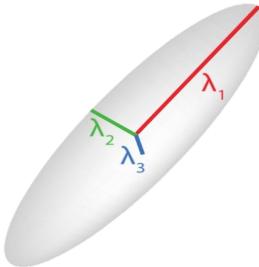
$$S_{DWI} = S_{b=0} \times e^{(-b \times D)}$$
$$D = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{yx} & D_{yy} & D_{yz} \\ D_{zx} & D_{zy} & D_{zz} \end{bmatrix}$$



Higher order
models

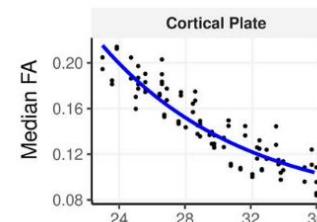
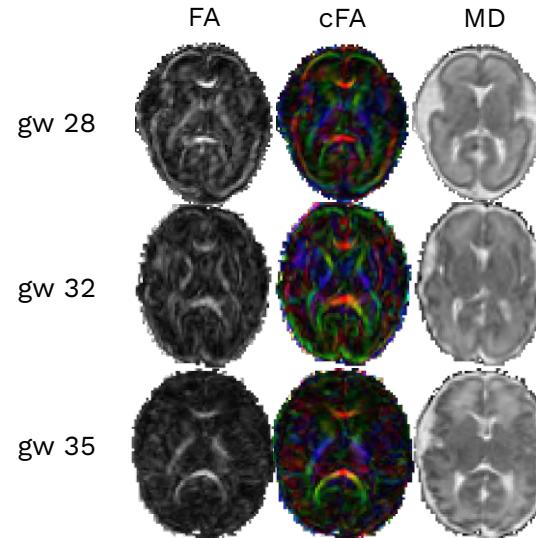
Fetal Diffusion MRI

Introduction

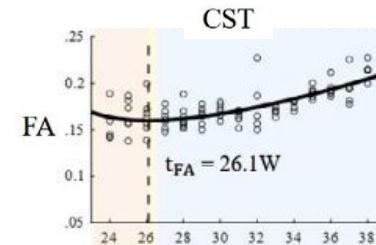


From the tensor can extract metrics:

- **Fractional Anisotropy** (dominant diffusion direction)
- **Mean Diffusivity** (proxy for water content)
- Axial and Radial Diffusivity



Calixto et al, Cerebral Cortex



Chen et al, Neuroimage

Do different cortical/white matter areas develop with different dynamics?

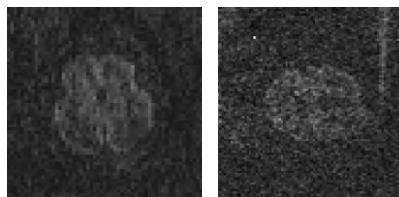
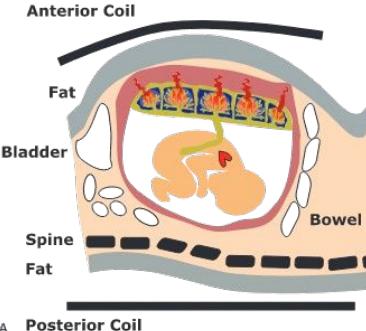
Fetal Diffusion MRI

Challenges - ROI

Coils

Maternal tissue between fetal brain and MRI coils

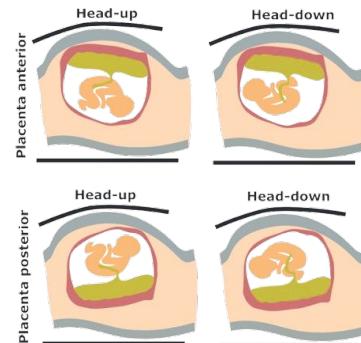
low SNR



Non standard orientation

Non standard orientation relative to scanner

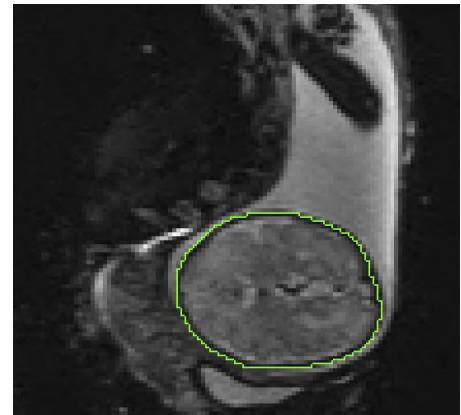
wrong color maps



Brain extraction

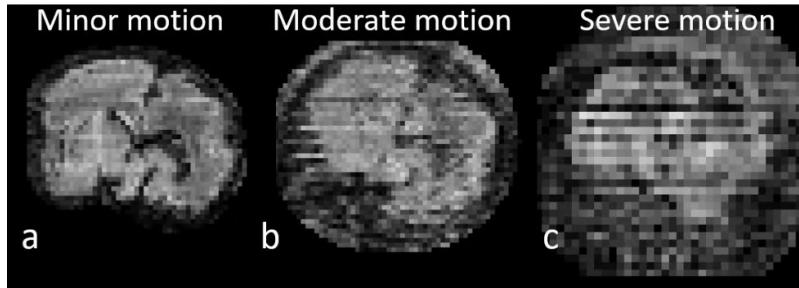
Brain needs to be located and extracted

need for specific tools



Fetal Diffusion MRI

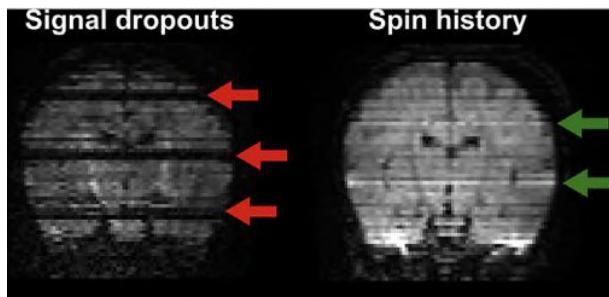
Challenges - Motion



Caused by:

- maternal breathing
- fetal motion

Motion can be assumed frozen during the readout of each slice.



Motion can cause:

- signal dropout
- slice cross-talks artifacts

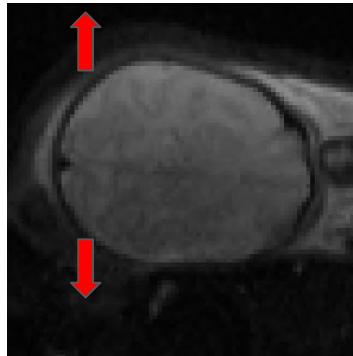
Fetal Diffusion MRI

Challenges - Geometrical distortions

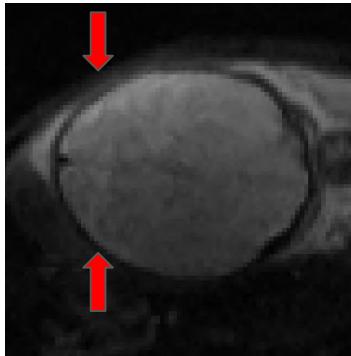
Fetal dMRI rely on EPI (Echo Planar Imaging) for efficient data acquisition.
But EPI suffer from local geometric distortions:

Magnetic Susceptibility

b0 with **AP** phase encoding



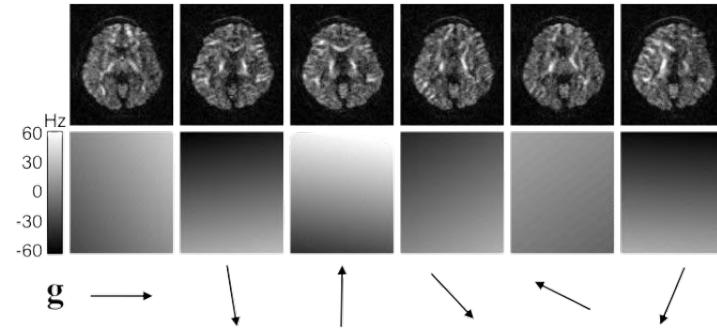
b0 with **PA** phase encoding



differences of **magnetic susceptibility** at tissue/air interface

Eddy currents

Bandwidth: 19.7 Hz/pixel Phase-encode direction: ←



rapid switch of diffusion gradients generate currents in nearby conductors

Outline

1. **Fetal Diffusion MRI:** challenges and limitations
2. **MarsFet:** clinical human acquisitions
3. **BaboFet:** research baboon acquisitions

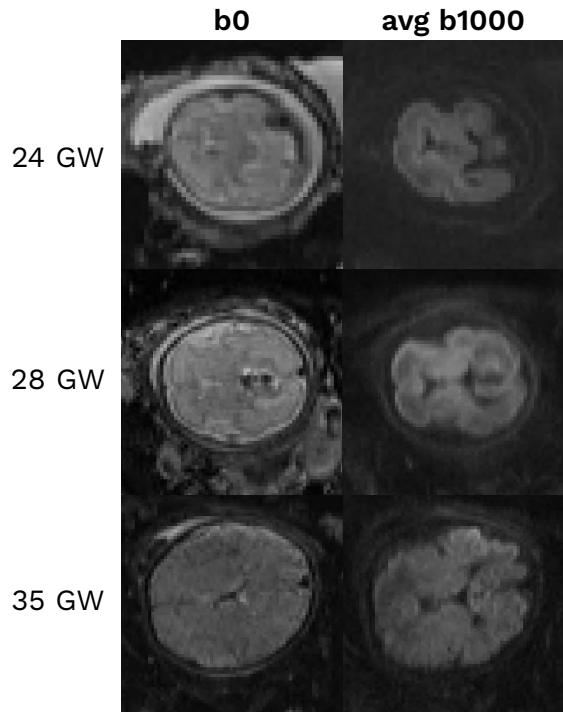
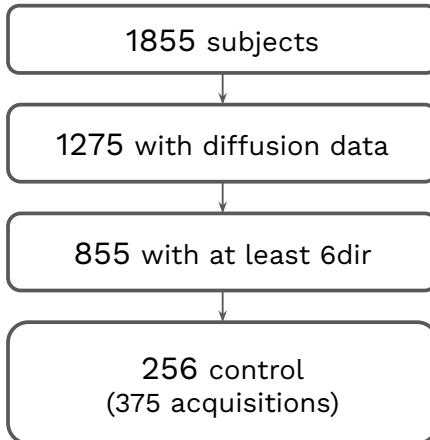
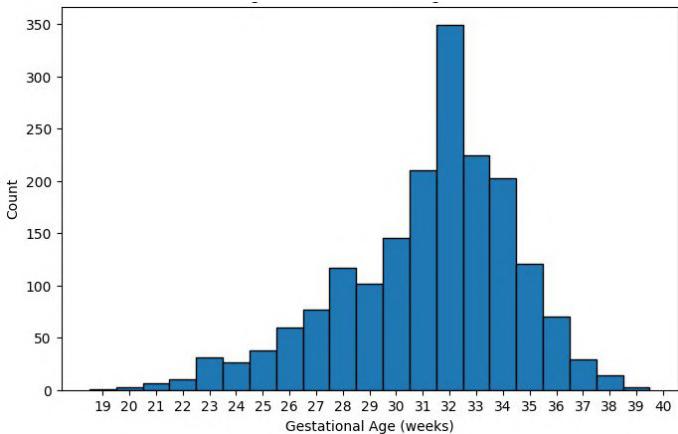
MarsFet

Dataset



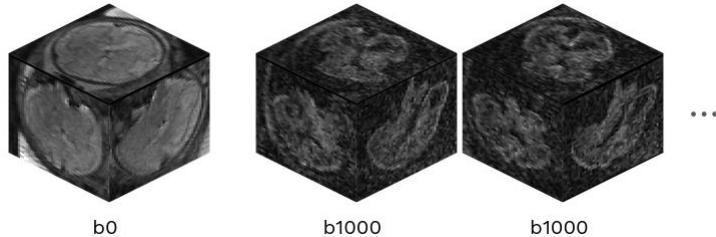
Large-scale fetal MRI dataset acquired during routine clinical examinations at *La Timone University Hospital* (Marseille, France) between 2008 and 2021.

- more than 1800 subjects
- pathological cases precisely annotated

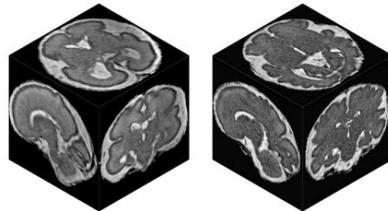




Diffusion data



Anatomical data



MarsFet cohort is an heterogeneous dataset due to the multiple acquisition protocols utilized.

Variability:

- 4 different MRI scanners
- 1.5 and 3T
- 6, 12 or 30 directions
- TR and TE

Typical acquisition:

- one stack
- isotropic (2mm)
- single shell $b=1000 \text{ s.mm}^{-2}$
- no Reverse Phase Encoding

Reconstructed T2w images are available but we decided not to use them

dHCP data

253 high quality fetal data

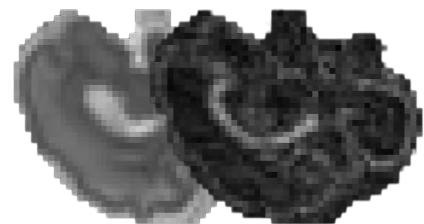
- $b=0$ (15 volumes)
- $b=400$ (46 volumes)
- $b=1000$ (80 volumes)
- SAFE sequence



dHCP pipeline

Code not available

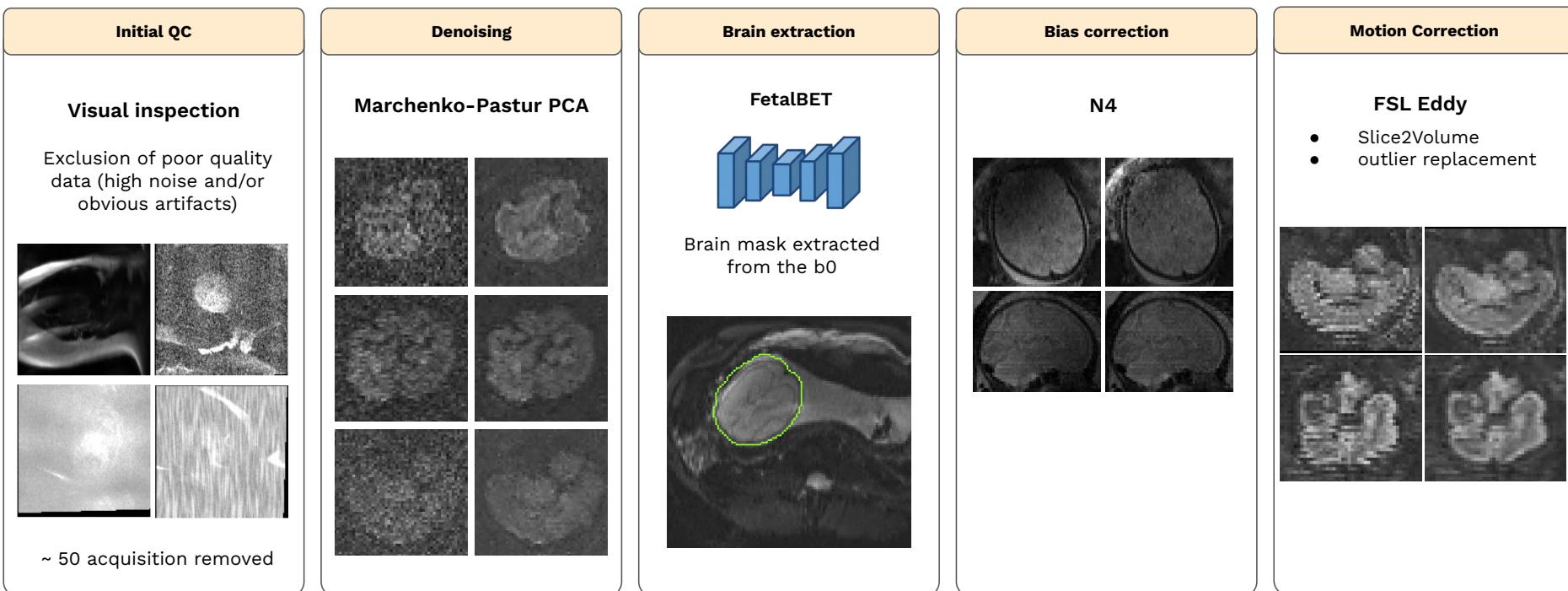
1. Denoising
2. **Dynamic distortion correction**
3. Bias field correction
4. Brain mask
5. **Multi-shell reconstruction (SHARD)**



Need of pipeline
suitable for clinical
acquisitions

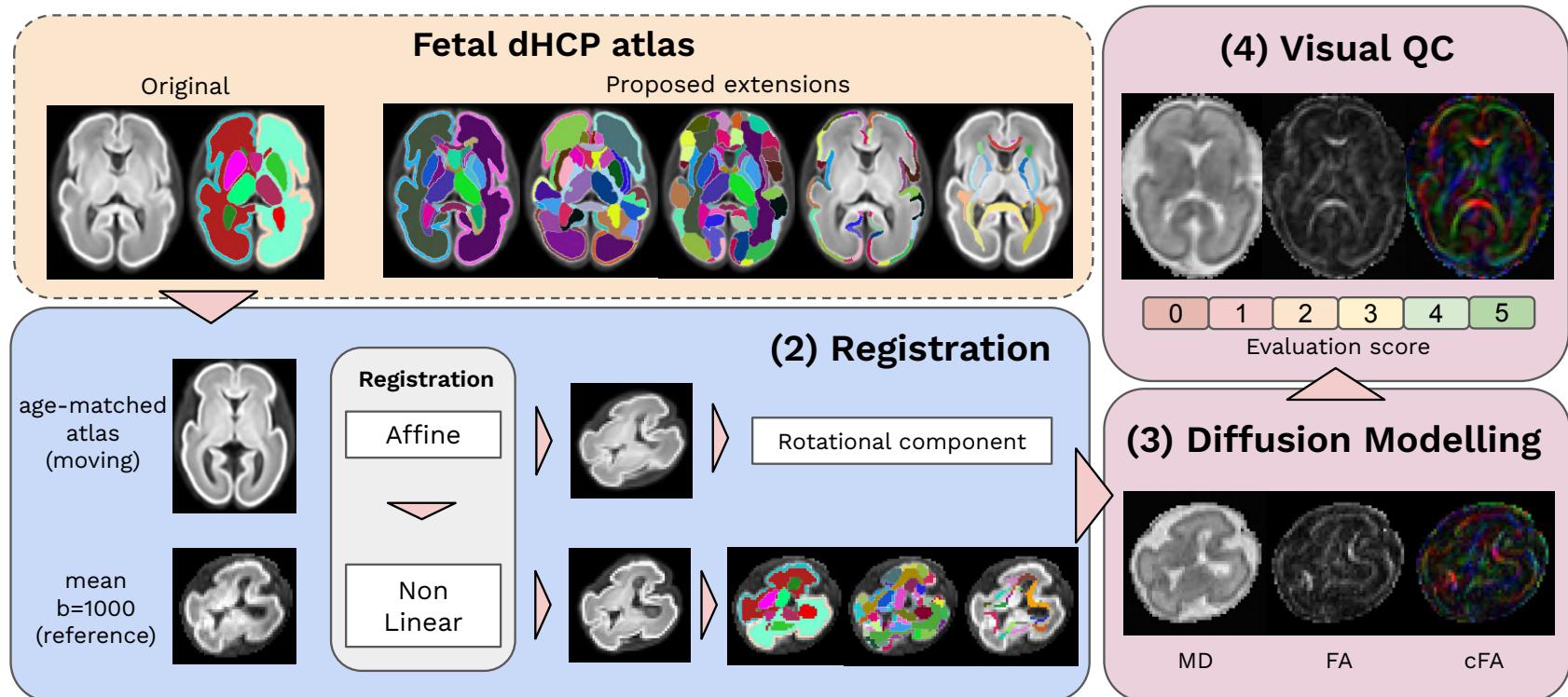
MarsFet

Processing pipeline



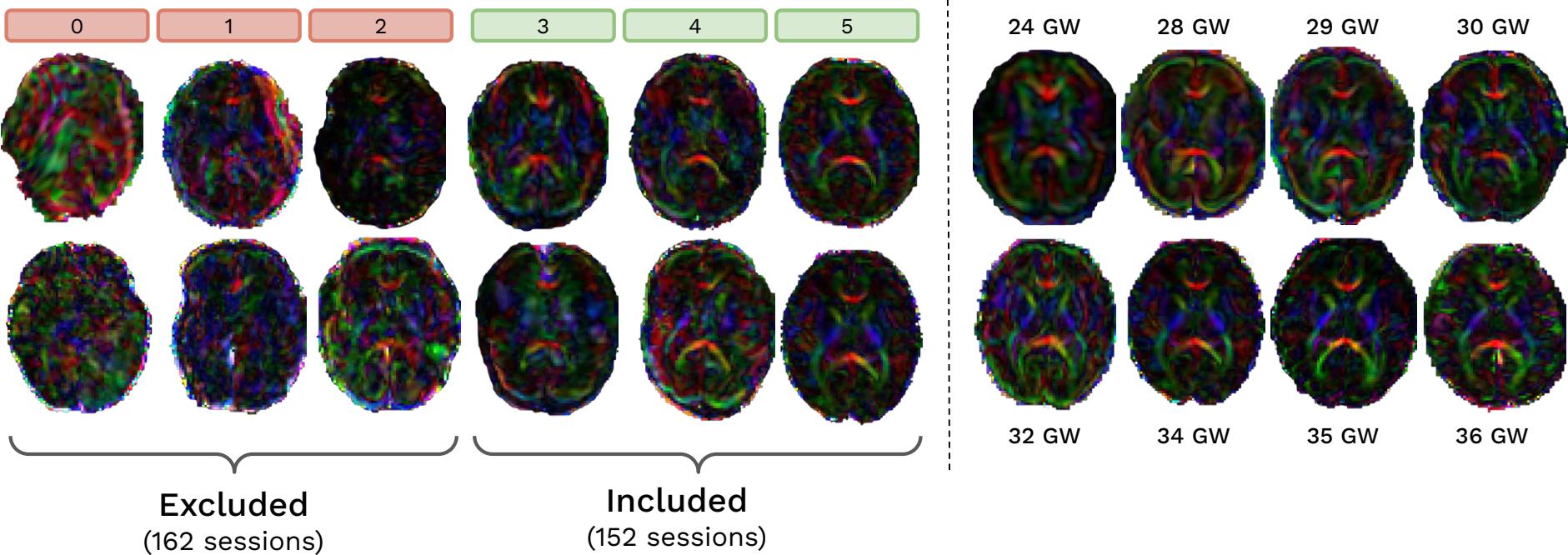
MarsFet

Processing pipeline



MarsFet

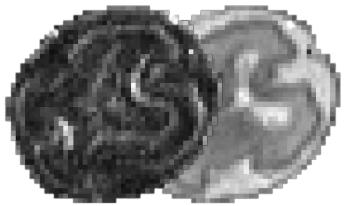
Results



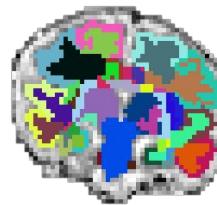
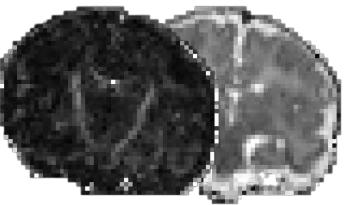
MarsFet

Trends

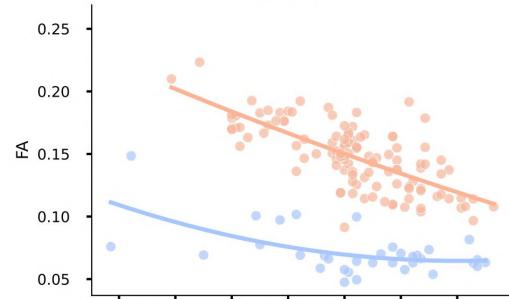
Tensor maps



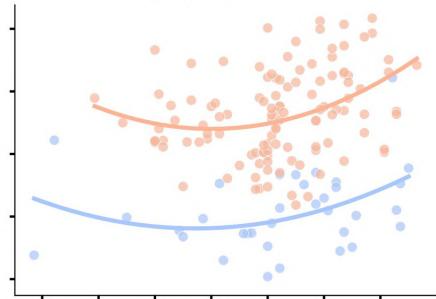
Parcellations



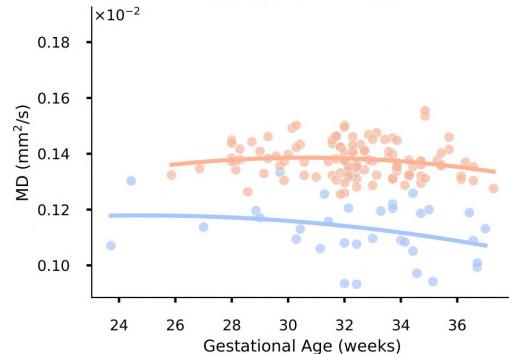
Cortical GM — FA



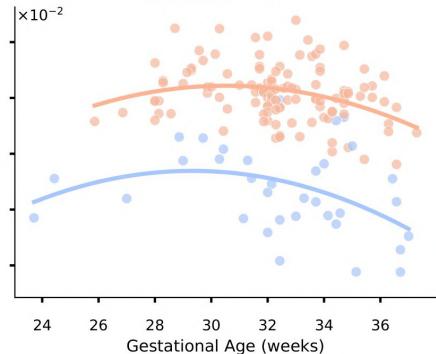
Isthmus — FA



Cortical GM — MD



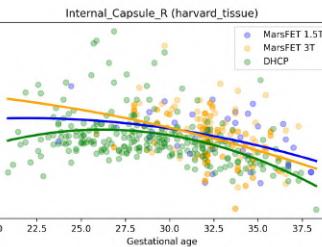
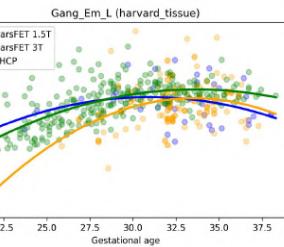
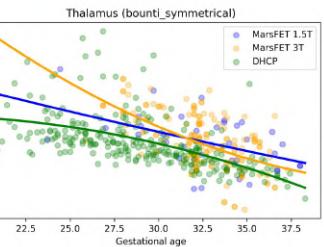
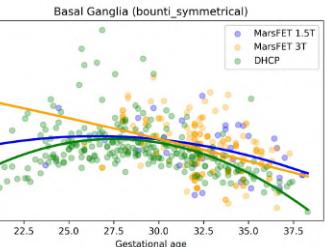
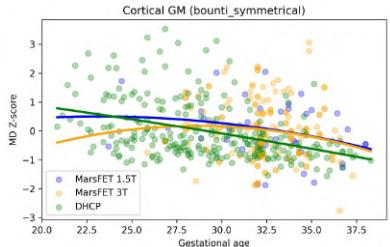
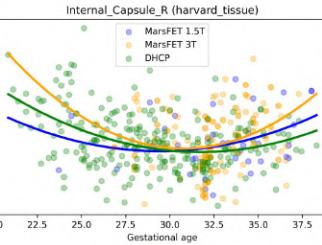
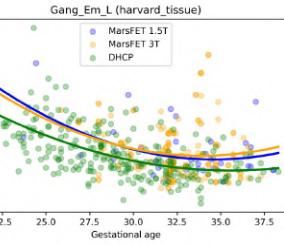
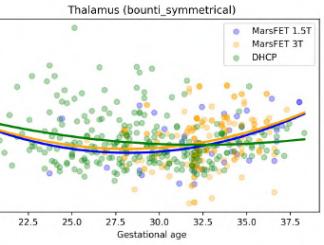
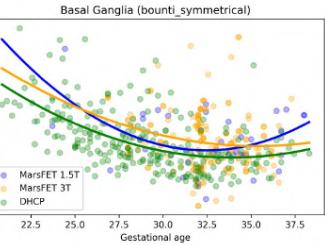
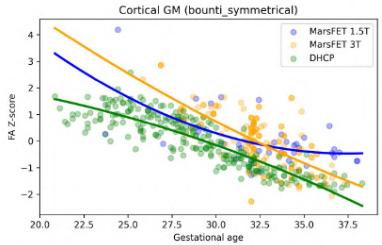
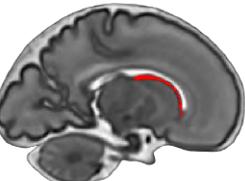
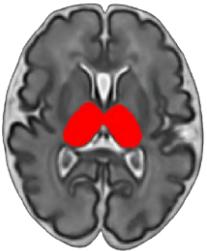
Isthmus — MD



— 1.5T — 3.0T

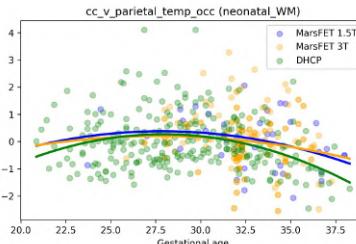
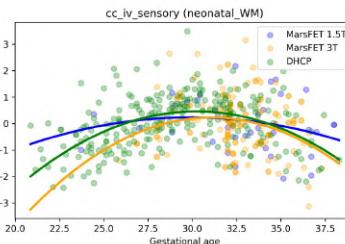
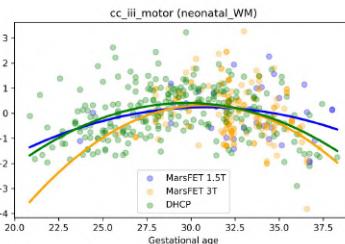
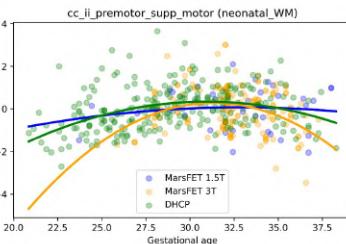
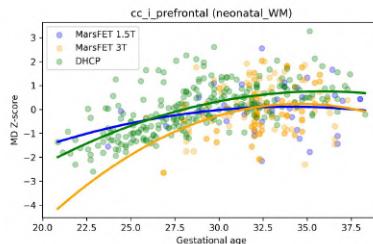
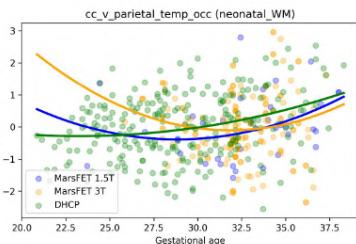
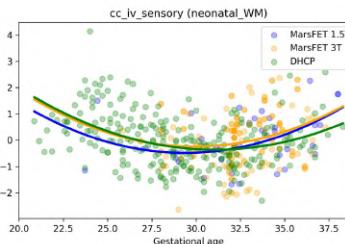
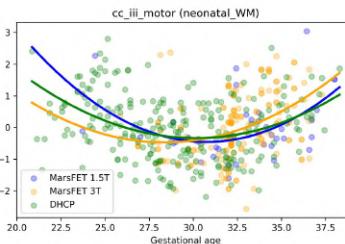
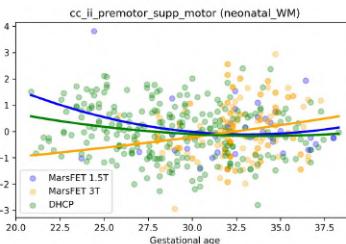
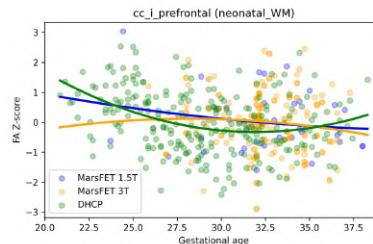
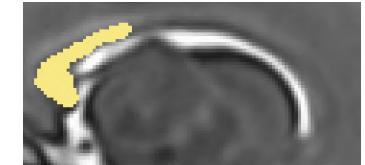
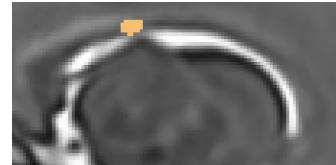
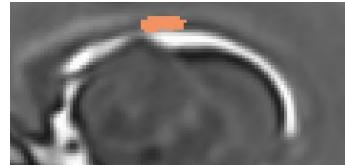
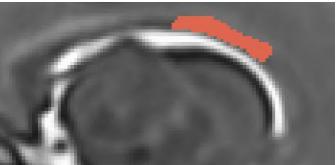
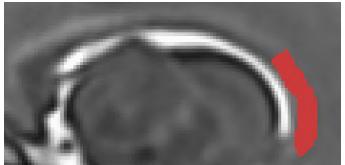
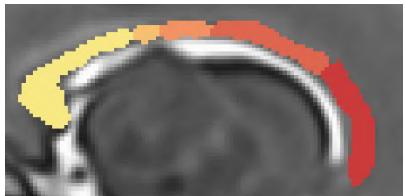
MarsFet

dHCP comparison

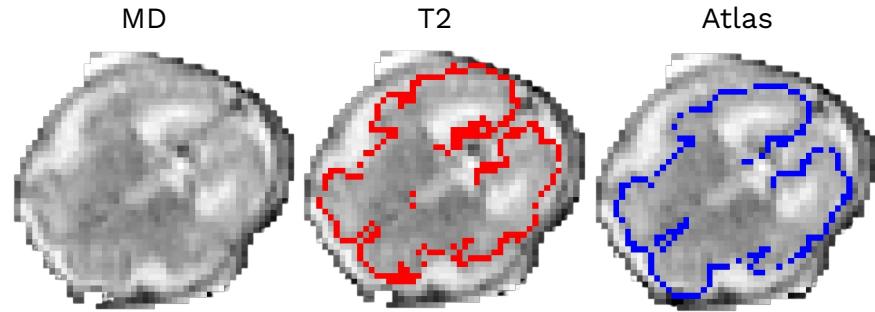
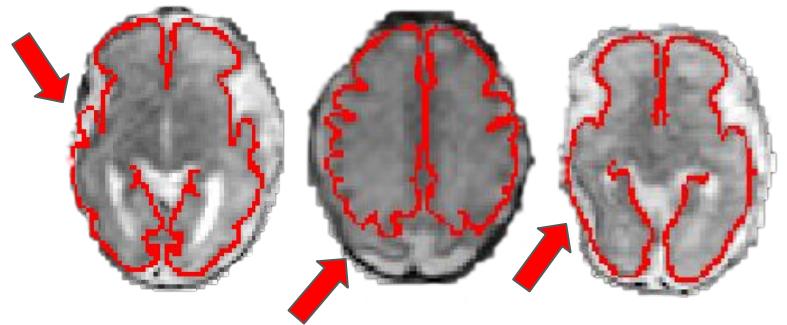


MarsFet

dHCP comparison



Improve parcellations in diffusion space using the subject reconstructed T2



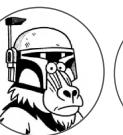
Need good quality anatomical reconstruction and segmentations

Outline

1. **Fetal Diffusion MRI:** challenges and limitations
2. **MarsFet:** clinical human acquisitions
3. **BaboFet:** research baboon acquisitions

BaboFet

Dataset

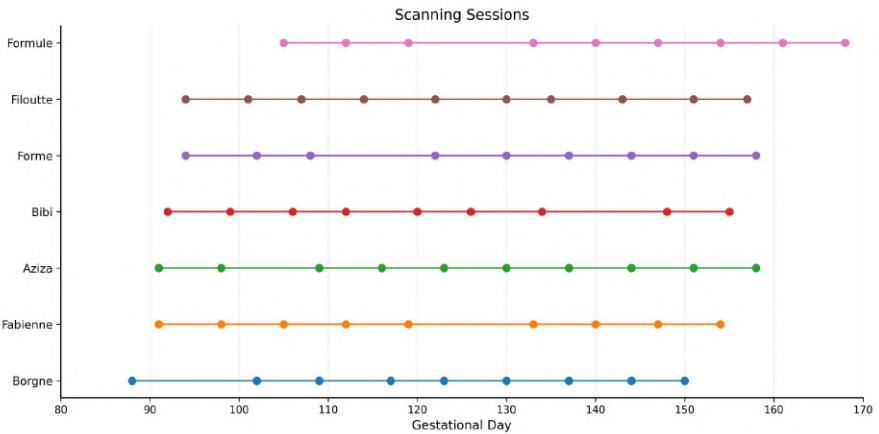


L. Renaud

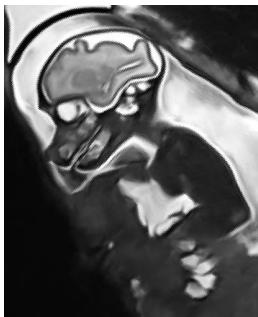
M. Clémenceau

Dataset of 7 pregnant baboons scanned longitudinally, once a week for 10 weeks, between 13wGA and 24wGA, acquired at CERIMED (Marseille, France).

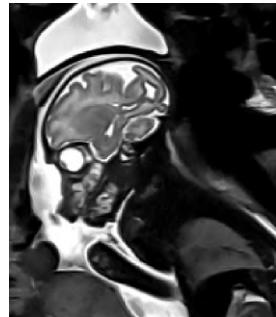
- **Anatomical:** 2D T2 HASTE $0.63 \times 0.63 \times 2 \text{ mm}^3$
- **Diffusion:** 2D Spin Echo EPI, $1.1 \times 1.1 \times 3 \text{ mm}^3$, 30 directions, $b=1000 \text{ s.mm}^{-2}$
- **Functional:** 2D Gradient-recalled Echo EPI, $2.5 \times 2.5 \times 2.5 \text{ mm}^3$, TR/TE=2000/30ms



14w



18w



22w

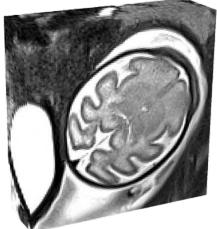


L. Renaud

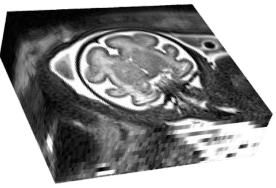
M. Clémenceau

Six 2D stacks of thick slices, 2 per plane with half voxel overlap.
Allow for super-resolution reconstruction

Anatomical



Axial



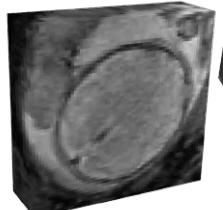
Coronal



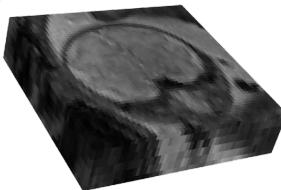
Sagittal

x2

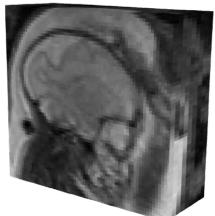
Diffusion



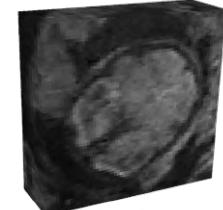
b0



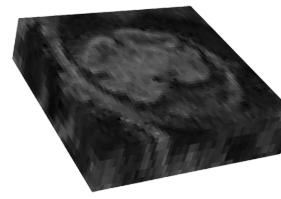
x2



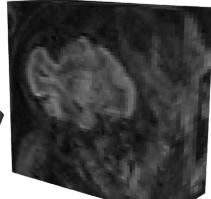
x2



dwi



x2



x2

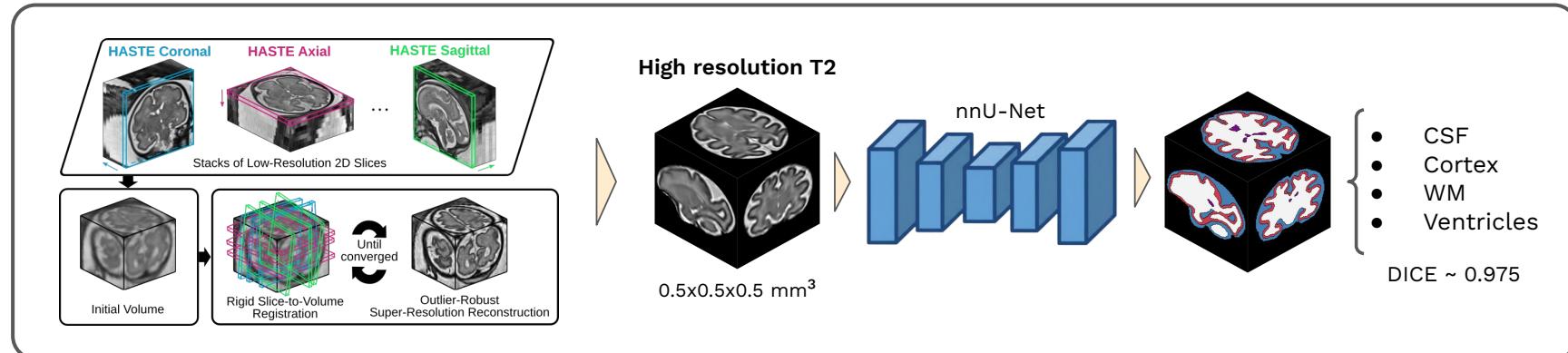
x2

x2

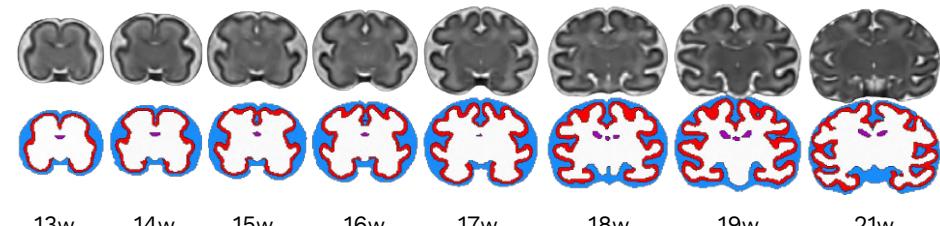
x2

BaboFet

Processing pipeline - anatomical

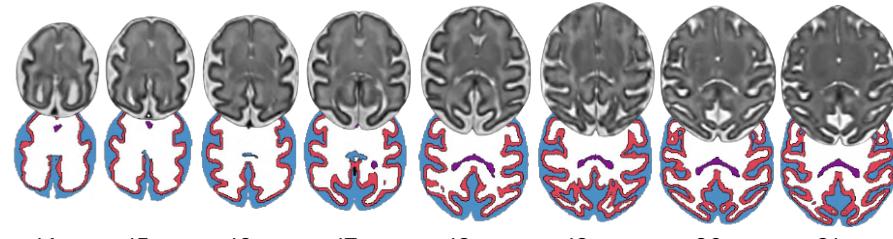


Sub-Bibi



13w 14w 15w 16w 17w 18w 19w 21w

Sub-Borgne



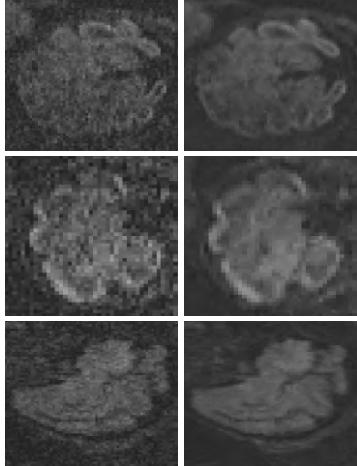
14w 15w 16w 17w 18w 19w 20w 21w

BaboFet

Processing pipeline - diffusion

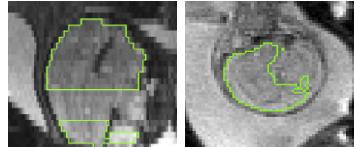
Denoising

Marchenko-Pastur PCA
and
Gibbs ringing removal



Brain extraction

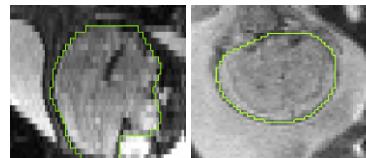
FetalBET struggles with
baboons



Trained **nnUNet** on 359
b0 volumes

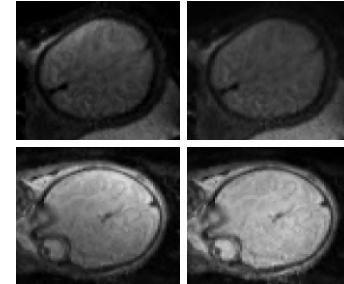


Dice: 0.959 ± 0.017

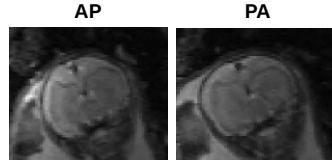


Bias and Distortion correction

N4 Bias correction



Topup

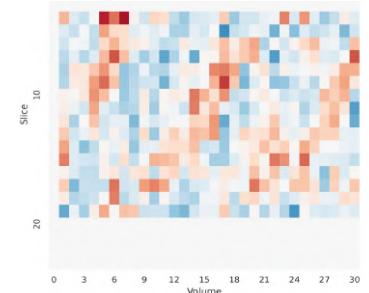
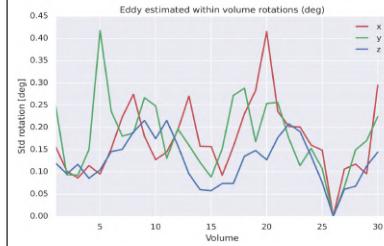


Field

Motion Correction

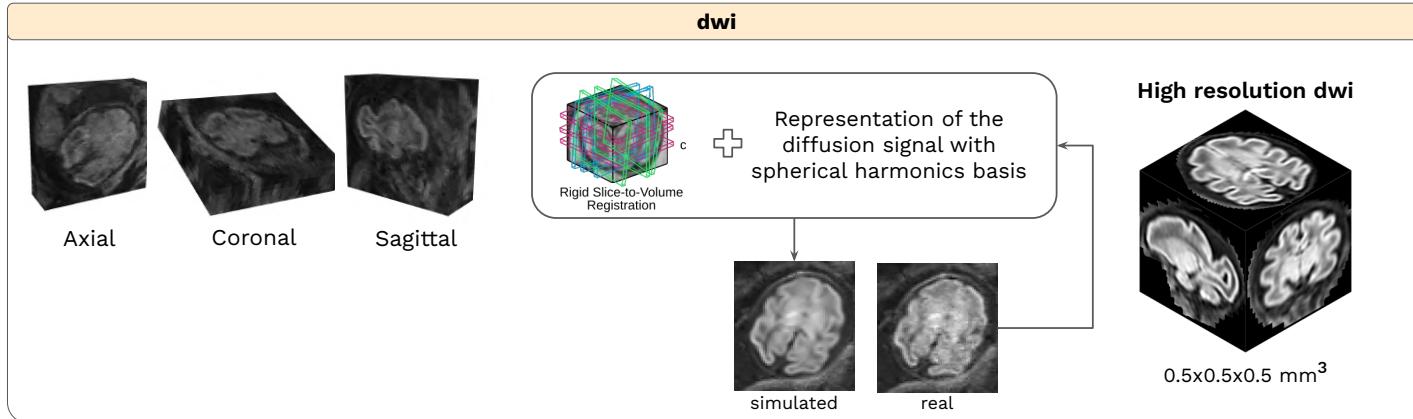
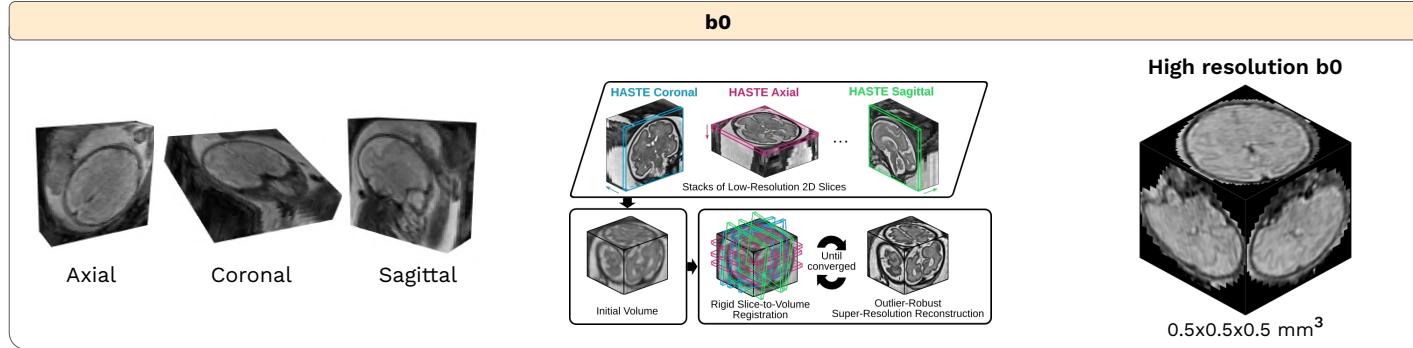
FSL Eddy

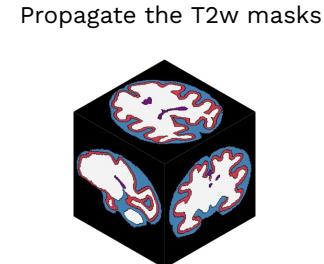
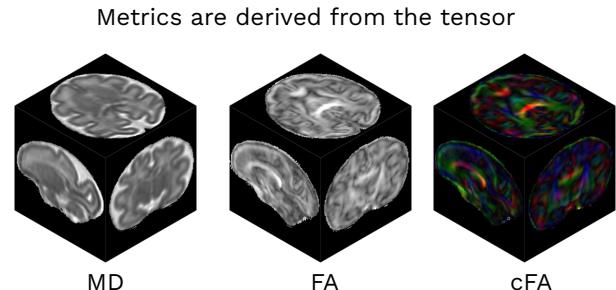
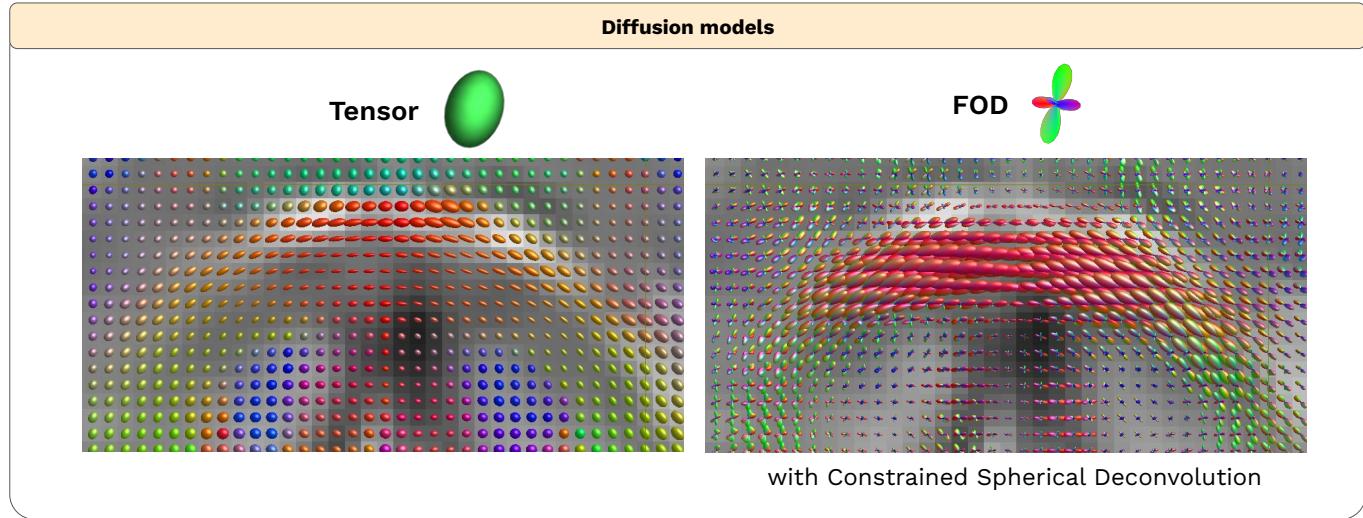
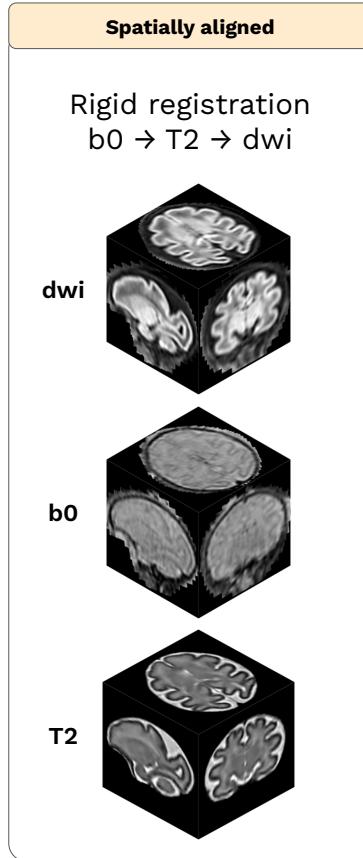
- Slice2Volume
- outlier replacement



BaboFet

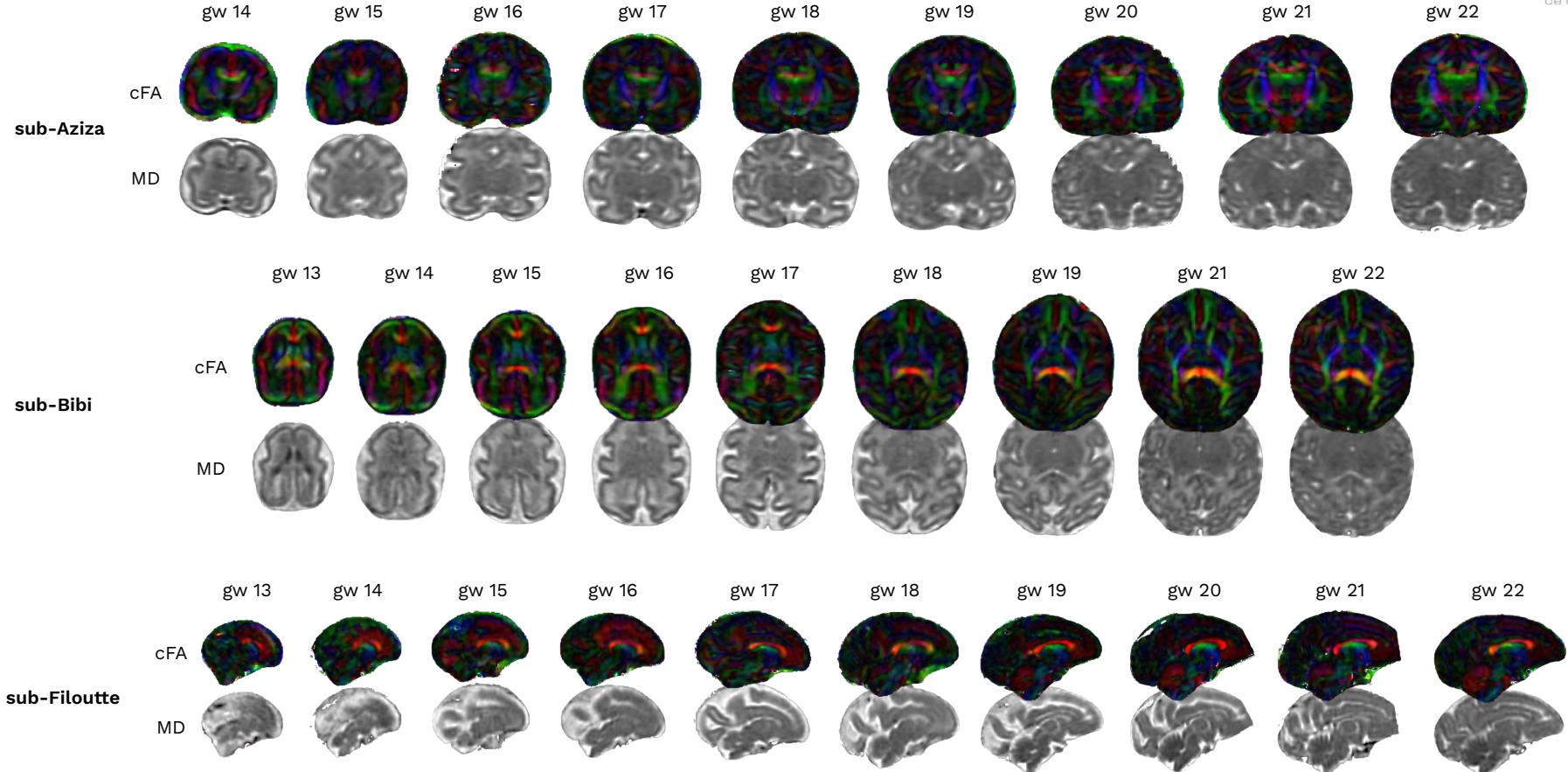
Super-resolution reconstruction





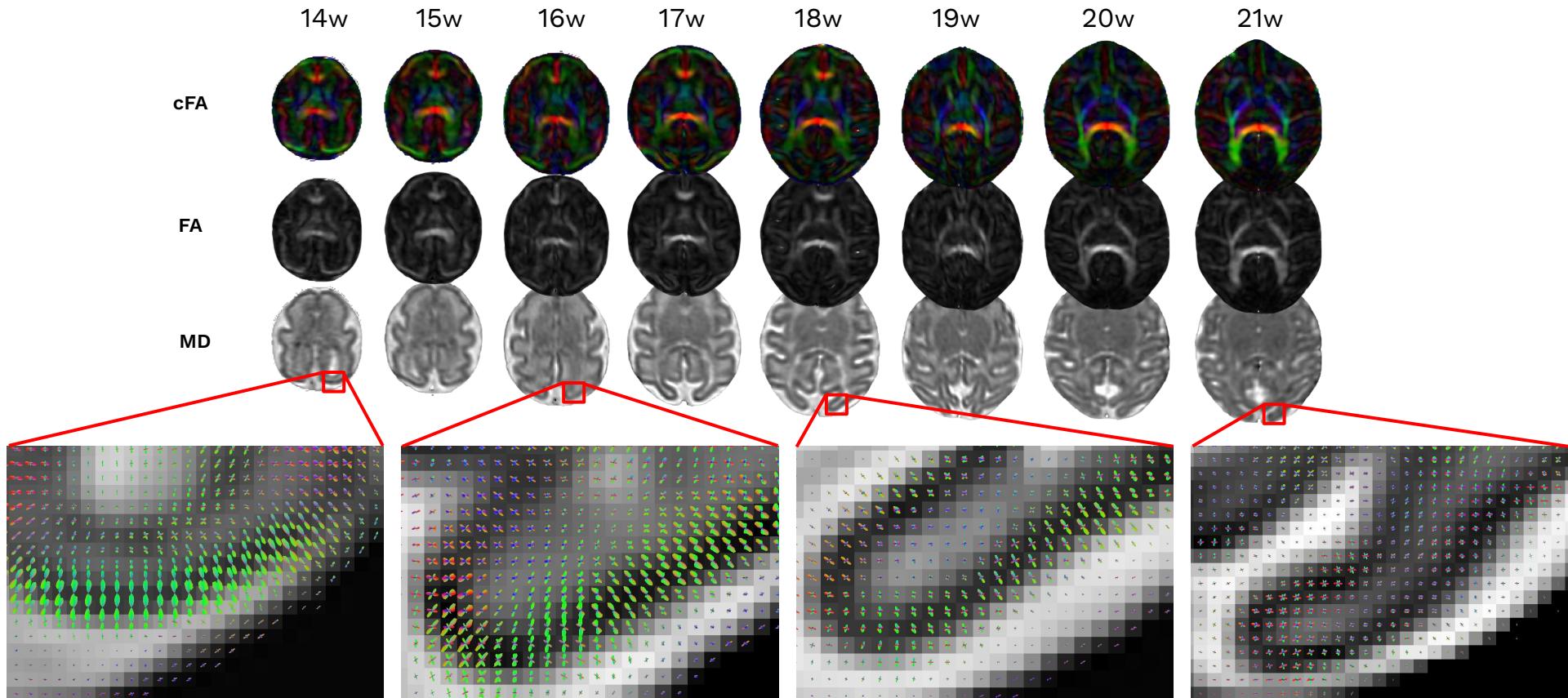
BaboFet

Results



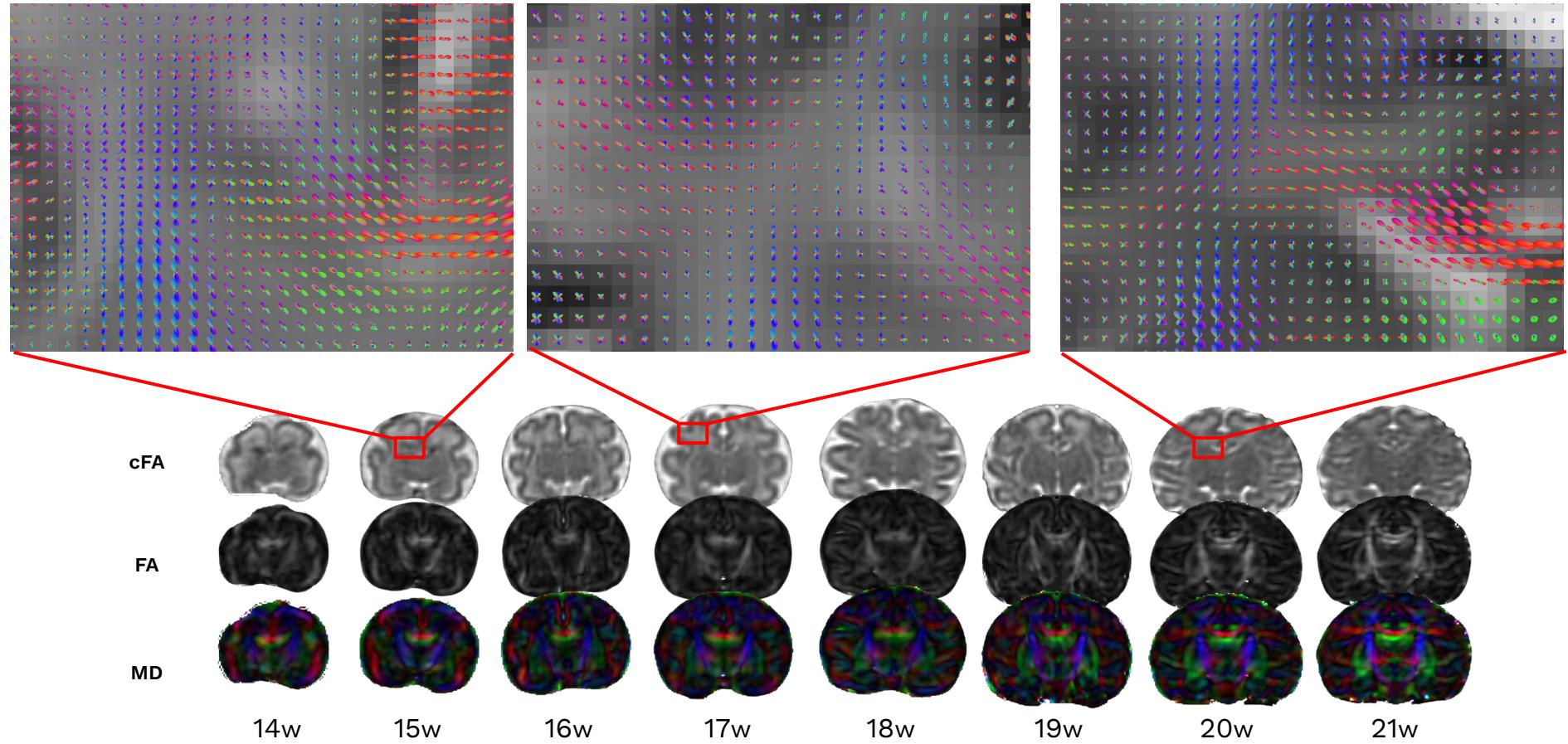
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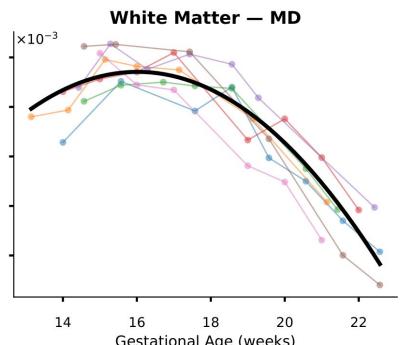
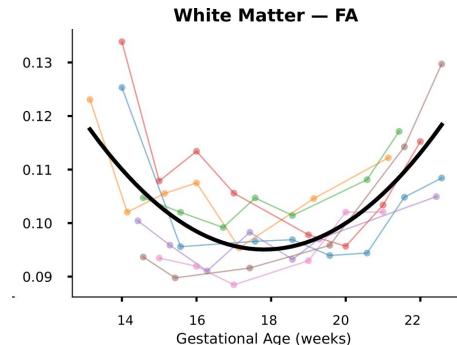
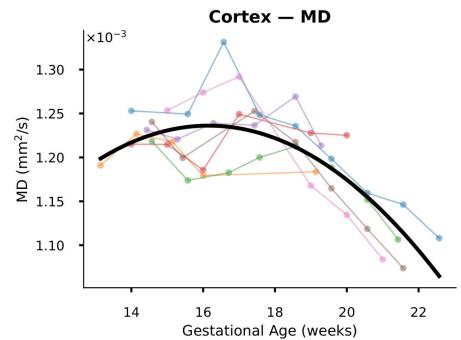
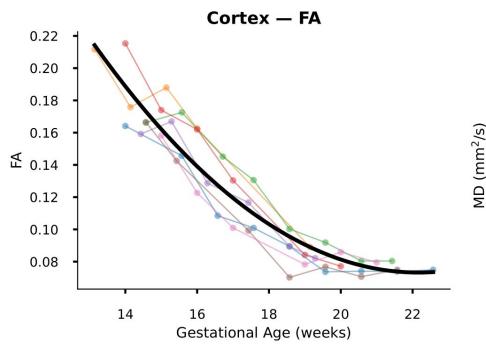
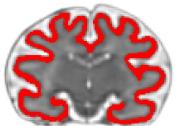
Results - cortex organization



BaboFet

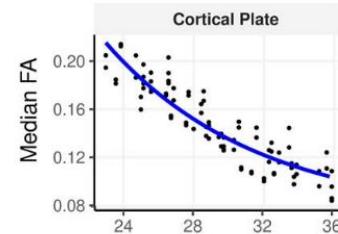
Results - crossing fibers



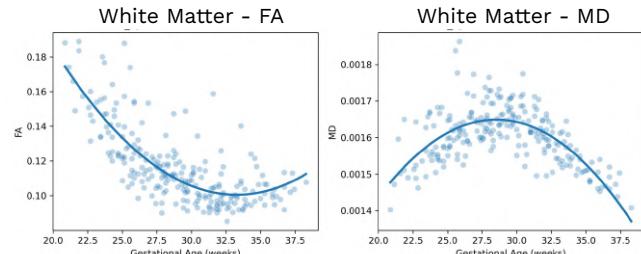


Literature

Calixto et al, Cerebral Cortex

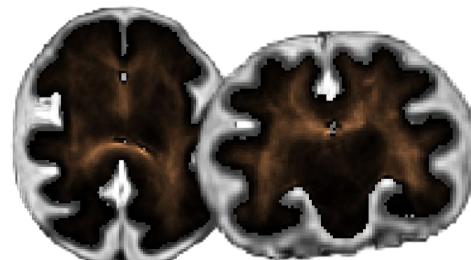
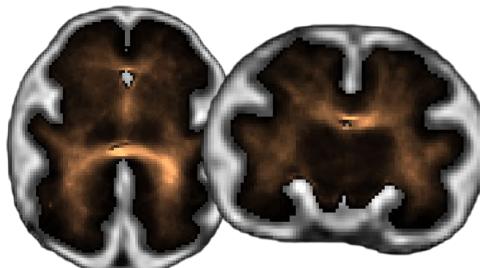
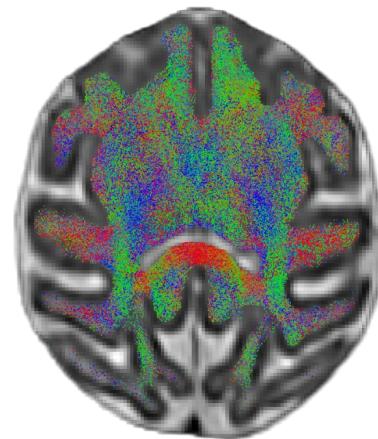
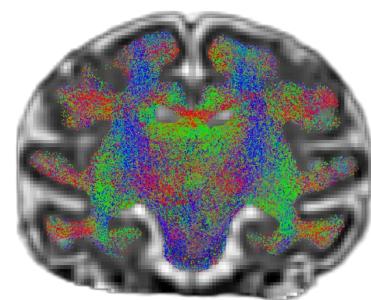
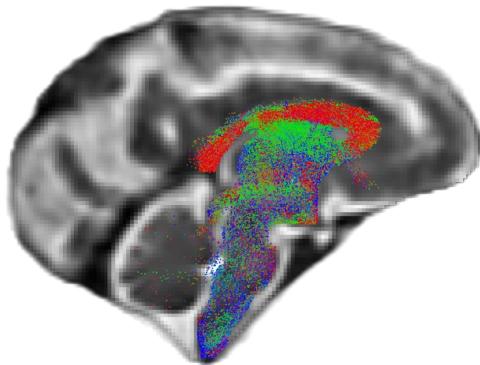


dHCP trends



BaboFet

Future work



THE PEOPLE



G. Auzias



O. Coulon



F. Rousseau



J. Sein



N. Girard



B. Leroux



D. Menieur



H. Dienye



M. Clémenceau



L. Renaud



L. Velly



A. Le Trotter



B. Nazarian



J.-L. Anton



A. Manchon



M. Milh

THANK YOU!